

REPORT NUMBER 3

MEASURING SLEEP BY WRIST ACTIGRAPH

ANNUAL REPORT

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Daniel J. Mullaney, Sam Messin, and William Mason

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20. Abstract, continued.

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Current results now allow us to specify design criteria for a miniaturized wrist-mounted activity monitor suitable for field or combat use.

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SUMMARY

A convenient method of monitoring personnel sleep and activity in field conditions is needed to promote medical planning for modern combat.

In the period from April 1980-March 1981, we have programmed, tested, and begun evaluations of a wearable digital activity system, and we have refined a computer process for recognizing sleep from this system. Together, these efforts enable us to collect data from freely ambulatory subjects which can be scored automatically for sleep/wake with accuracy comparable to EEG scoring. The system is ready for miniaturization leading to field use.

Our microprocessor-based digital activity monitor was built to our specifications, and we added external activity and illumination transducers. Actual data collection was implemented and 25 records totalling over 27,000 minutes have been obtained as of March, 1981. Fourteen records (12,739 minutes) collected with the digital monitor were scored retrospectively with 93.6% agreement with EEG sleep/wake scoring. Research is continuing to further increase the accuracy of the sleep recognition algorithm. Since the errors that occur include both mis-scoring sleep as wake and vice versa, they tend to cancel. Correlations between sleep durations scored from activity data and from EEG records were $r=.9760$ for digital monitor data.

Current results now allow us to specify design criteria for a miniaturized wrist-mounted activity monitor suitable for field or combat use.

FORWORD

For the protection of human subjects the investigator has adhered to policies of applicable Federal Law 45CFR46.

INTRODUCTION

Sleep loss and combat fatigue are increasing concerns for the modern army. A future war is likely to be extremely brief and intense, with victory and defeat determined in a few days or weeks. Soldiers using technically sophisticated modern weaponry will have little time for sleep, and plans must be made to enable personnel to perform effectively throughout the duration of a combat of unprecedented intensity. American troops may have to enter combat immediately after airlift to remote parts of the world, and plans must be developed to minimize the effects of jet-lag on personnel performance.

Military medicine therefore needs a practical method of quantifying sleep both to design personnel strategies and for potential monitoring of troops in actual field deployments.

Traditional physiologic methods for monitoring sleep through EEG-EOG-EMG recordings are completely impractical in actual or simulated combat settings, and subjective monitoring has been shown to be unreliable (1). In addition, both physiologic measures and observational methods for measuring sleep are costly, and considerable time is necessary to quantify sleep by scoring polygraph records.

We are developing a wrist activity monitoring technique as a solution to these problems.

Employing Delgado's (2) telemetric activity recording device, Kupfer et al (3) and Foster et al (4,5) described the use of activity data for quantifying sleep and assessing sleep quality in humans. Encouraged by the high correlations between EEG and actigraphic estimates of sleep -- 0.84 and 0.88 in two separate studies (6,7) -- Kripke et al (8) developed a system in which a piezoceramic activity transducer worn on a watchband recorded wrist activity onto a Medilog cassette tape recorder worn on a belt. With this transducer, Kripke et al (8) obtained a correlation of 0.98 between sleep duration determined from wrist activity and the EEG in five subjects.

A more exhaustive study of 63 nights of normal subjects and 39 nights in hospital patients with various sleep disorders was conducted under the first year of our contract (DAMD-17-78-C-8040, 1978-1979). All-night recordings of wrist activity, EEG, EMG and EOG were collected simultaneously on a 4-channel cassette. Each minute was scored as either sleep or wake by one rater using only activity data, and a second rater using only EEG-EOG-EMG data. The raters agreed on 94.5% of the minutes (96.3% for non-patients). Estimates of each subject's total sleep time with the two methods were correlated 0.89 (0.95 for non-patients). These results indicate that the wrist actigraphic analog recording contains sufficient information to produce a highly reliable scoring of sleep.

Having shown that sleep can be identified from activity data, we proposed in 1979 to design a 2-part sleep monitoring system. A digital activity monitor, consisting of an activity transducer, microprocessor and digital memory, would be worn on the wrist. A portable readout device, also microprocessor based, would read and reset the monitors, then interpret their data and generate a sleep report.

To realize this design, a first priority was to establish the optimal design, orientation and placement for the activity transducer. We found the piezo-ceramic transducer used in our previous research to be more sensitive than other available transducers and to be adequately omnidirectional. We also found the wrists to be more active than an ankle or the head, and therefore a better site for locating a transducer. The choice of wrists does not seem crucial, but the non-dominant wrist seems slightly superior (e.g., the left wrist).

Having established optimal transducer design characteristics, we turned our attention to digitizing, preprocessing and storing activity data. As reported in our 1979-1980 report, we found that digitizing at 240 Hz and summing every four digital conversions cancelled 60 Hz noise which sometimes contaminates activity recordings. We also found that a preprocessing algorithm which emphasized changes in activity level provided the best data for automatic sleep recognition. Our 1979-1980 report described our approach to empirically developing an algorithm to recognize sleep from digitized activity data. The further refinement of that approach, and its implementation in a wearable system will be described below.

FURTHER PROGRAM DEVELOPMENTS

Method

Data were obtained from subjects participating in studies involving EEG recording during both wake and sleep. A wrist activity transducer signal was sampled during both wake and sleep. The wrist activity transducer signal was sampled by the analog-to-digital (A/D) converter of our laboratory computer system at a conversion rate of 240 Hz. The analog data was digitized and stored as described in our 1979-1980 report, but only the optimal preprocessing transformation selected in that report was used in data analysis. A total of 20 records (13,488 minutes) were analyzed.

Development of the sleep recognition algorithm began with expressions incorporating a weighted sum of combinations of the digital data with potential for discriminating sleep from wake. Specifically, the expression took the form:

$$D = S \times (W_1 T_1 + W_2 T_2 + W_3 T_3 + W_4 T_4 + W_5 T_5 + W_6 T_6)$$

where S was a scale factor, W's were weights, and:

T_1 = the sum of the digital activity values for all 30 2-second data epochs in a minute,

T_2 = the activity value for the single most active epoch,

T_3 = the sum of the activity values in the two most active epochs separated by at least 30 seconds,

T_4 = the sum of the activity values in the most active 8 epochs.

Terms T_5 and T_6 were themselves weighted sums of term T_1 over the preceding 4 and following 2 minutes:

$$T_5 = W_{51} T_{1,i-1} + W_{52} T_{1,i-2} + W_{53} T_{1,i-3} + W_{54} T_{1,i-4}$$

$$T_6 = W_{61} T_{1,i+1} + W_{62} T_{1,i+2}$$

where $T_{1,i-1}$ is the maximal epoch value for the preceding minute, $T_{1,i+1}$ for the following minute, etc.

A minute was scored 'wake' if $D \geq 1.0$. For each given combination of weights, a range of weights (W) and scale factors (S) was substituted into the above expression for each minute, and the resulting sleep/wake score for all minutes. The proportion of minutes for which the automatic score and EEG score agreed was then computed for each scale value, and the maximum agreement served as a retrospective measure of the effectiveness of the weighting. The computer program (Appendix 1) varied the weighting of one term at a time, and searched for the combination of weights which produced the highest agreement.

As preliminary results became available, it became apparent that better agreement was obtained when $W_1 = W_3 = W_4 = 0$, i.e., the maximal epoch value in each minute was the best discriminator of sleep and wake. This unexpected result was extremely fortunate, since it permitted reducing the data required for sleep scoring by an order of magnitude compared to our prior expectation. We had expected that all 2-second epoch values for each minute would have to be stored.

Accordingly, a second expression was developed:

$$D = S \times (W_1 T_{2,i-4} + W_2 T_{2,i-3} + W_3 T_{2,i-2} + W_4 T_{2,i-1} + W_5 T_{2,i} + W_6 T_{2,i+1} + W_7 T_{2,i+2})$$

where W's represent weights and $T_{2,i}$ represents the maximal epoch value (T_2 in the previous expression) for the current minute, $T_{2,i-1}$ for the previous minute, $T_{2,i+1}$ for the succeeding minute, etc. Again, the computer varied the weighting and compared the resulting sleep/wake score with the EEG score until maximal agreement was obtained.

Seventeen of the 20 records were used in the algorithm development phase described above. The remaining three records were scored prospectively, i.e. each of the three records was scored individually with the single weighting and scale factor found optimal in the development phase. In this test, the laboratory computer simulated the actual deployment of an automatic sleep scoring system, with the results compared to EEG scoring.

Results

The optimal algorithm reached after analysis of the 17 records was:

$$D = .025 \times (.15 T_{2,i-4} + .15 T_{2,i-3} + .15 T_{2,i-2} + .08 T_{2,i-1} + .21 T_{2,i} + .12 T_{2,i+1} + .13 T_{2,i+2})$$

where $T_{2,i}$ represents the maximal epoch value in minute i, etc. If $D \geq 1.0$, the minute was scored 'wake', otherwise 'sleep'. The best retrospective agreement between sleep/wake scored automatically with this algorithm and scoring from

EEG records was 94.46% -- that is, 94.46% of all minutes from the 17 subjects were in agreement with the 'true' sleep/wake score. Agreement scores and the proportion of the record scored as sleep by EEG and by the automatic algorithm for each individual subject are shown in Table 1. Again, it should be noted that this is retrospective agreement, the data for these individuals already having been used to select the optimal algorithm.

The ability of this algorithm to score sleep/wake prospectively was tested with the remaining three records. For these records, only the single expression found optimal in the algorithm development phase was chosen prospectively to automatically score sleep/wake. Overall agreement of these three records with EEG scoring was 96.02%. Agreement and the proportion of each individual record scored sleep by both procedures is also shown in Table 1.

In order to understand the remaining shortcomings of the automatic sleep/wake scoring algorithm, data for all minutes mis-scored were listed and compared with the paper record. In general, the conditional probability of mis-scoring wake as sleep was higher (.062) than mis-scoring sleep as wake (.039). A major reason for the higher probability of mis-scoring wake was the tendency of some subjects to lie in bed quietly for up to half an hour before falling asleep, while generating alpha-frequency EEG. On the other hand, while most examples of mis-scoring sleep were due to the presence of activity during sleep, the source of error in these cases was not so much a failure of the actigraphic scoring concept as a problem with the 1-minute scoring epoch chosen for this study. Many of the 'activity during sleep' errors actually represented arousals, but the EEG record showed that the period of wakefulness was less than the one-half minute required to score a 1-minute epoch as wake.

Since mis-scoring occurred in both directions, the estimates of total sleep duration were better than might be inferred from the minute-by-minute agreement figures. The correlation coefficient between the proportion of the record scored as sleep automatically from activity and as hand-scored from EEG were $r=0.9889$ (for the 17 records scored retrospectively) and $r=0.9982$ (for the 3 prospective records). Thus, the automatic scoring represents the relative duration of sleep extremely accurately. Since sleep duration is the dimension of sleep most crucial to sustaining performance, we feel that the automatic sleep recognition procedure described here represents a very effective scoring technique.

A further test conducted with these data sought to determine the resolution in the stored data necessary to achieve these levels of accuracy. The digital activity value was stored on disk as a 16-bit word, i.e. a number in the range of 0-32767. To investigate the resolution requirement, the sleep recognition program was repeated with the same data, but the resolution was reduced by dividing by powers of 2 and truncating. There was no decrease in agreement with 4-bit data (0-15) and a decrease of only 0.1% with 3-bit data (0-7). This surprising result is important, since it means that more data can be stored in a given memory capacity of the wearable activity monitor, providing appropriate scale factors are chosen.

TESTING THE DIGITAL ACTIVITY MONITOR

In our original proposal to produce a wearable digital activity monitor, we suggested a design in which the signal from a piezo-ceramic activity transducer would be entered through an analog-to-digital converter into an IM6100 microprocessor, and the processed activity values stored in random-access memory. All electronic components of this proposed system would be CMOS for minimal power consumption.

As noted in our 1979-1980 Annual Report, we found that these components could be assembled by the Vitalog Corporation*. After extensive discussions with Vitalog, we ordered a prototype monitor consisting of an IM6100 microprocessor, IM6001 Parallel Interface Element, 6K x 12 RAM memory, 512 word EPROM memory, 8-channel A/D converter, crystal clock and an LED indicator light. The unit is powered by rechargeable 5.6 volt batteries. It is enclosed in a 15 cm x 9 cm x 5½ cm plastic case. Vitalog also provided an interface between the monitor and our Apple microcomputer.

After receiving the monitor, we designed and built an external transducer incorporating a piezo-ceramic element, a photocell, a battery and amplification circuitry necessary to match the A/D input requirements. (The photocell was included to permit an objective measure of "lights out" and "lights on" and potentially to investigate sleep onset latency.) This external transducer, 7 cm x 4 cm x 2 cm, is worn on a wrist band like a watch. It is attached to the monitor by a cable. A schematic diagram of the transducer circuitry is presented as Figure 1.

Having assembled and tested the monitor system, we began by investigating its technical capabilities. One very important technical consideration was the useful life of the battery charge, since this limits the duration of a recording session. Battery drain was found to be 3.4 mA when the processor was halted and 8.5 mA when running. Since in most applications the processor is idling much of the time, a third state (WAIT) can be entered which keeps the processor running, but not executing instructions, at a drain of about 5.2 mA. The battery life was found to be 70 hours at 8.5 mA (running continuously) and 180 hours at 5.2 mA (running with WAIT). We subsequently devised a system for changing batteries without disturbing the recording, removing this limit to recording duration. We also investigated the accuracy of the crystal clock, and found that it lost 1.2 seconds each hour, well within acceptable limits. While considerable improvement in battery life can probably be obtained in any future model, the Vitalog system already demonstrates the feasibility of powering a microprocessor-based wrist activity monitor.

The majority of our effort in preparing the monitor system for use has been in development of a monitor program to direct the collection and storage of activity data. The algorithms for converting the continuous analog signal from the activity transducer to a value representing activity for each minute were equivalent to those discussed above. The monitor program that was ultimately developed, tested, and used to collect digital activity records digitized the signal from the transducer at 240 Hz, and 4 consecutive values were summed to provide a measure of activity free of 60 Hz noise. The sum was then transformed

*Vitalog Corporation, 1056 California Avenue, Palo Alto, CA 94306.

to a difference score, and 120 such scores summed to produce an activity value for each 2-second data epoch. Every minute, the greatest 2-second activity value in that minute was stored. A voltage indicating the illumination level of the photocell was also digitized and stored each minute and a time code was signaled through the LED. The monitor program (Appendix 2) fills 448 memory locations, leaving 5696 locations available for data storage. This allows us to store two 12-bit data words (activity and illumination) each minute for 47 hours and 28 minutes. Since 4-bit resolution would be adequate, up to 6 times this duration or about 12 days sleep data could be stored were the illumination data sacrificed and battery changes feasible.

For test recordings, where it is necessary to compare digital activity records with EEG recordings, the LED was coupled through a receiving photocell to the polygraph to provide a time reference each minute on the paper record. The EEG recordings were scored, and both EEG and activity monitor scores were transferred to our laboratory computer system. To date, 25 laboratory recordings totalling over 27,000 minutes have been collected, and 14 have been fully analyzed retrospectively. Results are presented in Table 2. Retrospective agreement of these 14 records (12,739 minutes) is 93.6% with EEG scoring. The correlation coefficient between the proportion of each record scored as sleep by the two techniques is $r=.9760$.

In the final months of our 1980-1981 contract year, we plan to analyze a series of activity-monitored nights with prospective scoring to complete validation of our sleep scoring methodology. In addition, we will prepare a complete technical specification of the methodology from which a microminiaturized monitor wearable entirely on the wrist could be built. Our Vitalog digital monitor is fully programmable and in no way limited by the program described above. Any number of control programs could be written to record activity or illumination data differently and to monitor other functions through the unused A/D channels. These extended capabilities of the instrument can be utilized in our proposed 1981-1982 contract.

CONCLUSION

Mullaney, Kripke and Messin (9) have shown that a trained scorer can score wrist activity data for sleep/wake with accuracy approaching EEG scoring. In the present study, we have shown that wrist activity data can be digitized and scored automatically by computer with no loss in accuracy. Mullaney et al estimated that their activity scoring system was 5 to 10 times less costly than EEG scoring, and that the marginal decrease in accuracy was more than compensated by the greater amount of data that could be collected for a given expense. We feel that the automatic scoring system described here further improves the cost-benefit relationship by replacing the largely mechanical analog recording and playback system, including the polygraph, with an all-digital system. Automatic scoring is accomplished in seconds, eliminating the hours of skilled labor needed for writing out a polygraph record and the many minutes needed for visually scoring the record. Elimination of a scorer further reduces costs and for the first time makes the identification of sleep and wake fully objective, without the many opportunities for error and variability presented by human scoring. We are continuing with further algorithm refinements and testing, but it is unlikely much improvement can be obtained over the current results, nor is much improvement needed.

As of March, 1981, we have completed the major technical goals of our contract. Specifically, we have designed, built, tested, and evaluated a wearable digital activity monitor usable for sleep/wake scoring. Preliminary validation studies (using a retrospective technique) produced a $r=.9760$ correlation of automatic scoring of total sleep duration versus EEG scoring. This far exceeds our 90% design specification. Our technical development has been extremely successful. Judging from our experience with the same algorithm utilized with the laboratory computer, we believe there will be little or no degradation of validity in prospectively scored records, nevertheless, we are completing prospective validation in the remaining months of our 1980-1981 contract. In addition, we will submit an exact technical specification giving hardware and software specifications for a miniaturized microprocessor-controlled activity monitor. With this specification, a miniaturized monitor wearable entirely on the wrist could be designed and produced with currently available technology.

A miniaturized wrist-mounted sleep monitor could be used in field trials or in actual combat to monitor the fatigue and sleep-loss of Army troops.

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Figure 1. Schematic diagram of external activity transducer, photocell and level-matching amplification circuitry

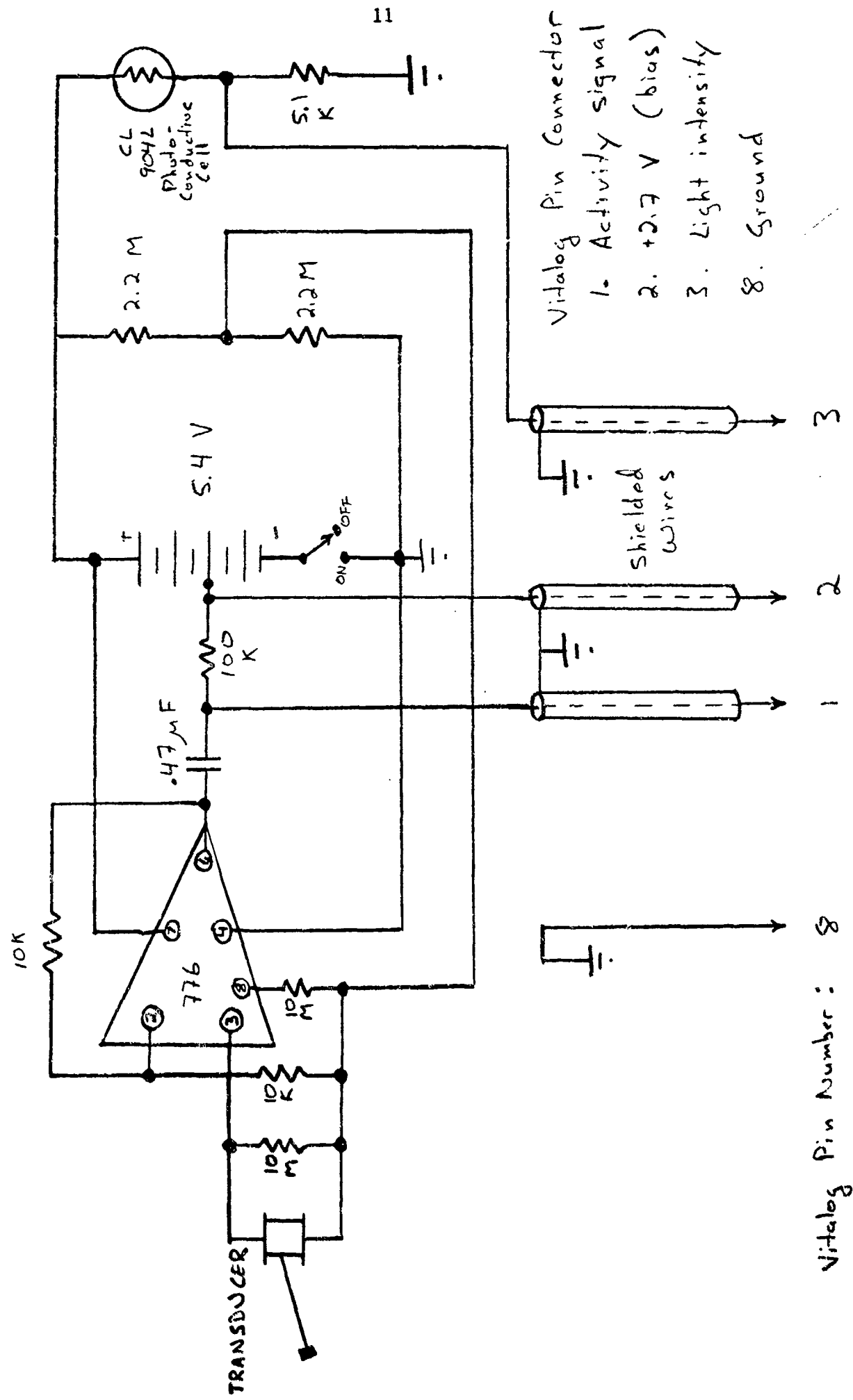


TABLE 1

Subject	Recording Duration (minutes)	% Agreement	% Sleep (EEG)	% Sleep (Act.)
1	353	97.17	0.00	2.83
2	574	96.17	45.47	46.86
3	632	95.89	56.80	59.65
4	903	83.82	29.57	34.33
5	660	97.42	54.55	56.21
6	798	95.36	41.73	44.11
7	845	96.80	37.99	40.95
8	1129	96.19	30.65	31.62
9	644	96.89	50.47	51.40
10	553	88.79	56.06	48.10
11	371	96.77	92.72	95.96
12	527	96.96	14.99	16.13
13	226	89.82	93.81	93.36
14	673	91.98	50.67	45.62
15	593	95.73	56.49	59.36
16	829	91.19	40.17	47.77
17	<u>692</u>	<u>94.08</u>	<u>15.17</u>	<u>20.18</u>
Total				
Retrospective	11002	94.46	42.09	43.98
18	369	93.50	70.19	76.69
19	846	93.62	28.84	31.68
20	<u>1271</u>	<u>98.35</u>	<u>36.82</u>	<u>37.69</u>
Total				
Prospective	2486	96.02	39.06	41.39

Table 1. Record duration, proportion of the record for which hand-scored EEG and automatically scored activity scores agree, and proportion of the record scored as sleep by the two techniques. Total duration and overall proportions for the records scored retrospectively and those scored prospectively are also presented.

TABLE 2

<u>Subject</u>	<u>Recording Duration</u>	<u>% Agreement</u>	<u>% Sleep (EEG)</u>	<u>% Sleep (Act.)</u>
1	366	89.92	85.71	95.80
2	2847	95.67	18.68	20.89
3	1472	97.95	24.27	25.91
4	2848	96.90	20.61	23.42
5	461	90.93	97.35	92.70
6	344	95.52	97.61	97.31
7	465	83.55	88.16	79.61
8	500	91.65	91.85	88.39
9	502	91.89	90.06	85.19
10	487	92.68	96.03	96.65
11	483	94.39	82.70	97.05
12	503	83.20	81.58	93.52
13	1100	92.12	35.47	39.32
14	487	90.17	89.33	98.33
Total				
Retrospective	12739	93.61	46.38	48.87

Table 2. Record duration, proportion of the record for which hand-scored EEG and automatically scored activity scores agree, and proportion of the record scored as sleep by the two techniques. Total duration and overall proportions are also presented.

APPENDIX 1

For Hewlett-Packard 1000

WHEEL T-00004 IS ON CR00334 USING 00026 BLKS R=0000

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0001 FTN4
0002 PROGRAM WHEEL(3,999)
0003 ..Finds parameters yielding best agreement for s/w.
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WHEEL

ABSTRACT: Finds parameters yielding best agreement for s/w.

CALLING SEQUENCE:
WHEEL,LUI,LUO,S/RJ

PARAMETERS OR ARGUMENTS:
LUI is interactive terminal, LUO is output device.
S/R is single pass (0)/repeat (1) feature
Default: Input=1 (System terminal)
Output=6 (Versatec)
S/R=0 (Single pass)

DETAILED DESCRIPTION:
-----
DIMENSION IDCB(3000),ISTAT(10),C(20),W(20)
DIMENSION IPO(01,20,4),LU(5),IFILE(3),NW(5),CX(20)
DIMENSION IBUF(3072),VECTR(20),PP(8),CW(20)
DATA IFILE/2HHD,2HAT,2H00/

C-----
C ASSIGN I/O DEVICES
C-----
CALL RMPAR (LU)
IF (LU.EQ.0) LU=1
LUI=LU
IF (LU(2).EQ.0) LU(2)=6
LUO=LU(2)

C-----
C INPUT PARAMETERS
C-----
50 WRITE (LUI,100)
100 FORMAT (/' HP' OR 'VI'? : '-')
READ (LUI,8000) NA
IF (NA.NE.2HHP) GO TO 110
IFILE=2HHD
LO=15
LIM=35
RESULT=1.

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0063 GO TO 150
0064 110 IF (NA.NE.2HV1) GO TO 50
0065 IF FILE=2HVD
0066 LO=66
0067 LIM=65
0068 WRITE (LUI,125)
0069 125 FORMAT (" MULTIPLY VITALOG SCORE BY: ")
0070 READ (LUI,*) XMULT
0071 LO=LO-XMULT*10
0072 LIM=LIM-XMULT*10
0073 150 WRITE (LUI,200)
0074 200 FORMAT (/" NUMBER OF MINUTES FORWARD: ")
0075 READ (LUI,*) IFW
0076 KJ=IFW+1
0077 WRITE (LUI,250)
0078 250 FORMAT (" NUMBER OF MINUTES BACKWARD: ")
0079 READ (LUI,*) IBW
0080 IF=IBW+IFW+1
0081 IF (IW.LE.10) GO TO 350
0082 WRITE (LUI,300)
0083 300 FORMAT (" *** 10 MINUTES MAX *** ")
0084 GO TO 150
0085 350 WRITE (LUI,400)
0086 400 FORMAT (/" ENTER WEIGHTS FOR MINUTE. . "/)
0087 K=0
0088 DO 500 I=-IBW,IFW
0089 K=K+1
0090 IF (I.GE.0) GO TO 400
0091 WRITE (LUI,470) K,I
0092 470 FORMAT (30X,12") I"12": ")
0093 GO TO 495
0094 480 IF (I.GT.0) GO TO 490
0095 WRITE (LUI,481) K
0096 481 FORMAT (30X,12") *I": ")
0097 GO TO 495
0098 490 WRITE (LUI,491) K,I
0099 491 FORMAT (30X,12") I+"11": ")
0099 495 READ (LUI,*) W(K)
0100 500 CONTINUE
0101 545 DO 550 I=1,4
0102 NW(I)=0
0103 550 CONTINUE
0104 WRITE (LUI,560)
0105 560 FORMAT (/" ENTER UP TO 4 WEIGHTS TO BE 'BRACKETED' : ")
0106 READ (LUI,*) NW(1),NW(2),NW(3),NW(4)
0107 WRITE (LUI,580)
0108 580 FORMAT (/"
0109 LK=4
0110 IF (NW(4).EQ.0) LK=3
0111 IF (NW(3).EQ.0) LK=2
0112 IF (NW(2).EQ.0) LK=1
0113 IF (NW(1).EQ.0) LK=0
0114 LN=3**LK
0115 DO 760 I=1,IW
0116 CH(I)=W(I)
0117 760 CONTINUE
0118 775 DO 800 K=1,61
0119 DO 800 J=1,20
0120 DO 800 I=1,4
0121 IPO(K,J,I)=0
0122 800 CONTINUE
0123 IF (LUI(3).EQ.1) GO TO 875
0124 IF (LUI(0).EQ.5) WRITE (LUI,850)
0125

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0127 875 DO 4200 IO=101,126
0128 IF (NA.EQ.2HVI) GO TO 900
0129 IF (IO.EQ.101) GO TO 4200
0130 IF (IO.EQ.107) GO TO 4200
0131 IF (IO.EQ.108) GO TO 4200
0132 IF (IO.EQ.114) GO TO 4200
0133 IF (IO.EQ.115) GO TO 4200
0134 IF (IO.EQ.117) GO TO 4200
0135 GO TO 950
0136 900 IF (IO.GE.115) GO TO 4200
0137 950 IF (IO.EQ.115)=KCVT(IQ)
0138 C-----
0139 C READ DATA FILE
0140 C-----
0141 1000 CALL OPEN (IDCB,IER,IFILE)
0142 IF (IER.LT.0) GO TO 9900
0143 CALL READ (IDCB,IER,IBUF)
0144 IF (IER.LT.0) GO TO 9910
0145 LEN=IBUF*256+IBUF(2)
0146 IL=LEN+2
0147 CALL READ (IDCB,IER,IBUF,IL,JL,-1)
0148 IF (IER.LT.0) GO TO 9920
0149 IF (LU(3).EQ.1) GO TO 2100
0150 WRITE (LUO,2000) IFILE,LEN
0151 2000 FORMAT (2H ,3A2,18- MINUTES--)
0152 C-----
0153 C PROCESS DATA
0154 C-----
0155 2100 DO 4000 I=3,IL
0156 DO 2200 J=IV,2,-1
0157 VECTR(J)=VECTR(J-1)
0158 ISTAT(J)=ISTAT(J-1)
0159 2200 CONTINUE
0160 ISTAT=1
0161 IF (NA.EQ.2HVI) GO TO 2300
0162 IF (IBUF(1).LE.0) IBUF(1)=63
0163 IF (IBUF(1).LT.128) GO TO 2500
0164 IBUF(1)=IBUF(1)-128
0165 ISTAT=0
0166 VECTR=FLOAT(IBUF(1))*XMULT
0167 IF (VECTR.GT.63) VECTR=63
0168 DO 3000 IZL=1,LN
0169 D=0.
0170 DOT=0.
0171 IF (I-2.LT.IV) GO TO 4000
0172 IF (IW(4).EQ.0) GO TO 3002
0173 CW(NW(4))=W(NW(4))+((IZL-1)/27-1)
0174 IF (IW(3).EQ.0) GO TO 3004
0175 CW(NW(3))=W(NW(3))+((MOD((IZL-1),27)/9-1)
0176 IF (IW(2).EQ.0) GO TO 3006
0177 CW(NW(2))=W(NW(2))+((MOD((IZL-1),9)/3-1)
0178 IF (IW(1).EQ.0) GO TO 3020
0179 CW(NW(1))=W(NW(1))+((MOD((IZL-1),3)-1)
0180 WJ=WJ+J
0181 DO 3000 IZ=1,IW
0182 W=0.0+CW(IZ)
0183 3000 CONTINUE
0184 DO 3000 IZ=1,IW
0185 C(IZ)=CW(IZ)/W
0186 3000 CONTINUE
0187 C (DOT PRODUCT LOOP)
0188 2600 DO 2700 K=1,IW
0189 DOT=DOT+VECTR(K)*C(K)
0190 2700 CONTINUE

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C191 DO 330 JJ=LO,LIM
C192 SCALE=JJ/1000.
C193 D=DOT*SCALE
C194 L=JJ-(LO-1)
C195 KS=0
C196 IF (D.GE.1.0) KS=2
C197 LS=15*STAT(KJ)
C198 KLS=KS+LS+1
C199 IPO=IZL,L,KLS)=IPO(IZL,L,KLS)+1
C200 CONTINUE
C201 3800 CONTINUE
C202 3900 CONTINUE
C203 4000 CONTINUE
C204 4200 NS=IPO(1,1,1)+IPO(1,1,3)
C205 NN=IPO(1,1,1)+IPO(1,1,2)+IPO(1,1,3)+IPO(1,1,4)
C206 HMAX=0
C207 DO 4700 J=1,LN
C208 HMAX=J
C209 DO 4600 I=LO,LIM
C210 L=I-(LO-1)
C211 NC=IPO(J,L,1)+IPO(J,L,4)
C212 HMAX=MAX0(HMAX,NC)
C213 IF (HMAX.NE.NC) GO TO 4510
C214 SSMAX=1/1000.
C215 MAXJ=J
C216 HMAX=MAX0(HMAX,NC)
C217 IF (HMAX.NE.NC) GO TO 4600
C218 MAYC=NC
C219 SMAX=1/1000.
C220 MAXI=L
C221 4600 CONTINUE
C222 IF (HMAX(4).EQ.0) GO TO 4602
C223 CW(HMAX(4))=V(HMAX(4))+((J-1)/27-1)
C224 IF (HMAX(3).EQ.0) GO TO 4504
C225 CW(HMAX(3))=V(HMAX(3))+((MOD((J-1),27)/9-1)
C226 IF (HMAX(2).EQ.0) GO TO 4605
C227 CW(HMAX(2))=V(HMAX(2))+((MOD((J-1),9)/3-1)
C228 IF (HMAX(1).EQ.0) GO TO 4606
C229 CW(HMAX(1))=V(HMAX(1))+((MOD((J-1),3)-1)
C230 WJ=J
C231 DO 4650 I=1,10
C232 WJ=WJ+CW(I)
C233 CONTINUE
C234 DO 4675 I=1,10
C235 CX(I)=CW(I)/WJ
C236 CONTINUE
C237 PC=100*FLOAT(HMAX)/FLOAT(NN)
C238 IF (LU(3).EQ.1) GO TO 4700
C239 WRITE (LUO,4600) (CW(I),I=1,10),SMAX,PC
C240 FORMAT (1H,10F6.1,F7.4,F7.2)
C241 4600 CONTINUE
C242 PS=100*FLOAT(NS)/FLOAT(NN)
C243 PCC=100*FLOAT(HMAX)/FLOAT(NN)
C244 DO 4800 LM=1,4
C245 PP(LM)=100*FLOAT(IPO(MAXJ,MAXI,LM))/FLOAT(NN)
C246 CONTINUE
C247 IF (LU(3).EQ.1) GO TO 4950
C248 WRITE (LUO,4043)
C249 4043 FORMAT (//)
C250 WRITE (LUO,4900) PCC,NN,PS,(PP(I),I=1,4)
C251 4900 FORMAT (//,4PERCENT CORRECT: "F6.2" %)
C252 1/ MINUTES SCORED: "16
C253 2/ PERCENT SLEEP: "F6.2" %/
C254 3/ "F6.2" %

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0255 4950 IF (NM(4).EQ.0) GO TO 5002
0256     VM(4)=V(NM(4))*((MAXJ-1)/27-1)
0257 5002 IF (NM(2).EQ.0) GO TO 5004
0258     VM(3)=V(NM(3))*((MOD((MAXJ-1),27)/9-1)
0259 5204 IF (NM(2).EQ.0) GO TO 5006
0260     VM(2)=V(NM(2))*((MOD((MAXJ-1),9)/3-1)
0261 5206 IF (NM(1).EQ.0) GO TO 5008
0262     VM(1)=V(NM(1))*((MOD((MAXJ-1),3)-1)
0263 5008 WRITE (LUO,5M10) (V(I),I=1,10),SSMAX,PCC
0264 5010 FORMAT (1H,10F5.1,F6.3,F6.2)
0265     IF (LU(3).EQ.0) GO TO 9053
0266     DO 9040 I=1,4
0267     IF (NM(I).EQ.0) GO TO 9040
0268     NM(I)=NM(I)+1
0269     IF (NM(1).GT.10) NM(1)=1
0270 9040 CONTINUE
0271     GO TO 600
0272 9050 WRITE (LUI,3009)
0273 0809 FORMAT (' MORE? -')
0274 0874 READ (LUI,0850) IANS
0275 0893 FORMAT (A2)
0276     IF (IANS.EQ.2HVE) GO TO 545
0277 9000 STOP 7777
0278 9900 WRITE (LUI,9990) IER
0279 9901 STOP 1
0280 9910 WRITE (LUI,9990) IER
0281 9920 STOP 2
0282 9920 WRITE (LUI,9990) IER
0283 9930 STOP 3
0284 9990 FORMAT (' *** ERROR-10' // ' *** ')
0285 9999 STOP
0286     END
0287     ENDS

```

APPENDIX 2

For Vitalog IM6100 microprocessor

00010 1-00004 IS ON CP00234 USING 00000 BLKS R-0000

0001 /ACTIC00P

0002 /RECORDS OUTPUT OF ACTIGRAM TRANSDUCER AND PHOTOCELL
0003 /RESOLUTION=1 MINUTE, DURATION=47HR.28MIN
0004 /TIME CODE EACH MINUTE THRU L.E.D.

0005 /AUTHOR: JOHN WEBSTER

0006 STORE = MAX I STORE

0007 /PAGE 0

0008 *0

0009 FTHADP. 0 /INTRPT RETURN ADDR
0010 INTRPT. JTP /INTRPT PNTR

0011 /AUTOMARK REGISTERS

0012 #13 0 /RESERVED FOR A/D. . .
0013 A13. 0 /BUFFER POINTER
0014 A14. 0 /RESERVED FOR DIFF. . .
0015 A15. 0 /SCORE POINTERS
0016 A16. 0 /DATA STORE POINTER
0017 DATAP. 0

0018 /INTERPT SERVICE ROUTINE

0019 #26 /INTRPTV. DCA ACSAVE /SAVE REGISTERS

0020 RAL
0021 DCA LKSAVE

0022 PCRA
0023 DCA CPASAV

0024 JMS GETACT /GET ACTIVITY SCORE
0025 TAD CRASPV /PESTORE REGISTERS

0026 WYRA
0027 CAF

0028 TAD LKSAVE

0029 RAR ACSAVE

0030 TAD
0031 ICA
0032 JTP I PTHADR

0033 /ACTIVITY SCORE SET-UP

0034

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0045

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0050

0051

0053	045	1113	TAP	AMRD	/SET UP PIE FOR A /D
0054	046	CS05	WCPA		/START WITH CH.1 (BIAS)
0055	047	7201	CLA IAC		
0056	048	3046	JMS	A2D	
0057	049	7041	CIA	BIAS	/NEGATE AND SAVE
0058	050	3121	BCA	A2D	/THEN CH.0 (ACT)
0059	051	4066	JMS	BIAS	/FIND DIFFERENCE
0060	052	1171	TAP	BIAS	/PAKE INTO BUFFER
0061	053	7413	BCA I	A13	/RESET BUFFER ENTP. . .
0062	054	1013	TAP	A13	/IF AT END (E0B)
0063	055	1114	TAP	STEND	
0064	056	7640	SZA CLF		
0065	057	5064	JMP	.+3	
0066	058	1111	TAP	STKBEG	
0067	059	3013	BCA	A13	
0068	060	5444	JMP I	PEADAD	

ANALOG TO DIGITAL CONVERSION

0069	061	7407	HLT		/CHAN. SELECT
0070	062	0501	WPIE1		
0071	063	7200	CLA ILL		/SET UP BACKUP CNTG
0072	064	1115	TAP	MCNT	
0073	065	3116	BCA	MCNTR	/START CONVERSION
0074	066	6511	WPIE2		/DONE (EOC)?
0075	067	6513	SKIP2		
0076	068	7410	SAP	DONE	
0077	069	5073	JMP	MCNTR	/NO. INCR. BACKUP
0078	070	2116	BCA	.-4	/YES
0079	071	5074	JMP	PEAD1	/MASK GARBAGE &
0080	072	6500	AND	X377	/EXIT
0081	073	0117	JMP I	A2D	
0082	074	5466			

CONSTANTS AND VARIABLES

0083	075	104	MAXEP.	0	/ACCUMULATES MAXIMAL EPOCH SCORE
0084	076	105	LITE.	0	/HOLDS LITE LEVEL VALUE
0085	077	106	ACSAVE.	0	/SAVES AC DURING INTPT
0086	078	107	LKSAVE.	0	/SAVES LINK DURING INTPT
0087	079	108	CPASAV.	0	/SAVES CRA DURING INTPT
0088	080	109	STKBEG.	547	/POINTS TO ACT SCORE BUFFER
0089	081	110	ERADR.	0	
0090	082	111	AMRD.	201	/INITIAL CRA VALUE
0091	083	112	STKEND.	7221	/END OF ACT SCORE BUFFER
0092	084	113	MCNT.	7766	/TIME DELAY FOR A/D
0093	085	114	MCNTR.	0	/COUNTER FOR TIME DELAY
0094	086	115	X377.	377	/USED TO MASK A/D CONV
0095	087	116	MS.	-6	
0096	088	117	BIAS.	0	/HOLDS TRANS. BIAS VALUE
0097	089	118	BJOPO.	4220	/INITIAL CPB VALUE
0098	090	119	BARBEG.	677	/POINTS TO START OF RECORDER MEM.

0107	125	0000	MINUT.	0	/MINUTE COUNT
0108	126	0000	TCODE.	0	/TIME CODE
0109	127	7775	MS.	-3	
0110	130	0000	GPPS.	0	/COUNTER FOR TIME CODE
0111	131	0000	CCNTP.	0	
0112	132	7773	MS.	-5	
0113	133	0000	TCNTP.	0	
0114	134	0000	CODE1.	0	/TIME CODE '0' OR '1'
0115	135	0000	TFLAG.	0	/TIME CODE FLAG
0116	136	7742	M30.	-30	
0117	137	0000	MINDIV.	0	/MINUTE DIVIDER
0118	140	0000	EPSCN1.	0	/ACCUMULATES EPOCH SUM
0119	141	0000	DIFSUM1.	0	/ACCUMULATES DIFSCP SUMS
0120	142	7610	M120.	-120	
0121	143	0000	EPDIV.	0	/EPOCH DIVIDER
0122	144	0000	SUM14.	0	/ACCUMULATES SUM TO 4
0123	145	7774	M4.	-4	
0124	146	0000	CNT4.	0	/COUNTS 4
0125	147	0177	X177.	177	/MASK FOR DIFSCP
0126	150	7700	X7700.	7700	
0127	151	0000	DATAPD.	0	/HOLDS DATA PRIOR TO STOPE
0128	152	0600	CODET.	CODET	/POINTS TO TIME CODE RTN
0129	153	0400	DIFSC.	DIFSCP	/POINTS TO DIFSCP RTN
0130	154	0000	CRATIF.	0	/TEMP CRA STOPE
0131	155	1000	FLD1.	1000	/ACRA TO GET FIELD 1
0132	156	2001	HE11M.	2001	/- END OF FIELD
0133	157	7776	M2.	-2	
0134	160	7766	M10.	-10	
0135	161	7600	T200.	7600	/ACRA TO WAIT
0136	162	4000	Q4000.	4000	/HOLDS MOST RECENT SUM4
0137	163	0000	LATEST.	0	/POINTS TO DIFSCP BUFFER
0138	164	0557	BUFLOC.	557	/BUFFER LOC
0139	165	0000	BUFN.	0	
0140	166	0000	M10US.	0	
0141	167	0000	OFLOW.	0	
0142	170	0000	PRDCT.	0	/POINTS TO STORE PTN
0143	171	0640	STOPE.	STORES	
0144	172	0000	DIFOUT.	0	
0145	173	0000	BUF.	0	
0146	174	7765	M11.	-11	
0147	175	7770	M8.	-8	
0148	176	7777	M1.	-1	
0149	177	0077	X77.	77	
0150					
0151					
0152					
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0155					
0156					
0157					
0158					
0159					

0215	261	3105	DCA	MINOT	/ENTER EACH EPOCH
0216	262	3140	DCA	EPD1V	
0217	263	3141	DCA	DFSUM	
0218	264	3142	DCA	M120	
0219	265	3143	DCA	EPD1V	/ENTER EACH FOUR A/D'S
0220	266	3144	DCA	SUM4	
0221	267	3145	TAD	M4	
0222	270	3146	DCA	CNT4	
0223	271	3135	TAD	TFLAG	
0224	272	7640	SZA CLA	CODETS	
0225	273	4552	JMS I		
0226	274	6001	ION	/ENTER EACH A/D	
0227	275	7300	CLA CLL	A13	
0228	276	1013	TAD	A14	/IS A/D BUFFER EMPTY?
0229	277	7041	CIA	NEW	/YES. ENTER WAIT STATE
0230	300	1014	TAD		
0231	301	7440	SZA	04000	
0232	302	5315	JMP		
0233	303	6504	PCRA		
0234	304	7421	IDL		
0235	305	7501	MDA		
0236	306	1162	TAD		
0237	307	6505	WCRG		
0238	310	7701	ACL		
0239	311	6505	WCPA		
0240	312	7000	NOP		
0241	317	7000	NOP		
0242	319	5275	JMP	EACH	/NO. READ NEXT VALUE
0243	315	7300	CLA CLL	A14	/AND SUM TO 4
0244	316	1414	TAD I	SUM4	/RESET BUFFER IF AT END
0245	317	1145	TAD	SUM4	
0246	310	3144	DCA	A14	
0247	321	1014	TAD	STKEND	
0248	322	1114	TAD	.+3	
0249	323	7640	SZA CLA	STKREG	/SUMED 4 YET?
0250	324	5327	JMP	A14	/NO
0251	325	1111	TAD	CNT4	/YES. FIND DIFF. SCP.
0252	326	3014	DCA	EACH	
0253	327	2146	ISZ	SUM4	
0254	330	5275	JMP	DFSOP	
0255	331	1144	TAD	DFSOP	
0256	332	4553	JMS I	DFSOP	
0257	333	7100	CLL	DFSOP	
0258	334	1141	TAD	DFSOP	
0259	335	1141	SZL	DFSOP	
0260	336	7240	STA	DFSOP	
0261	337	3141	DCA	DFSOP	/TRUNCATE IF TOO LARGE
0262	340	2143	ISZ	EPD1V	/IS IT AN EPOCH YET?
0263	341	5266	JMP	FOUP	/NO
0264	342	1141	TAD	DFSOP	/YES. FIND MAXIMAL. . .
0265	343	7110	CLL PAR	DFSOP	/EPOCH EACH MINUTE
0266	344	7041	CIA		
0267	345	1104	TAD	NAMEP	

0269	347	JMP	.+4	/NO
0270	350	TAP	DFSUM	/YES. REPLACE OLD
0271	351	CLL	MAXEP	
0272	352	PCA	MINDIV	/IS IT A MINUTE YET?
0273	353	ISZ	EPOCH	/NO
0274	354	JIF		/YES. PEAK LITE LEVEL
0275	355	IOF	.+5	/EPOCH A/N. CH.2
0276	356	TAP	A2B	
0277	357	JIG	DATUED	
0278	360	PCA		
0279	361	IOB	.+5	
0280	362	JIF		
0281	363	2		
0282	364	IOF		/AND STOPE IN RECODER
0283	365	IOF		/MEMORY
0284	366	IOF		/NOW GET MAXIMAL EPOCH
0285	367	STOPE		/AND STORE IT IN NEXT
0286	368	HLT	MAXEP	/MEMORY LOCATION
0287	369	TAP	DATUED	
0288	371	PCA		
0289	372	IOB		
0290	373	STOPE		
0291	374	HLT		
0292	375	IF	FINIT	
0293				
0294				
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ADDRESS	DATA	INSTR	OPCODE	PC	PC+1	PC+2	PC+3	PC+4	PC+5	PC+6	PC+7	PC+8	PC+9	PC+10	PC+11	PC+12	PC+13	PC+14	PC+15	PC+16	PC+17	PC+18	PC+19	PC+20	PC+21	PC+22	PC+23	PC+24	PC+25	PC+26	PC+27	PC+28	PC+29	PC+30	PC+31	PC+32	PC+33	PC+34	PC+35	PC+36	PC+37	PC+38	PC+39	PC+40	PC+41	PC+42	PC+43	PC+44	PC+45	PC+46	PC+47	PC+48	PC+49	PC+50	PC+51	PC+52	PC+53	PC+54	PC+55	PC+56	PC+57	PC+58	PC+59	PC+60	PC+61	PC+62	PC+63	PC+64	PC+65	PC+66	PC+67	PC+68	PC+69	PC+70	PC+71	PC+72	PC+73	PC+74	PC+75	PC+76	PC+77	PC+78	PC+79	PC+80	PC+81	PC+82	PC+83	PC+84	PC+85	PC+86	PC+87	PC+88	PC+89	PC+90	PC+91	PC+92	PC+93	PC+94	PC+95	PC+96	PC+97	PC+98	PC+99	PC+100	PC+101	PC+102	PC+103	PC+104	PC+105	PC+106	PC+107	PC+108	PC+109	PC+110	PC+111	PC+112	PC+113	PC+114	PC+115	PC+116	PC+117	PC+118	PC+119	PC+120	PC+121	PC+122	PC+123	PC+124	PC+125	PC+126	PC+127	PC+128	PC+129	PC+130	PC+131	PC+132	PC+133	PC+134	PC+135	PC+136	PC+137	PC+138	PC+139	PC+140	PC+141	PC+142	PC+143	PC+144	PC+145	PC+146	PC+147	PC+148	PC+149	PC+150	PC+151	PC+152	PC+153	PC+154	PC+155	PC+156	PC+157	PC+158	PC+159	PC+160	PC+161	PC+162	PC+163	PC+164	PC+165	PC+166	PC+167	PC+168	PC+169	PC+170	PC+171	PC+172	PC+173	PC+174	PC+175	PC+176	PC+177	PC+178	PC+179	PC+180	PC+181	PC+182	PC+183	PC+184	PC+185	PC+186	PC+187	PC+188	PC+189	PC+190	PC+191	PC+192	PC+193	PC+194	PC+195	PC+196	PC+197	PC+198	PC+199	PC+200	PC+201	PC+202	PC+203	PC+204	PC+205	PC+206	PC+207	PC+208	PC+209	PC+210	PC+211	PC+212	PC+213	PC+214	PC+215	PC+216	PC+217	PC+218	PC+219	PC+220	PC+221	PC+222	PC+223	PC+224	PC+225	PC+226	PC+227	PC+228	PC+229	PC+230	PC+231	PC+232	PC+233	PC+234	PC+235	PC+236	PC+237	PC+238	PC+239	PC+240	PC+241	PC+242	PC+243	PC+244	PC+245	PC+246	PC+247	PC+248	PC+249	PC+250	PC+251	PC+252	PC+253	PC+254	PC+255	PC+256	PC+257	PC+258	PC+259	PC+260	PC+261	PC+262	PC+263	PC+264	PC+265	PC+266	PC+267	PC+268	PC+269	PC+270	PC+271	PC+272	PC+273	PC+274	PC+275	PC+276	PC+277	PC+278	PC+279	PC+280	PC+281	PC+282	PC+283	PC+284	PC+285	PC+286	PC+287	PC+288	PC+289	PC+290	PC+291	PC+292	PC+293	PC+294	PC+295	PC+296	PC+297	PC+298	PC+299	PC+300	PC+301	PC+302	PC+303	PC+304	PC+305	PC+306	PC+307	PC+308	PC+309	PC+310	PC+311	PC+312	PC+313	PC+314	PC+315	PC+316	PC+317	PC+318	PC+319	PC+320	PC+321	PC+322	PC+323	PC+324	PC+325	PC+326	PC+327	PC+328	PC+329	PC+330	PC+331	PC+332	PC+333	PC+334	PC+335	PC+336	PC+337	PC+338	PC+339	PC+340	PC+341	PC+342	PC+343	PC+344	PC+345	PC+346	PC+347	PC+348	PC+349	PC+350	PC+351	PC+352	PC+353	PC+354	PC+355	PC+356	PC+357	PC+358	PC+359	PC+360	PC+361	PC+362	PC+363	PC+364	PC+365	PC+366	PC+367	PC+368	PC+369	PC+370	PC+371	PC+372	PC+373	PC+374	PC+375	PC+376	PC+377	PC+378</
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LNXT.	ISZ	BUFN	LNXT.	ISZ	BUFN
0377 461 2165	JNP	LX10	0378 462 5240	CLL	MINLO
0379 463 7100	TAD	MINLO	0380 464 1340	CIA	MINLO
0381 465 7041	DCA	MINLO	0382 466 3340	SZL	MINHI
0383 467 7430	IAC	MINHI	0384 470 7001	TAD	MINHI
0385 471 1341	CIA	PRDLO	0386 472 7041	DCA	PRDLO
0387 473 3341	SZL	PRDLO	0388 474 7100	IAC	PRDHI
0389 475 1342	TAD	PRDHI	0390 476 1340	TAD	MINHI
0391 477 3342	DCA	MINHI	0392 500 7430	SZL	PRDHI
0393 501 7001	IAC	PRDHI	0394 502 1343	TAD	MINHI
0395 503 1341	TAD	MINHI	0396 504 3343	DCA	PRDHI
0397 505 1164	TAD	PRDHI	0398 506 3016	TAD	PRDHI
0399 507 1164	TAD	PRDHI	0400 510 3015	DCA	PRDHI
0401 511 1174	TAD	PRDHI	0402 512 3165	TAD	PRDHI
0403 513 1415	TAD	PRDHI	0404 514 3173	DCA	PRDHI
0405 515 1163	TAD	PRDHI	0406 516 3416	TAD	PRDHI
0407 517 1173	TAD	PRDHI	0408 520 3163	DCA	PRDHI
0409 521 2165	ISZ	PRDHI	0410 522 5313	JNP	PRDHI
0411 523 1342	TAD	PRDHI	0412 524 7510	SPA	PRDHI
0413 525 7041	CIA	PRDHI	0414 526 7002	BSW	PRDHI
0415 527 7004	RAL	PRDHI	0416 530 0147	AND	PRDHI
0417 531 5600	JNP	PRDHI	0418 531 5600	JNP	PRDHI
0419 531 5600	JNP	PRDHI	0420 531 5600	JNP	PRDHI
0421 531 5600	JNP	PRDHI	0422 540 0000	JNP	PRDHI
0423 541 0000	JNP	PRDHI	0424 542 0000	JNP	PRDHI
0425 543 0000	JNP	PRDHI	0426 544 0000	JNP	PRDHI
0427 545 0000	JNP	PRDHI	0428 546 0000	JNP	PRDHI
0429 547 0000	JNP	PRDHI	0430 548 0000	JNP	PRDHI

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0485	600	7402	HLT	/GENERATE TIME CODE (OCTAL MINUTES)	
0486	601	2133	ISZ	/ENTER EACH 4 A/D'S IF TFLAG SET	
0487	602	5225	JMP	/TIME FOR ANOTHER DIGIT	
0488	603	1160	TAD	/NO	
0489	604	3133	DCA		
0490	605	2131	ISZ	/YES, START OCTAL GROUP	
0491	606	5215	JMP	/NO, OUTPUT DIGIT	
0492	607	1145	TAD	/YES, SKIP DIGIT	
0493	610	3151	DCA		
0494	611	2130	ISZ	/4 OCTAL GROUPS YET?	
0495	612	7410	SKP		
0496	613	3135	DCA	/YES, CLEAR TFLAG	
0497	614	5225	JMP	/LITE ON	
0498	615	6506	STLITE		
0499	616	1126	TAD	/GET NEXT MSB	
0500	617	7104	CLL PAL		
0501	620	3126	DCA		
0502	621	7430	SZL	/BINARY 1 OR 0?	
0503	622	1127	TAD	/1:HOLD LITE 5 UNITS	
0504	623	1176	TAD	/0:HOLD LITE 1 UNIT	
0505	624	3134	DCA		
0506	625	1134	TAD	/HOLD LITE ON?	
0507	626	7500	SMA		
0508	627	6507	CLLITE	/NO, CLEAR IT	
0509	630	7001	IAC	/YES	
0510	631	3134	DCA		
0511	632	5600	JMP I		
0512					
0513					
0514					
0515					
0516					
0517					
0518					
0519					
0520					
0521	640	7402	HLT	/STORE DATA	
0522	641	6504	PCRA	*640	
0523	642	3154	DCA	STORES.	
0524	643	1124	TAD		
0525	644	7650	SNA CLA		
0526	645	5251	JMP		
0527	646	1155	TAD		
0528	647	6505	UCRA		
0529	650	7300	CLA CLL		
0530	651	1151	TAD		
0531	652	3417	DCA I		
0532	653	1154	TAD		
0533	654	6505	UCRA		
0534	655	7300	CLA CLL		
0535	656	1017	TAD		
0536	657	1156	TAD		
0537	658	7650	SNA CLA		
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0539	662	2240	ISZ	STORES	/NO, RETURN +1
0540	663	5640	JMP	STORES	/YES, WHICH FLD?
0541	664	1124	TAD	FLDFLG	
0542	665	7440	SZA		
0543	666	5640	JMP	STORES	/FLD 1, RTRN 2 END
0544	667	2124	ISZ	FLDFLG	/FLD 0, SWITCH TO FLD 1
0545	670	7240	STA	DATAP	
0546	671	3017	DCA	STORES	/RESET DATA PNTR TO TOP
0547	672	2240	ISZ	STORES	
0548	673	5640	JMP	STORES	/RTRN +1
0549					
0550					
0551					/RECORDER MEMORY
0552					/MAXIMAL EPOCH ACTIVITY SCORE AND
0553					/LIT LEVEL FOR EACH MINUTE ARE
0554					/STORED IN ALTEPHATE MEMORY LOCS
0555					/FROM LOC. 700 TO 5777 (FLD 0)
0556					/AND 10000 TO 15777 (FLD 1)
0557					
0558					
0559					*700
0560					
0561					
0562					\$33
0563					

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