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Identification of ca	vernous nerves (CI	Ns) and prostate sur	gical margins are tw	vo critical detei	minants for the outcome of radical		
prostatectomy. Currently there is no real time cancer diagnosis technology available when doing the prostate cancer tumor							
removal surgery.	Our group is develo	ping a miniaturized	Coherent Anti-Stoke	es Raman scat	tering (CARS) system to identify		
malignant prostate	e tissue and tumor r	nargin without optica	al labels or contrast	agents. We ha	ave successfully finished the design		
of a high precision, label-free microendoscope based on the integration of CARS, microelectromechanical systems (MEMS),							
and four-wave mix	ting (FWM) noise si	uppression technolo	gies. The 14 mm tr	ansversal dian	neter of the round-shaped CARS		
microendoscope p	probe paves the way	y towards future har	ndheld multimodal C	ARS imaging f	for real time minimally invasive		
prostate cancer diagnosis. We have examined the feasibility of multimodal prostate imaging with CARS and second harmonic							
generation (SHG) using patient specimen and mouse models. The next step will be in vivo imaging and algorithm development							
with the all-fiber microendoscope system. This work presents a significant milestone in CARS endoscopy development using							
micro optics and MEMS mirror which greatly reduce the size of CARS endoscopy while keeping high imaging definition quality.							
15. SUBJECT TERMS							
coherent anti-Stokes Raman scattering; endoscopy; endomicroscopy; fiber optics; micro-electromechanical systems							
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1. Introduction

Identification of cavernous nerves (CNs) and prostate surgical margins are two critical determinants for the outcome of radical prostatectomy. Coherent Anti-Stokes Raman scattering (CARS) is a label-free imaging technique which can differentiate prostate cancer tissues and cavernous nerves (CNs) based on intrinsic macromolecular contrast without the use of any labeling agents. One major obstacle for intraoperative and surgical application of CARS is the bulky size of the original CARS system which was built on free space optics. To overcome this hurdle, we replaced the bulk optics with their fiber optic counterparts to build an all-fiber-based CARS microendoscope in order to be able to visualize prostate and cancer tissues during prostatectomy and evaluate CARS imaging for prostate cancer tissue differentiation.

2. Keywords

Coherent anti-Stokes Raman scattering; non-linear optics; endomicroscopy; fiber optics; microelectromechanical systems; prostate cancer; prostatectomy, *in vivo* cancer differentiation; optical diagnostics; medical imaging; image quantification; machine learning

3. Overall Project Summary

The specific aims have not been significantly modified from the original approved statement of work. Aim 1 is the development of a miniaturized device by refining the original, bulky CARS system into a compact all-fiber CARS microendoscope by replacing the original, bulky free-space optics with their fiber optic counterparts. Because of the miniaturized size and minimization of nonlinear effects, we hypothesize that our full-fiber microendoscope can image the CH₂ chemical bonds of macromolecules in tissues and allow the *in vivo* identification of cavernous nerves and differentiation of prostate cancer and surgical margins which will be tested in Aim 2.

Aim 1: To refine our existing CARS microendoscope into a fiber device for *in vivo* cancer imaging.

A. Refine laser, detection, and data acquisition (DAQ) subsystems with fiber optic components.

B. Develop a fiber probe based on microelectromechanical systems (MEMS) technology and consisting of a polarization maintaining fiber, a MEMS scanning mirror, and micro-optics.

We have refined our original bulky free-space optical CARS system into a compact all-fiber CARS microendoscope and finished the development of the fiber probe (Aim 1A and Aim 1B) in Year 1. We have also tested the signal collection efficiency with a single fiber (SMF28) and a customized fiber bundle composed of 6 multimode fibers (MMFs) with the same polarization control scheme as previously published [1]. The work has led to three conference proceedings papers [2-4].

C. Assemble and characterize the all-fiber-based CARS microendoscope system.

In Year 2, we presented the design principle of our miniaturized probe at the 2014 conference of Society of Photo-Optical Instrumentation Engineers (SPIE) Photonics West and the presentation has led to publication of a conference proceedings paper [4], and a full journal paper has been submitted to Biomedical Optics Express [5]. Figure 1 shows the assembled design of the fiber-based CARS microendoscope probe. The specifications are given in Table 1. The exit pupil diameter of the collimator system is designed to match the diameter of the MEMS mirror and the entrance pupil diameter of the micro-endoscope system. For the micro-endoscope part, the numerical aperture is 0.73, FOV is160 μ m x 160 μ m, working distance is 0.37 mm, and designed spatial resolution is 1 micron. The total length of our CARS micro-endoscope is 40.5 mm and the achromatic wavelengths are 450nm, 663nm, 817nm, and 1064nm. To enhance the signal collection efficiency, the micro-endoscope system is designed with achromatic wide angle keplerian telescope beam expander system

delivering the collimated light to maximum cover the back aperture of light focusing system in order to increase the NA of the micro-endoscope.



Figure 1. Assembled design of the fiber-based CARS microendoscope probe.

Basic System Descriptions	Parameters		
Excitation Wavelength range for delivery	817nm(pump), 1064nm(stokes)		
Signal wavelength to be collected from tissue	663nm(CARS) 500nm(TPEF) 400nm(SHG)		
Input aperture (diameter of exit pupil)	Agree with the dimension of MEMS scanning mirror 1.12mm		
Distance from the MEMS mirror to objective lens	4mm		
NA(after immersion in water)	0.75		
Actual resolution	0.78 micron or smaller		
Field of view	160µmx160µm		

Table 1.	Basic system	parameters	of CARS	microend	oscope	probe

High spatial overlap on sample image side is achieved with 0.46 μ m resolution at the center field of view and 0.57 μ m at the marginal field of view, the 'ideal' resolution is half the goal to achieve for the as-built system. Misalignment in the microendoscope system would generate mismatch between the pump and Stokes beams and create difficulty for CARS signal generation. Tolerance budget is used to ensure that each component is manufactured adhering strictly to the specifications and integrated well into the CARS microendoscope probe

with the highest precision possible. Monte Carlo simulation of the CARS microendoscope probe was performed using the following parameters listed in Table 2.

Radius	Airspace and glass thickness	Index tolerance	V#	Surface Irregularity	Element wedge	Element tilt	Element decenter
0.1 mm	0.025mm	0.0005	0.8%	0.25 fringe	8 μ m TIR	0.001 radians	20 <i>µ</i> m

Table 2. Tolerance budget of CARS micro-endoscope probe.

Wave front quality of the fiber collimator was evaluated at 785 nm using an Optocraft wave front sensor. The airspace between the fiber and optics was adjusted to achieve wave front quality smaller than 0.05 λ RMS (root mean square) at 785 nm, which is within the design tolerance 0.5 λ at 785 nm. Figure 2(a) and (b) present the manufactured product of CARS collimator and fiber cable which have a 900 micron furcation blue tube and a 2.5 mm diameter stainless steel ferrule, Fig 2(c) presents the CARS microendoscope probe lens, Figure 1(d) presents the experimental setup for the CARS microendoscope resolution testing, while Figure 2(e), (f), and (g) present the spatial resolution result from microendoscope imaging testing. The resolving power of the microendoscope lens was investigated by acquiring transmission images of a USAF resolution test target (Edmund Optics). Lights of different wavelengths (575nm, 660nm, and 850nm) were used to test the resolution as shown in the figure. The USAF resolution target was placed at the focus position of the microendoscope barrel, the 20 mm objective lens and image receiver (Samsung phone) were used to acquire a high resolution targeted image. The smallest element, 3 in the 9th group, was resolved by the microendscope. It has a line spacing of 645 line pairs/mm, corresponding to a line width of approximately 0.78 µm. There is no distortion in the shape of the individual lines in the image except for a conical defocus deformation in the 660nm resolution image in which the transmission resolution image is not at the center of the objective.



Figure 2. (a) PM1300 fiber part of the CARS microendoscope probe; (b) Collimator part of CARS microendoscope probe; (c) Microendoscope part of the CARS probe; (d) Resolution experiment setup of CARS microendoscope; (e),(f), and (g) Resolution measurement (575nm, 660nm, 850nm respectively) from microendoscope imaging testing.

Aim 2: To evaluate the ability of our CARS microendoscope to image cavernous nerves and prostate surgical margins *in vivo* using intrinsic CH₂-based molecular contrast.

A. Evaluate the utility of the CARS microendoscope to image patient surgical specimens ex vivo and transgenic mouse model for prostate cancer (TRAMP) mice in vivo.

Human prostate tissues were obtained from the Houston Methodist Hospital Tissue Bank. These specimens were from patients undergoing radical prostatectomy and snap frozen immediately after tissue removal. We thawed the tissues at room temperature approximately 30 min before imaging. Figure 3 represents the typical imaging result of CARS and second harmonic generation (SHG) for prostate gland and the surrounding stroma with the microscope setup. For CARS imaging, we use 817 nm and 1064 nm as pump and Stokes wavelength and collect CARS emissions at 640-680 nm. Cell nuclei are shown as dark round spots in Figure 3A (vellow arrow). Our previous study has shown that real-time differentiation of cancerous glands from normal prostate tissue can be achieved with cellular features such as cell neighbor distance, size and shape of nuclei, which are illustrated by CARS imaging [6]. Previously, we have also shown that collagen deposition in tissues can be illustrated by SHG imaging [7]. In prostate cancer tissue, Type I collagen fibers in stroma are shown by SHG signals collected at 405-415 nm (Fig. 3B). Combining the two modalities of CARS and SHG, cancer cell invasion into surrounding stroma can be further illustrated, which is critical for the grading of prostate cancer. To incorporate the multi-modal label-free imaging technology as a real-time diagnostic platform, size of the miniaturized optics is a critical factor as the fiber probe has to fit into ports of robotic arms and go through the incisions in the patient's abdomen. Resolution is the other critical factor which is needed for clear visualization of cell nuclei with sizes around 5-10 µm. With an estimated resolution of 1 µm, we expect to detect and differentiate normal and diseased prostate glands and stroma based on cellular feature analysis at the surgical margin.



Figure 3. CARS and SHG images of prostate cancer tissue taken under microscope setup. (A) CARS image. Yellow arrow points to a cell nucleus. (B) SHG image. Scale bar: 50µm.

We have also tested the feasibility of using TRAMP mice for CARS and SHG imaging of prostate cancer with microscope setup. The development and function of the prostate in mice are comparable to that in humans, so that mice are an ideal subject for our experiments. TRAMP mice are prostate cancer transgenic mice and C57/BL6 mice are the wildtype counterparts, both of them will be ordered from Jackson labs. The surgery and imaging process was performed on mice at week 17 and week 20. Figure 4 shows the CARS and SHG images of prostate tumor developed in TRAMP mice, and Figure 5 shows the normal prostate imaging result. The cancer cells are clearly illustrated in mouse prostate cancer tissue. Yellow arrow indicates a typical cell nucleus in Figure 4A. Normal prostate tissue is mostly composed of stroma tissue which is clearly visualized by SHG imaging. Yellow arrow indicates a typical fibrous collagen structure in Figure 5B. Current results show that CARS and SHG imaging can differentiate prostate cancer tissue from normal with mouse model. Later experiments will be carried out with assembled fiber system and live animals for algorithm development and validation in Aim 2B and Aim 2C.



Figure 4. CARS and SHG images of mouse prostate cancer tissue with microscope setup. (A) CARS image. Yellow arrow points to a cell nucleus. (B) SHG image. Scale bar: 25µm.



Figure 5. CARS and SHG images of normal mouse prostate tissue with microscope setup. (A) CARS image. (B) SHG image. Yellow arrow points to a fibrous structure of collagen. Scale bar: 50µm.

We will complete Aim 2B and Aim 2C in year 3.

B. Develop algorithms for image quantification and characterization of prostate and periprostatic tissues in TRAMP mice.

C. Validate the performance of microendoscope imaging and image analysis algorithms to identify prostate and periprostatic tissue in vivo.

4. Key Research Accomplishments

- 1. Examined fiber-based imaging by an endomicroscopy prototype with customized fiber bundle composed of 6 multimode fibers and 18 multimode fibers
- 2. Examined the feasibility of using TRAMP mice for CARS imaging of prostate cancer
- 3. Assembly and testing of the miniaturized microendoscope probe as originally proposed

5. Conclusion

We have successfully finished the design of a high precision, label-free microendoscope based on the integration of CARS, MEMS, and FWM noise suppression technologies. The high spatial resolution (0.78 μ m) and distortion-free images of CARS microendoscope are obtained from USAF target. Image testing results show our microendoscope probe meet the expected computational modeling design specification with good optical alignment, and at the same time, unwanted fiber-generated non-resonant FWM noise is eliminated using our polarization scheme applied in this probe optical system. 14 mm transversal diameter of the round-shaped CARS microendoscope probe paves the path towards a future handheld multimodal CARS imaging for real-time, minimally invasive prostate cancer diagnosis. We have examined the feasibility of multimodal prostate imaging with CARS and SHG using patient specimens and mouse models. The next step will be *in vivo* imaging and algorithm development with an all-fiber microendoscope system.

6. Publication, Abstracts, and Presentations

- Zhengfan Liu, Zachary A. Satira, Xi Wang, Xiaoyun Xu, Xu Chen, Kelvin Wong, Shufen Chen, Jianguo Xin, Stephen T.C. Wong. Fiber bundle-based endomicroscopy prototype with two collection channels for simultaneous multimodal coherent anti-Stokes Raman scattering and second-harmonic generation imaging, Multiphoton Microscopy in the Biomedical Sciences XIV. Proceedings of the SPIE, 894814, 2014
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7. Inventions, Patents, and Licenses

Nothing to report

8. Reportable Outcomes

- 1) A miniaturized CARS probe has been designed and is being fabricated for *in vivo* identification of cavernous nerves and differentiation of prostate cancer and surgical margins.
- The prototype of fiber bundle-based endomicroscopy has been tested with two collection channels for simultaneous multimodal coherent anti-Stokes Raman scattering and second-harmonic generation imaging.

9. Other Achievements

- 1) This DOD award supports three postdoctoral trainees (Xu Chen, Xiaoyun Xu, and Xi Wang)
- 2) This award also provides research opportunities for one masters student (Olen Rambow, graduated Jun 2014) and one PhD student (Zhengfan Liu)

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Appendices

Our work has led to publication of two conference proceedings papers in the past funding year.



Paper Abstract

A Coherent Anti-Stokes Raman Scattering (CARS) microendoscope probe for early stage label-free prostate cancer diagnosis at single cell resolution is presented. The handheld CARS microendoscope probe includes a customized microelectromechanical systems (MEMS) scanning mirror as well as miniature optical and mechanical components. In our design, the excitation laser (pump and stokes beams) from the fiber is collimated, reflected by the reflecting mirror, and transmitted via a 2D MEMS scanning mirror and a micro-objective system onto the sample; emission in the epi-direction is returned through the micro-objective lens, MEMS and reflecting mirror, and collimation system, and finally the emission signal is collected by a photomultiplier tube (PMT). The exit pupil diameter of the collimator system is designed to match the diameter of the MEMS mirror and the entrance pupil diameter of the micro-objective system. The back aperture diameter of the microobjective system is designed according to the largest MEMS scanning angle and the distance between the MEMS mirror and the back aperture. To increase the numerical aperture (NA) of the micro-objective system in order to enhance the signal collection efficiency, the back aperture diameter of the micro-objective system is enlarged with an upfront achromatic wide angle Keplerian telescope beam expander. The integration of a miniaturized micro-optics probe with optical fiber CARS microscopy opens up the possibility of in vivo molecular imaging for cancer diagnosis and surgical intervention.

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PROCEEDINGS PAPER



Paper Abstract

Label-free multiphoton imaging is promising for replacing biopsy and could offer new strategies for intraoperative or surgical applications. Coherent anti-Stokes Raman scattering (CARS) imaging could provide lipid-band contrast, and second harmonic generation (SHG) imaging is useful for imaging collagen, tendon and muscle fibers. A combination of these two imaging modalities could provide rich information and this combination has been studied by researchers to investigate diseases through microscopy imaging. The combination of these two imaging modalities in endomicroscopy imaging has been rarely investigated. In this research, a fiber bundle consisted of one excitation fiber and 18 collection fibers was developed in our endomicroscopy prototype. The 18 collection fibers were divided into two collection channels with 9 fibers in each channel. These two channels could be used together as one channel for effective signal collection or used separately for simplifying detection part of the system. Differences of collection pattern of these two channels were investigated. Collection difference of central excitation fiber and surrounding 18 fibers was also investigated, which reveals the potential ability of this system to measure forward to backward (F/B) ratio in SHG imaging. CARS imaging of mouse adipocyte and SHG imaging of mouse tail tendon were performed to demonstrate the CARS and SHG tissue imaging performance of this system. Simultaneous CARS and SHG imaging ability of this system was demonstrated by mouse tail imaging. This fiber bundle based endomicroscopy imaging prototype, offers a promising platform for constructing efficient fiber-based CARS and SHG multimodal endomicroscops for label free intraoperative imaging applications.

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