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Individuals exercise and work in a	wide range	of environmental co	onditions (e.g	temper	ature, humidity, sun, wind, rain, and water).	
Depending on the environmental of	conditions ar	nd a person's metabo	lic rate and cl	lothing, e	exercise can accentuate heat gain or heat	
loss, causing body temperature to	rise or fall. I	Healthy humans nor	mally regulate	e body (c	ore) temperatures near 37°C at rest, and	
with environmental and/or exercis	e perturbation	ons, body temperatur	res can fluctua	ate betwe	een 35°C and 41°C without adverse health	
consequences. Fluctuations outsid	e that range	can be associated w	ith morbidity	and mort	ality. In this chapter, the term exercise	
refers to dynamic exercise, and tra	aining refers	to repeated days of	exercise in a s	specific n	nodality leading to adaptations. The term	
stress refers to environmental and	or exercise	conditions that tend	to influence th	he body's	heat content, and strain refers to the	
phys1ologtc consequences of stres	ss. The mag	nitude of stress and t	he resulting s	train depe	end on a complex interaction among	
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HUMAN WATER AND ELECTROLYTE BALANCE

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Summary

Among the greatest challenges to body water homeostasis is the imposition of prolonged exercise and environmental stress. Sweating results in water and electrolyte losses. Because sweat output often exceeds water intake, there is an acute water deficit that results in a hypertonic hypovolemia and intracellular and extracellular fluid contraction. Although water and electrolyte needs increase as a result of exercise, physiological and behavioral adaptations allow humans to regulate daily body water and electrolyte balance so long as food and fluid are readily available. Although there is presently no consensus for choosing one hydration assessment approach over another, deviations in daily fluid balance can be determined with the use of two or more markers, which should provide added diagnostic confidence when serial measures are made. Hypohydration increases heat storage by reducing sweating rate and skin blood-flow responses for a given core temperature. In addition, hypohydration increases the risk for heat exhaustion and is a risk factor for heat stroke. Aerobic exercise tasks can be adversely affected if hypohydration exceeds 2% of normal body mass, with the potential effect greater in warm environments and lesser in cool environments. Hyperhydration provides no thermoregulatory or exercise performance advantages over euhydration in the heat. Excessive consumption of hypotonic fluid over many hours can lead to hyponatremia. Marked electrolyte losses can accelerate the dilution and exacerbate the problem. Hyponatremia can be avoided by proper attention to diet and fluid needs.

Introduction

Humans typically maintain stable day-to-day body water and electrolyte balance so long as food and fluid are readily available (Institute of Medicine, 2005). The ability to detect and correct for water and electrolyte flux is essential considering the potential day-to-day imposition of physical activity and environmental stressors and the negative consequences of gross fluid and electrolyte imbalances on health and performance.

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Water (total body water) plays many unique and vital roles within the body. Water is the principal chemical constituent of the human body and serves as the solvent for biochemical reactions supporting cellular homeostasis (Institute of Medicine, 2005). Water is also essential to sustain cardiovascular volume, and serves as the medium for transport within the body by supplying nutrients and removing waste. Water has unique properties, such as high specific heat, which allow it to absorb metabolic heat within the body, thus playing a vital role in thermoregulation. In addition, cell hydration is an important signal to regulate cell metabolism and gene expression (Haussinger and Gerok, 1994).

For an average young adult male, total body water is relatively constant and represents 50–70% of body weight (Sawka, 1988). The distribution of total body water is divided into intracellular fluid (ICF) and extracellular fluid (ECF) compartments. The ICF and ECF contain ~67% and ~33% of total body water, respectively. The ECF is further divided into the interstitial and plasma spaces (Sawka, 1988). Figure 32.1 depicts these fluid compartments and common mechanisms for compartmental fluid exchange.

The hydration of lean body mass is fairly constant (~73% water) across the lifespan and independent of sex and ethnicity. As a result, variability in total body water is primarily due to differences in body composition (Institute of Medicine, 2005). For example, using the equation, total body water = $0.73 \times$ lean body mass + $0.1 \times$ fat mass (Institute of Medicine, 2005), two individuals of 90 kg and body compositions of 15% and 30% fat will have total



FIG. 32.1 Schematic of the approximate volume of water and mechanisms for exchange between plasma, interstitial fluid (ISF), and intracellular fluid (ICF) compartments. Example assumes total body water (TBW) of ~45L for a 70-kg individual. Adapted from Sawka (1988).

body water values of 57.2 L and 48.7 L, respectively. Thus, similar absolute total body water losses would result in a greater percentage of total body water losses for individuals with more body fat.

Water balance represents the net difference between water intake and loss. However, when losses exceed intakes. total body water is decreased. Within the course of a day, it is not uncommon to see wide deviations in hydration status. The most common type of dehydration (hypertonic hypovolemia) is caused by a net loss of hypotonic body fluids such as sweat, e.g. during heavy physical labor or exercise. For example, individuals may dehydrate during physical activity or exposure to hot weather because of fluid non-availability or a mismatch between thirst and body water losses (Costill, 1977; Sawka, 1992). In these instances, the person begins the task with normal total body water and dehydrates over a prolonged period. A different type of dehydration (isotonic dehydration) occurs as a result of illness (diarrhea, vomiting), exposure to extreme environments (cold, high altitude), injury (hemorrhage, burns), or use of certain medications (diuretics).

Fluid replacement is encouraged during physical activity to avoid excessive dehydration, as water losses that exceed approximately 2% of initial body mass have been repeatedly shown to compromise endurance performance capability (Sawka *et al.*, 2007). However, indiscriminate drinking of water and other electrolyte-poor beverages without consideration of need can have negative consequences. Hyponatremia is a clinical example of the consequences of overdrinking and can be produced by drinking in excess of volume necessary to restore total body water, and by drinking in excess of what is necessary to preserve electrolyte balance (Vrijens and Rehrer, 1999; Montain *et al.*, 2001).

This chapter reviews the physiology, needs, and assessment of human water and electrolyte balance. The extent to which water and electrolyte imbalances affect temperature regulation and exercise performance are also considered. Throughout the chapter, euhydration refers to normal body water content, hypohydration refers to a body water deficit, and hyperhydration to increased body water content. Dehydration refers to the dynamic loss of body water.

Physiology of Water and Electrolyte Balance

Net body water balance (loss = gain) is generally regulated well as a result of thirst and hunger drives coupled with free access to food and beverage (Institute of Medicine, 2005). This is accomplished by neuroendocrine and renal responses (Andreoli *et al.*, 2000) to body water volume and tonicity changes, as well as non-regulatory social-behavioral factors (Rolls and Rolls, 1982). These homeo-static responses collectively ensure that small degrees of hyper- and hypohydration are readily compensated for in the short term. Using water balance studies, Adolph (Adolph and Dill, 1938; Adolph, 1943) found that daily body water varied narrowly between 0.22% and 0.48% in temperate and warm environments, respectively. However, exercise and environmental insult often pose a greater acute challenge to fluid balance homeostasis.

When body water deficits occur from sweat losses, a hypertonic hypovolemia generally results. Plasma volume decreases and plasma osmotic pressure increases in proportion to the decrease in total body water. Plasma volume decreases because it provides the fluid for sweat, and osmolality increases because sweat is ordinarily hypotonic relative to plasma (Costill, 1977). Resting plasma osmolality increases in a linear manner from about 288 mosmol/kg when euhydrated to more than 300 mosmol/kg when hypohydrated (Institute of Medicine, 2005). The increase in osmotic pressure is primarily due to increased plasma sodium and chloride with no consistent effect on potassium concentrations (Edelman et al., 1958; Senay, 1968; Kubica et al., 1983). Figure 32.2 shows the impact of hyperosmotic hypovolemia on fluid regulation, i.e. conservation of water at the site of the kidney and acquisition of water via the stimulation of thirst.

Incomplete fluid replacement decreases total body water and, as a consequence of free fluid exchange, affects each fluid space (Figure 32.1) (Costill et al., 1976; Nose et al., 1983; Durkot et al., 1986; Singh et al., 1993). For example, Costill et al. (1976) determined the distribution of body water loss among the fluid spaces as well as among different body organs during hypohydration. They dehydrated humans via exercise and heat exposure to a range of body mass losses from 2.2% to 5.8% of body mass and determined the fluid deficit apportioned between plasma and the intracellular and extracellular spaces. At a 2.2% body mass loss, 10% of total body water losses were from the plasma and 30% and 60% were from the intracellular and extracellular spaces, respectively. At 5.8% body mass loss, 11% of total body water losses were from the plasma, and 50% and 39% were from the intracellular and extracellular spaces, respectively. This demonstrates that hypohydration results in osmotic water redistribution from the intracellular to extracellular fluid space to maintain blood volume,



FIG. 32.2 Schematic diagram of fluid regulation in situations of fluid deficit and surfeit. Solid lines indicate the osmotically stimulated pathways (primary) and dashed lines indicate volume-stimulated pathways (secondary). ⊗ indicates negative feedback pathways; ANP, atrial natiuretic peptide; ADH, antidiuretic hormone; CNS, central nervous system; ECF, extracellular fluid; OPR, oropharyngeal reflex. Adapted from Reeves *et al.* (1998).

but it also underscores that body water losses are shared among all fluid compartments.

Different methods of dehydration are known or suspected to affect the partitioning of body water losses differently than those just described. For example, diuretics increase urine formation and generally result in the loss of both solutes and water. Diuretic-induced hypohydration generally results in an isotonic hypovolemia, with a much greater ratio of plasma loss to body water loss than either exercise or heat-induced hypohydration (Kubica *et al.*, 1983). As a result, relatively less intracellular fluid is lost after diuretic administration, since there is not an extracellular solute excess to stimulate redistribution of body water. Factors such as heat acclimatization status, posture, climate, and mode and intensity of exercise can also produce significant variability in the distribution of fluids throughout body fluid compartments.

Consequences of Fluid Imbalance

During prolonged physical exercise, profuse sweating coupled with the challenges of drinking enough often leads to dehydration by 2–6% of typical body mass (Sawka *et al.*, 2005). Although this is more common in hot environments, similar deficits are observed in cold climates when working in heavy clothing (O'Brien *et al.*, 1996). The mismatch between intakes and losses is due to

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physiological and behavioral factors. There are other situations where individuals purposefully dehydrate to gain a performance advantage. For example, boxers, power lifters, and wrestlers will dehydrate to compete in lower weight classes, presumably to improve their strength-to-mass ratio.

Water deficits increase the core temperature and heartrate response to exercise and increase perception of effort to perform any given physical task (Sawka, 1992). In warm weather, the core temperature is typically increased an additional 0.1–0.2°C for every percent body weight lost due to water losses, whereas heart rate increases an additional 3–5 bpm (Sawka, 1992; Institute of Medicine, 2005). The magnitude of the penalty is of sufficient magnitude that it effectively negates the core temperature and cardiovascular advantages conferred by high aerobic fitness and heat acclimation (Sawka, 1992). In cooler weather, hypohydration induces a more modest impact on core temperature and heart rate (Cheuvront *et al.*, 2005a).

The thermal and cardiovascular burden accompanying dehydration are regulated adjustments to compensate for the reduced ability to deliver heat from core to skin without compromising blood pressure. Consistent with this hypothesis are observed increases in the threshold core temperature for skin vasodilatation and commencement of sweating, and reduced sensitivity of each to changes in core temperature (Kenney and Johnson, 1992; Montain *et al.*, 1995). Both the singular and combined effects of plasma hyperosmolality and hypovolemia have been implicated for mediating these thermoregulatory adjustments (Sawka, 1992). As mentioned earlier, the thermal and cardiovascular adjustment is tempered in cooler environments (Sawka *et al.*, 1983; Kenefick *et al.*, 2004; Cheuvront *et al.*, 2005a).

A physiological consequence of hypohydration is deterioration in the ability to perform endurance-type physical activities. For example, McGregor *et al.* (1999) reported that semi-professional soccer players who were hypohydrated by >2% of body mass were less able to sprint during the later stages of a variable-intensity running protocol meant to simulate match play. They also took longer to complete an embedded soccer dribbling task. Hypohydration appears to have little or no effect on muscular strength (Greiwe *et al.*, 1998; Evetovich *et al.*, 2002) or anaerobic performance (Jacobs, 1980; Cheuvront *et al.*, 2005a) but sometimes has been reported to reduce dynamic small-muscle endurance (Montain *et al.*, 1998; Bigard *et al.*, 2001) and tolerance to repeated bouts of high-

intensity work (Judelson *et al.*, 2007). Hypohydration in excess of 2% body mass is, however, associated with deterioration in the ability to execute sport-specific skills

excess of 2% body mass is, however, associated with deterioration in the ability to execute sport-specific skills (Dougherty *et al.*, 2006; Baker *et al.*, 2007). For example, Baker *et al.* (2007) reported that basketball players attempted fewer shots and were less able to make shots linked with movement (e.g. lay-up) when hypohydration had exceeded 3%, and shooting was further impaired when 4% hypohydrated. While the mechanism remains unresolved, it may be linked to changes in vestibular function and/or vestibular sensitivity as a consequence of water deficit (Lepers *et al.*, 1997; Gauchard *et al.*, 2002).

The threshold for performance decrements appears to be at or about >2% of body mass, at least in temperatewarm-hot environments (Cheuvront et al., 2003). As the level of dehydration increases, aerobic exercise performance is degraded proportionally (Institute of Medicine, 2005). It has previously been demonstrated that high levels of aerobic fitness and acclimatization status provide some thermoregulatory advantage. However, dehydration seems to cancel out this protective effect during exercise heat stress (Buskirk et al., 1958; Sawka et al., 1983; Merry et al., 2010). A review of studies (Cheuvront et al., 2003) that observed the specific effects of hypohydration (-2% body mass) on aerobic exercise performance found that, in environments of >30°C, aerobic exercise performance was decreased by anywhere from 7% to 60%. It also appears that the magnitude of the effect increases as exercise extends beyond 90 minutes. Overall what can be taken from this review is that the impact of hypohydration on prolonged work effort is magnified by hot environments and probably worsens as the level of hypohydration increases.

The performance penalty accompanying hypohydration may be dampened in cool weather. Cheuvront and Sawka (2005) observed an 8% reduction in total work during a 30-minute cycling time trial when hypohydrated by 3% of body mass in a 20°C environment. However, in a 2°C environment, no effect of hypohydration was observed. More recently, Kenefick *et al.* (2010) observed decrements in aerobic performance (15-minute cycling time trial) of -3%, -5%, -12%, and -23% in 10°C, 20°C, 30°C, and 40°C respectively, when volunteers were hypohydrated by 4% of body mass. Therefore, the temperature cusp at which dehydration altered aerobic exercise performance to an extent considered meaningful appears to be at 20°C.

The physiological factors that contribute to the hypohydration-mediated aerobic exercise performance



FIG. 32.3 The impact of dehydration on physiological function and ability to perform work/exercise relative to percent losses in body mass. Adapted from Greenleaf (1992).

decrements include increased body core temperature, increased cardiovascular strain, increased glycogen utilization, and perhaps altered central nervous system function (Montain et al., 1998; Febbraio, 2000; Nybo and Nielsen, 2001; Cheuvront et al., 2010b). Though each factor is unique, evidence suggests that they interact to contribute in concert, rather than in isolation, to degrade aerobic exercise performance (Cheuvront et al., 2003). The relative contribution of each factor may differ depending on the specific activity, environmental conditions, heat acclimatization status, and athletic prowess, but elevated hyperthermia probably acts to accentuate the performance decrement. One explanation for the impact of hypohydration on exercise performance is a reduction in circulating blood and plasma volume. Cardiac filling is reduced and larger fractional utilization of oxygen is required at any given workload (Cheuvront et al., 2010b). Ultimately, these responses have a negative impact on exercise/work performance, especially in warm/hot environments.

Hypohydration and hyperthermia have also been shown to degrade cognitive/mental performance when concentration, skilled tasks, and tactical issues are involved (Institute of Medicine, 2005). The evidence is stronger for a negative effect of hyperthermia than for mild hypohydration on degrading cognitive/mental performance (Cian *et al.*, 2000), but the two are closely linked when physically active in warm/hot weather. The impact of hypohydration on physiological function, ability to perform work/exercise and survivability are depicted in Figure 32.3.

Illnesses and Disease

In clinical medicine, disturbances of body fluid and electrolyte balance are associated with significant medical costs, morbidity, and mortality across the lifespan (Warren et al., 1994; Black et al., 2003). Fluid and electrolyte imbalances represent a common problematic complication of acute medical treatment scenarios (e.g. cardiovascular, renal, burns) and are also functionally linked to a number of acute and chronic diseases (Manz, 2007). The World Health Organization (1995) considers hypohydration of ≤5% of body mass to be mild on a life-threatening scale. When substantial solute (electrolyte) is lost in situations of long duration work and heat stress (profuse sweating), or during cold or high-altitude exposure, and in numerous illnesses and disorders (e.g. gastroenteritis, hyperemesis, diuretic treatment, dialysis), an isotonic or hypotonic hypovolemia is the result (World Health Organization, 1995; Mange et al., 1997; Cheuvront et al., 2005b; Sawka et al., 2007). However, proper diagnosis of hypovolemia of isotonic or hypotonic origins, especially in austere environments, remains elusive because an accurate and reliable method for assessment has not yet been developed (McGee et al., 1999).

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It has been suggested that chronic plasma hypertonicity as a result of hypohydration may promote obesity and related metabolic dysregulation, and may play a role in chronic disease (Haussinger *et al.*, 1993; Keller *et al.*, 2003; Stookey *et al.*, 2004). Presently, support is limited, but there is increasing evidence that chronic mild hypohydration may account for various morbidities including urolithiasis (kidney stones), urinary tract infections, bladder and colon cancer, constipation, hypertension, venous thromboembolism, coronary artery disease, mitral valve prolapse, stroke, gallstones, glaucoma, and dental diseases (Manz, 2007). While further epidemiological studies will be needed to determine possible links between chronic hypohydration and these morbidities, the dangers of over-drinking (hyponatremia), are well known.

Hyponatremia

Hyperhydration is not easy to sustain since overdrinking of water or carbohydrate-electrolyte solution produces a fluid overload that is rapidly excreted by the kidneys (Figure 32.2) (Freund et al., 1995). However, excessive intake of hypotonic fluid, especially over an extended time, can dilute plasma sodium to dangerously low levels (<135 mEq/L). Dilution of plasma sodium will induce movement of water from the extracellular fluid into cells. If it occurs rapidly and is of sufficient magnitude, this fluid shift can congest the lungs, swell the brain, and alter central nervous system function. The clinical signs and symptoms associated with hyponatremia include confusion, disorientation, mental obtundation, headache, nausea, vomiting, aphasia, incoordination, and muscle weakness with the severity of symptomatology related to the magnitude of decline in serum sodium and the rapidity with which it develops (Knochel, 1996). Complications of severe and rapidly evolving hyponatremia include seizures, coma, pulmonary edema, and cardiorespiratory arrest. Symptomatic hyponatremia arises during clinical care, but has developed in otherwise healthy individuals participating in marathon and ultramarathon competition (Davis et al., 2001; Speedy et al., 2001; Hew et al., 2003), military training (Garigan and Ristedt, 1999; O'Brien et al., 2001), and recreational activities (Backer et al., 1993).

The hyponatremia associated with prolonged exercise most often occurs when individuals consume low-sodium drinks or sodium-free water in excess of sweat losses, either during or shortly after completing exercise (Garigan and Ristedt, 1999; Montain *et al.*, 2001; Speedy *et al.*, 2001). Unreplaced sodium losses contribute to the rate and magnitude of sodium dilution. In those individuals who produce a relatively salty sweat, there are situations where drinking sodium-free water at rates near to or slightly less than sweating rate can theoretically produce biochemical hyponatremia when coupled with the progressive loss of electrolytes (Montain *et al.*, 2001). As such, the mechanism that leads to exercise-associated hyponatremia is overdrinking in its absolute (volume-related) and relative forms (relative to sodium loss).

Exercise-associated hyponatremia can be prevented by not drinking in excess of sweating rate, and by consuming salt-containing fluids or foods when participating in exercise events that produce multiple hours of continuous or near-continuous sweating.

Hydration Assessment

Human hydration assessment is a key component for prevention and proper treatment of fluid and electrolyte imbalances (Mange et al., 1997; Oppliger and Bartok, 2002; Cheuvront et al., 2005). The efficacy of any assessment marker depends critically upon the nature of body fluid losses. In many clinical and most sports medicine situations, hypertonic hypovolemia occurs when there is net loss of hypotonic body fluids (Mange et al., 1997; Cheuvront et al., 2005; Sawka et al., 2007). The rise in extracellular tonicity is a hallmark clinical feature that provides diagnostic distinction from isotonic or hypotonic hypovolemia (Feig and McCurdy, 1977; Mange et al., 1997). Hypotonic fluid losses modulate renal function and urine composition in accordance with the body water deficit (Robertson and Mahr, 1971), thus providing the fundamental framework for using blood (osmolality, sodium, fluid regulatory hormones) and urine (osmolality, specific gravity, color) as principal body-fluid hydration assessment measures.

Although plasma osmolality is the criterion hydration assessment measure for large-scale fluid needs assessment surveys (Institute of Medicine, 2005), the optimal choice of method for assessing hydration is limited by the circumstances and intent of the measurement. Popular hydration assessment techniques vary greatly in their applicability to laboratory or field use because of methodological limitations which include the necessary circumstances for accurate measurement, ease of application, and sensitivity for detecting small but meaningful changes in hydration status (Table 32.1). Large population heterogeneity explains, in part, why there are presently few hydration

Technique	Advantages	Disadvantages
Complex markers		
Total body water (dilution)	Accurate, reliable	Analytically complex, expensive, requires baseline and serial measures
Plasma osmolality	Accurate, reliable (clinical standard)	Analytically complex, expensive, invasive
Simple markers		
Fluid input/output	Accurate, reliable (clinical standard)	Requires urinary catheter and serial measures
Urine concentration	Easy, rapid, screening tool	Easily confounded, timing critical, frequency and color subjective
Body mass	Easy, rapid, screening tool	Requires baseline; confounded by changes in body composition
Other markers		
Blood:		
Plasma volume Plasma sodium Fluid balance bormones	No advantages over osmolality (except hyponatremia detection for plasma sodium)	Analytically complex, expensive, invasive, multiple confounders
Bioimpedance	Easy, rapid	Requires baseline, multiple confounders
Saliva	Easy, rapid	Highly variable, multiple confounders
Physical signs	Easy, rapid	Too generalized, subjective
Tilt test (orthostatic challenge)	Rapid	Highly variable, insensitive, requires tilt table or ability to stand
Thirst	Positive symptomatology	Subjective and variable, develops late and is quenched early

TABLE 32.1 Laboratory hydration assessment techniques summary

Adapted from Institute of Medicine (2004) and Cheuvront et al. (2005).

TABLE 32.2	Biomarkers	of	hydration	status
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Measure	Euhydration	Population reference interval	Dehydration
Total body water (L)	<1%	N/A	≥3%(?)
Plasma osmolality (mmol/kg)	<290	285-295	≥297
Urine specific gravity (units)	<1.02	1.005-1.035	≥1.025
Urine osmolality (mmol/kg)	<700	300-900	≥831
Urine color (units)	<4	N/A	≥5.5
Body weight ^a (kg)	<1%	N/A	≥2%

^aPotentially confounded by changes in body composition during very prolonged assessment periods. Compiled from Kratz et al. (2004), Cheuvront et al. (2005, 2010a), and Sawka et al. (2007).

status markers that display potential for high nosological sensitivity from a practical, single measure (Cheuvront *et al.*, 2010a). Change measures can provide good diagnostic accuracy, but their usefulness also depends on the homogeneity of measures taken on the same person if dayto-day monitoring is desired (Cheuvront *et al.*, 2010a). More acute change measures (over hours) require a valid baseline and control over confounding variables. Table 32.2 provides definable thresholds which can be used as a guide to detect a negative body fluid balance stemming from hypertonic hypovolemia. Hydration should be considered adequate when any two assessment outcomes are consistent with euhydration (Table 32.2) (Cheuvront and Sawka, 2005; Sawka *et al.*, 2007). Values that occur between euhydration and hypohydration represent typical human variation (Kratz *et al.*, 2004) in homeostatic setpoints relating to biology as well as to social (diet) and environmental (exercise, climate) influences.

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Water and Electrolyte Needs

Human water and electrolyte needs should not be based on a "minimal" intake, as this might eventually lead to a deficit and possible adverse performance and health consequences. The Food and Nutrition Board of the Institute of Medicine instead base the dietary recommended intake (DRI) for water needs on an adequate intake (AI). The AI is based on experimentally derived intake levels that are expected to meet nutritional adequacy for essentially all members of a healthy population. The Al level for water is 2.7 to 3.7 L/day for sedentary women and men over age 19, respectively (Institute of Medicine, 2005). These values represent total water intake from all fluids (80%) and foods (20%). The AI for sodium is 1.5 g/day, or 3.8 g/day sodium chloride (Institute of Medicine, 2005). It should be recognized, however, that endurance athletes and occupational laborers performing extended hours of work, particularly in warm climates, may greatly exceed the AI for water and sodium (Institute of Medicine, 2005).

Table 32.3 (Rehrer and Burke, 1996) illustrates the wide variability in hourly sweat losses observed both within and between sports and occupations. Depending upon the duration of activity and heat stress exposure, the impact of these elevated hourly sweat rates on daily water requirements will vary. Figure 32.4 depicts generalized modeling approximations for daily water and sodium requirements based upon calculated sweating rates as a function of daily energy expenditure (activity level) and air temperature (Institute of Medicine, 2005). Applying this prediction model, it is clear that daily water requirements can increase two- to six-fold from baseline by simple manipulation of either variable. For example, daily water requirements for any given energy expenditure in temperate climates (20°C) can triple in very hot weather (40°C). In addition to air temperature, other environmental factors also modify sweat losses to include relative humidity, air motion, solar

TABLE 32.3 Sweating rates for different sports

Sport	Mean (L/h)	Range (L/h)
Water polo	0.55	0.30-0.80
Cucling	0.80	0.29-1.25
Cycling	1.10	0.54-1.83
Rackothall	1.11	0.70-1.60
Soccer	1,17	0.70-2.10

Data compiled from Rehrer and Burke (1996).

load, and choice of clothing for protection against environmental elements (Latzka and Montain, 1999). Therefore, water losses, and hence water needs, will vary considerably among moderately active people based on changing extraneous influences.

Sweat contains electrolytes, primarily sodium chloride and to a lesser extent potassium, calcium, and magnesium (Costill et al., 1975; Costill, 1977; Verde et al., 1982). Sweat sodium concentration averages ~35 mEq/L (range 10-70 mEq/L) and varies depending upon diet, sweating rate, hydration level, and heat acclimation state (Allan and WIlson, 1971; Costill et al., 1975). Sweat potassium concentration averages 5 mEq/L (range 3-15 mEq/L), calcium averages 1 mEq/L (range 0.3-2 mEq/L), magnesium averages 0.8 mEq/L (range 0.2-1.5 mEq/L), and chloride averages 30 mEq/L (range 5-60 mEq/L) (Costill, 1977). Neither gender, maturation nor aging seems to have marked effects on sweat electrolyte concentrations (Morimoto et al., 1967; Meyer et al., 1992). Sweat glands reabsorb sodium by active transport, but the ability to reabsorb sweat sodium does not increase proportionally with the sweating rate. As a result, the concentration of sweat sodium increases at high sweating rates (Allan and



FIG. 32.4 Daily water needs and required daily sodium intake estimated from sweat-loss predictions as a result of changes in physical activity and air temperature. Daily energy expenditures of A = 3600 kcal/ C = 2400 kcal/day,and B = 2900 kcal/day,day, D = 1900 kcal/day corresponds to very active, active, low activity, and sedentary. Adapted from Institute of Medicine (2005).

Wilson, 1971; Costill et al., 1975; Buono et al., 2008). Heat acclimation improves the ability to reabsorb sodium, thus heat-acclimated persons have lower sweat sodium concentrations (>50% reduction) for any given sweating rate (Allan and Wilson, 1971).

Generalized modeling approximations for daily sodium needs based upon calculated sweating rates as a function of daily energy expenditure (activity level) and air temperature (Institute of Medicine, 2005) are presented in Figure 32.4. This analysis assumes that persons are heat acclimated and have a sweat sodium concentration of 25 mEq/L (about 0.6 g/L). The average American diet contains -4 g/ day sodium (Institute of Medicine, 2005) but varies greatly depending upon ethnic preferences for food. Increases or decreases in sodium stores are usually corrected by adjustments in a person's salt appetite. In addition, when physical activity increases, the additional caloric intake associated with increased activity usually covers the additional sodium required (Institute of Medicine, 2005). Therefore, sodium supplementation is generally not necessary, as normal dietary sodium intake appears adequate to compensate for sweat sodium losses (Sawka et al., 2007). There are two exceptions: first, prolonged heavy sweating can produce substantial salt losses, and secondly, for those unacclimatized to the weather, during the first few days of warm/hot weather as they will be secreting saltier than usual sweat. Salting food to taste is usually an adequate solution in these circumstances. Another strategy is to rehydrate with fluids containing ~20 mEq/L of sodium. Most commercial sports beverages approximate this concentration (Sawka et al., 2007).

Fluid Replacement

The 2007 American College of Sports Medicine Position Statement on Exercise and Fluid Replacement (Sawka et al., 2007) summarizes current knowledge regarding fluid and electrolyte needs and the impact of their imbalances on performance and health. This statement stresses the fact that individuals have varying sweat rates, and individual fluid needs can be very different despite performing a similar task in nearly identical environmental conditions. The ACSM Position Statement also provides recommendations in relation to hydration prior to, during, and following exercise/activity. Briefly, the objective is to begin physical activity euhydrated and with normal plasma electrolyte levels. If sufficient beverages are consumed with

meals and a protracted recovery period (8 to 12 hours) has elapsed since the last exercise session, then the person should already be close to being euhydrated (Institute of Medicine, 2005). During exercise the objective is to drink enough fluid to prevent excessive dehydration (>2% body mass loss) to accrue and compromise performance. The amount and rate of fluid replacement depends upon an individual's sweating rate, the exercise duration, and opportunities to drink. It is recommended that individuals should monitor body mass changes during training/ activity to estimate their sweat lost during a particular exercise task with respect to the weather conditions.

Carbohydrate consumption can be beneficial to sustain exercise intensity during high-intensity exercise events of ~1 hour or longer, as well as less intense exercise/activity sustained for longer periods (Coyle and Montain, 1992). Carbohydrate-based sports beverages are used to meet carbohydrate needs, while attempting to replace sweat water and electrolyte losses. Carbohydrate solutions of 5–10% consumed at a rate of 1 L per hour would approximate a consumption rate of 1 g per minute, which has been demonstrated to maintain blood glucose levels and exercise performance (Coyle and Montain, 1992). The greatest rates of carbohydrate delivery have been achieved with a mixture of simple sugars (e.g. glucose, sucrose, fructose, maltodextrin).

The Institute of Medicine also provides general guidance for composition of "sports beverages" for persons performing prolonged physical activity in hot weather (Institute of Medicine, 1994). The need for these different components will depend on the specific exercise task (e.g. intensity and duration) and weather conditions, and can be met using non-fluid sources such as gels, energy bars, and other foods. Following activity, consumption of normal meals and snacks with a sufficient volume of plain water will restore euhydration, provided the food contains sufficient sodium to replace sweat losses (Institute of Medicine, 2005). If hypohydration is substantial (>2% body mass loss) with a relatively short recovery period (<4–6 hours), then an aggressive rehydration program may be merited (Maughan *et al.*, 1996).

In most cases of gastrointestinal tract disturbances that result in diarrhea and/or vomiting (-1 day), typical intake of food and fluid over the course of a few days will correct fluid and electrolyte losses. However, when these maladies are left untreated, prolonged bouts (>1 day) may require a unique fluid replacement strategy. Severe hypohydration

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of this type can require intravenous rehydration and hospitalization. However, when possible, oral rehydration with an oral electrolyte solution is the treatment of choice and is recommended by the World Health Organization (1995). While sport drinks contain carbohydrate and electrolytes, they are specifically designed for situations of hypertonic hypovolemia. The fluid and electrolyte losses resulting from diarrhea and/or vomiting (isotonic dehydration) can be more rapidly corrected with oral rehydration solutions containing 50–90 mEq per liter of sodium and ~20 mEq per liter of potassium, and ingested with complex carbohydrates (World Health Organization, 1995).

Future Directions

The ability to assess hydration state is vitally important in clinical, occupational, and sport settings. Further work is required to develop simple, accurate, non-invasive technologies or methods that can assess hydration state without the need for baseline or repeated measures.

A wide range in the percent decrement of aerobic exercise performance due to dehydration has been reported in the literature. Further work is needed to more precisely define the specific impacts of dehydration on aerobic exercise performance.

In the scientific literature a number of chronic health conditions have been suggested to be associated with hydration, including kidney stones, gallstones, bladder, colon and other cancers, arrhythmias, and blood clots among other conditions. Further work is required to determine if any link between hydration state and these and other conditions exists.

The etiology of skeletal muscle cramps has been debated in the scientific literature. Dehydration and sodium deficits have been proposed as a causal mechanism. Further work is required to determine the relationship between dehydration/sodium deficits and skeletal muscle cramps.

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Sweat rate prediction equations for outdoor exercise with transient solar radiation

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Gonzalez RR, Cheuvront SN, Ely BR, Moran DS, Hadid A, Endrusick TL, Sawka MN. Sweat rate prediction equations for outdoor exercise with transient solar radiation. J Appl Physiol 112: 1300-1310, 2012. First published January 12, 2012; doi:10.1152/japplphysiol.01056.2011.-We investigated the validity of employing a fuzzy piecewise prediction equation (PW) [Gonzalez et al. J Appl Physiol 107: 379-388, 2009] defined by sweat rate $(m_{sw}, g \cdot m^{-2} \cdot h^{-1}) = 147 + 1.527 \cdot (E_{req}) - 0.87 \cdot (E_{max})$, which integrates evaporation required (Ereq) and the maximum evaporative capacity of the environment (Emax). Heat exchange and physiological responses were determined throughout the trials. Environmental conditions were ambient temperature $(T_a) = 16-26^{\circ}C$, relative humidity (RH) = 51-55%, and wind speed (V) = 0.5-1.5 m/s. Volunteers wore military fatigues [clothing evaporative potential $(i_m/clo) = 0.33$] and carried loads (15-31 kg) while marching 14-37 km over variable terrains either at night (N = 77, trials 1–5) or night with increasing daylight (N = 33, trials 6 and 7). PW was modified (Pw,sol) for transient solar radiation ($R_{\rm sol}$, W) determined from measured solar loads and verified in trials 6 and 7. PW provided a valid m_{sw} prediction during night trials (1-5) matching previous laboratory values and verified by bootstrap correlation (r_{bs} of 0.81, SE \pm 0.014, SEE = \pm 69.2 g·m⁻²·h⁻¹). For trials 6 and 7, E_{req} and E_{max} components included R_{sol} applying a modified equation Pw,sol, in which $m_{sw} = 147 + 1.527 \cdot (E_{req,sol}) - 0.87 \cdot (E_{max})$. Linear prediction of $m_{sw} = 0.72 \cdot \dot{P}w$, sol + 135 (N = 33) was validated ($R^2 = 0.92$; SEE = $\pm 33.8 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$) with PW β -coefficients unaltered during field marches between 16°C and 26°C T_a for $m_{sw} \le 700 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$. PW was additionally derived for cool laboratory/night conditions $(T_a < 20^{\circ}C)$ in which E_{req} is low but E_{max} is high, as: PW,cool $(g \cdot m^{-2} \cdot h^{-1}) = 350 + 1.527 \cdot E_{req} - 0.87 \cdot E_{max}$. These sweat prediction equations allow valid tools for civilian, sports, and military medicine communities to predict water needs during a variety of heat stress/exercise conditions.

thermoregulation; modeling; load carriage; environmental indexes; fluid replacement

NUMEROUS public health (21, 38), military medicine (6–11, 23, 28, 29) and sports medicine (29, 39) situations exist where it is important to estimate water needs. When performing physical exercise in warm-hot environments, sweat loss is the "critical" factor to calculate water requirements (18, 21, 23, 38). We recently developed from laboratory experiments a fuzzy piecewise equation (PW) that predicts measured sweat losses within a standard error estimate (SEE) of ± 137 ml/h (17). The equation was also validated against several laboratory (indoor) studies with soldiers wearing military clothing-equipment, as

well as one field study (outdoors) in which soldiers wore chemical protective clothing while exposed to constant and low solar loads and low-intensity and high-intensity metabolic rates (M, W/m^2). Therefore, both the initial model development and the validation studies represented conditions impacted by constant mild-to-moderate solar radiation.

Sweating rate $(m_{sw}, g \cdot m^{-2} \cdot h^{-1})$ is calculated from PW as: 147 + 1.527 \cdot (E_{req}) - 0.87 \cdot (E_{max}) (17). Prediction accuracy is improved by 50-60% over legacy equations (41) and PW has wide applicability to a broader range of environmental temperatures, metabolic rates, and modern military clothing equipment configurations. However, it is unknown if the PW equation provides an improvement over other conventional equations that predict sweat loss with solar load (42). Furthermore, PW has not been validated over extensive military operational missions (outdoors) that encompass heat loads from transient solar radiation. Previous studies have shown that sweat rate is altered by solar heat flux (14, 30) and the whole body sweat rate is elevated proportional to the magnitude of thermal and exercise load. Accurate measurements of required evaporative heat loss (Ereq) can be predicted by analyzing key heat exchange parameters of the heat balance equation (5, 15, 20, 24). The impact of solar radiation in modifying heat exchange, and thus sweat rate prediction, is easily determined empirically (15, 16, 24, 25, 30). The most strenuous military operations are often conducted in early morning hours that are subject to transient solar radiation coupled with cooler environmental temperatures. A requirement exists to carefully measure sweat rate during outdoor military activities with and without solar radiation to determine the validity of the PW equation for these conditions and ascertain if PW should be modified from appropriate empirical measurements.

The purposes of this study were 1) to validate the original PW sweat prediction equation, derived from laboratory studies, for implementation outdoors at night and with transient solar circumstances in soldiers performing military activities and wearing military clothing-equipment; and 2) to decide whether a modified PW equation should be developed de novo, and if so, then determine if it provides a reliable prediction of sweat rate during prolonged work with transient solar radiation conditions. Our hypothesis was that regression coefficients in the fuzzy piecewise algorithm deriving the PW (15, 44) would be robust enough to permit valid m_{sw} predictions during outdoor night marches, but would require adjustment (Pw,sol) for transient solar radiation exposures and possibly cooler conditions. Consequently, an additional hypothesis was that the PW equation, adapted with required solar load factors, will provide a reliable sweat loss (water needs) prediction equation that is

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Table 1. Description of conditions for the night marches (trials 1–5)

Trial	Ν	Section	Time, min	Distance, km	Terrain Type, % of Section	Terrain Factor (η)
1 and 2	25	1	60	6	Base course, 40%; sand, 60%	1.4
		2	50	5	Hard road, 40%; plowed field, 10%; hard road, 50%	1.4
		3	50	5	Hard road, 40%; plowed field, 10%; hard road, 50%	1.4
		4	68	5	Base course, 40%; sand, 60%	1.4
		5	30	3	Base course, 40%; sand, 60%	1.4
3	12	1	60	6	Hard road, 40%; wet hard sand, 60%	1.5
		2	50	5	Hard road, 40%; plowed field, 10%; hard road, 50%	1.5
		3	65	6.5	Wet hard sand, 80%; dry sand, 20%	1.5
		4	65	6.5	As above	1.5
		5	55	5.5	Same as section 2	1.5
		6	75	7.5	Dry sand, 80%; 1 km on hard road, 20%	1.5
4 and 5	40	1	55	6	Trial 4: -7.3 km/h (%gradient -0.7) descent on gravel, 15 min rest; trial 5: -9.6 km/h (%gradient -0.8), 15 rest	1.3
		2	55	6	Trial 4: 10 km/h ascent on gravel; 17 min rest; trial 5: 7.8 km/h (% gradient 0.7) ascent; 17 min rest.	1.3
		3	28	2	<i>Trial 4</i> : -16.1 km/h (%gradient -0.8) descent on gravel, completion; <i>trial 5</i> : 1.7 km/h ascent (%gradient 0.2), march completion.	1.3

N is number of volunteers completing each trial. Section is the type of road during each march, % time, and various ascent/descent (km/h; % gradient) marches of *trials 4* and 5. Terrain factor (η) is unit coefficient of Pandolf equation prediction (31, 32), as modified by Santee et al. (35) for specific descent marches.

functional for a wide range of indoor and outdoor operational scenarios with improved prediction over legacy equations (41, 42) and other modeling approaches (3, 24, 46) that account for solar radiation. As in the previous study (17), we applied Tseng's and coworkers (44) fuzzy piecewise analysis to predict sweat losses measured from field data assuming that m_{sw} (lumped efferent eccrine output) has both linear and nonlinear characteristics as a function of core temperature (T_{core}) and skin temperature (Tsk) inputs (15, 24, 37). Nonthermal factors (43) that may affect the general gain of the efferent thermal drive and sweating threshold were not accounted for in the analysis. The sweat loss equations (indoor and transient solar load) in the present study should be considered as lumped derivatives and include central nervous system sudomotor drive principally from thermal factors with nonthermal factors having minimal effect (37).

METHODS

One-hundred ten male soldier volunteers participated in numerous outdoor field trials. The appropriate institutional human use review boards approved the protocol, and all volunteers provided written informed consent. Investigators adhered to policies for protection of human subjects as prescribed in US Army Regulations 70–25 and US Army Medical Research and Materiel Command Regulation 70–25. The research was conducted in adherence with the provisions of Code 45 of Federal Regulation part 46.

Experimental studies. Experimental data were collected by staff of the Heller Institute of Medical Research. Seven outdoor marches were performed by active military units and incorporated into their training,

with accommodations made for careful data collection. The military units maintained normal leadership, training hours, clothing-equipment, and work rates (load and speed) applicable to actual missions. Exercise level per se, state of hydration, and sleep state in the subjects all were controlled. Subjects were well-hydrated at the beginning and during rest, and none of the subjects was sleep deprived.

The outdoor marches were conducted near field stations exhibiting diverse terrains (desert, Mediterranean coastal, and various foothill areas). Tables 1 and 2 describe the number of subjects and specific conditions for the night (*trials* 1-5) and transient solar radiation (*trials* 6 and 7) outdoor marches, respectively. Data were collected on 77 volunteers who marched at night (*trials* 1-5), and some of these individuals participated in multiple trials. Thirty three supplementary volunteers marched during the transient solar radiation conditions (*trials* 6 and 7). Table 3 shows many of the variables and equations with essential modifications used in the study.

Physiological measures. Oxygen uptake was measured from a cohort of the volunteers. These data were then used to estimate metabolic rate of other individuals in each group. Metabolic rate was calculated from a 90-s sample of expired air collected using a K4B (COSMED, Italy) metabolic measurement device. Marching pace and grade were estimated using a Garmin GPS navigator. Oxygen uptake calculations were estimated based on weight, load, walking speed + grade, and terrain factor using Pandolf et al. (32) equations and Santee et al. (35) modifications for some downhill trials to estimate net heat production. In some cases, a median terrain factor coefficient was chosen since portions of some marches occurred on gravel, sand, and paved road (Tables 1 and 2). The oxygen uptake calculation was for the exercise portion only, as rest periods were estimated at a metabolic rate of 120 W (average of $63 \pm 3 \text{ W/m}^2$)(15, 24). A standard respiratory exchange ratio for a mixed diet was estimated for consis-

Table 2. Description of conditions for the transient solar load marches (trials 6 and 7)

Trial	Ν	Section	Time, min	Distance, km	Terrain Type/% of Section	Terrain Factor (η)
6	20	1	65	6.0	Gravel, 100%; 18-min rest period	1.30
		2	48	4.4	Gravel, 100%; 17-min rest period	1.30
		3	62	6.0	Gravel, 100%	1.30
7	13	1	58	5.8	Paved road, 43%; gravel, 57%	1.25
		2	71	6.7	Gravel, 100%	1.25
		3	62	5.8	Paved road, 43%; gravel, 57%	1.25

Abbreviations are same as Table 1. *Trial* 6 began at 0330 and ended at 0700; average global solar load (gSL) monitored from 2 stations = 63 W/m^2 . *Trial* 7 began at 1420 and ended at 1800; average gSL = 265 W/m^2 .

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Variable	Units	Description	Formula	Refs.	Modification in Present Study
PW	$g \cdot m^{-2} \cdot h^{-1}$	Sweat rate prediction by fuzzy piecewise (PW) change point regression	$\begin{array}{l} 147 + (1.527 \!\cdot\! E_{req}) - \\ (0.87 \!\cdot\! E_{max}) \end{array}$	17, 44	Calculation by bootstrap correlation of original and night field data: equation remains valid $N > 500$ cases; outliers do not statistically change comparison; SEE within $\pm 69 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$
М	W/m ²	Metabolic heat production	Calculated from measured oxygen uptake (Vo ₂) and Pandolf equation	15, 32, 35	Pandolf equation adjusted by Santee coefficients
$\dot{P}_{ m w,sol}$	$g \cdot m^{-2} \cdot h^{-1}$	Sweat rate prediction for transient solar load	$147 + (1.527 \cdot E_{req,sol}) - (0.87 \cdot E_{max})$	This study, Fig. 3	Solved for R_{sol} per march time using transient solar field data; sweat rate becomes predictable as OLS equation: $0.72 \cdot \dot{P}$ w,sol + 135, $R^2 = 0.92$
E _{max}	$g \cdot m^{-2} \cdot h^{-1}$	Maximum evaporation capacity of a given environment	$E_{max}=\omega h_e(P_{s,sk}-P_a)$	15	Adjusted by skin wettedness (ω). The fraction of the total body area (A_D) covered by sweat [wetted area (A_w)], i.e., A_w/A_D . and evaporative heat transfer coefficient, h_e
E _{req}	$g \cdot m^{-2} \cdot h^{-1}$	Required evaporation from heat balance includes total skin evaporation, all respired, non eccrine, and metabolic water losses	$E_{req} = M - (Wext) - DRY - S$	15	Valid for indoor lab and night field data; for transient solar field study, $E_{req,sol}$ first solved for R_{sol} as input to heat balance equation to determine Pw ,sol.
R + C	W/m^2	Dry or sensible heat loss	$[6.45 \cdot (T_a - T_{sk})]/I_T$	4, 15	,
E _{res} C _{res}	W/m ² W/m ²	Respiratory heat loss Convective heat loss	$\begin{array}{l} (E_{res} + C_{res}) = \ A_d \cdot M[0.0014 \\ (34 - T_a) + \ 0.0023 \cdot \\ (44 - P_a)] \end{array}$	15	Modified by ambient temperature and water vapor pressure, maximum Ta and Pa, evaporative potential (Emax), respiratory exchange ratio (R)
E_{dif}	W/m ²	Skin diffusion	$E_{dif} = 0.05 \cdot E_{max}$	15	
m _{res} P _a	g/min kPa or Torr	Metabolic heat loss Ambient water vapor pressure	$m_{res} = Vo_2 \cdot (R \cdot 0.53)$ (RH/100) \cdot exp[18.6686 - (4030.183/T_a + 235)];Antoine equation	17 15	
h _c	$W \cdot m^{-2} \cdot C^{-1}$	Convective heat transfer coefficient	$h_{c} = 1.2 \cdot [(M - 50) \cdot (P_{B}/760)]^{0.39}$	15	Modified by walking, free and forced convection, barometric pressure
Πe	will it c	coefficient	$(2.2 \cdot n_c \text{ or anternativery, with clothing})$ $(2.2 \cdot i_m)/(I_T \cdot 0.155)$		(P _B), Lewis relation at sea level (2.2°C/Torr)
hr	$W \cdot m^{-2} \cdot {}^{\circ}C^{-1}$	Radiative heat transfer equation	$ \begin{split} h_{\rm r} &= 5.67 \cdot 10^{-8} \cdot 0.97 \cdot 0.77 \cdot \\ &[({\rm T}_{\rm sk} + 273)^4 - ({\rm MRT} + \\ &273)^4]/({\rm T}_{\rm sk} - {\rm MRT}) \end{split} $	15	Unmodified
I _T	clo	Total clothing insulation, sum of air (I _a) and fabric (I _{cl}) layer insulation	$(I_a + I_{cl})$	4, 15	$clo = 0.155^{\circ}C \cdot m^2/W$ or thermal conductance of 6.45 $W \cdot m^2/K$
F _{cle}	ND	Effective clothing factor for heat exchange from articulated manikin			
P _{s,sk} R _{cl}	kPa or Torr m²∙K/W	Skin saturation vapor pressure Intrinsic (fabric) thermal resistance	Antoine equation solved for T_{sk} $R_{cl} = R_T - 1/[(h_c+h_r)] \cdot fcl$	15 1, 15	Reciprocal of thermal conductance
$\begin{array}{l} R_t \\ V_{air} \text{ or } V \end{array}$	m²•K/W m/s	Total clothing resistance Ambient air movement (velocity	0.155•I _T Input variable	1, 15 7, 15, 17	Modified by wind and body motion Direct observations
V_{eff}	m/s	Effective air motion produced by wind speed and M	v_{air} + (0.004) (M·A _D - 105)	24, 32	Unmodified
σ		Stefan-Boltzman constant	$5.67 \times 10^{-8} \text{W} \cdot \text{m}^{-2} \cdot \text{K}^{-4}$	1, 15	Unmodified
W _{ext} A _P	W/m^2 m^2	External work based on activity Projected surface area exposed to	Pandolf equations Fanger, ASHRAE equations	32 1, 13	Santee (35) modifications Upright walking
f_{eff}	%	Fraction of body surface exposed to solar load at a given time (A_r/A_D)	Fanger, ASHRAE equations	1, 13	Upright walking
αLW	W	Long wave absorptivity	Breckenridge and Goldman	4, 16	Upright walking
αSW	W	Short wave absorptivity	Breckenridge and Goldman equations	4, 16	Upright walking

 Table 3. Nomenclature and description of key variables and equations implemented

Continued

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Table 3.—*Continued*

Variable	Units	Description	Formula	Refs.	Modification in Present Study
R _{sol}	W	Matthew solar radiant heat flow	$\begin{array}{r} -0.0003 \cdot (\text{gSL})^2 + \\ 0.681 \cdot (\text{gSL}) + 3.136 \end{array}$	25	Adjusted by A_D and $F_{cl.e}$ for inclusion into heat balance to determine $E_{req.sol}$ (W/m ²)
ERF	W/m^2	Effective radiant field	$\frac{h_r (MRT - T_a);@}{[(0.835 \cdot R_{sol})/A_D]}$	15	Interchangeable variables
gSL	W/m^2	Global solar load	Direct weather station data; pyranometer values	25	Direct measurement from weather station data
$I_{\rm TH}$		Total solar irradiance of a horizontal object	$R_{\rm D} \cdot \sin\beta + R_{\rm dif}$	2, 13	Meteorological variables
Me,th		Radiant flux emitted as thermal radiation by a surface.	Shapiro et al., outdoor equations	42	Unmodified
MRT	°C	Mean radiant temperature	$T_a + ERF/h_r$	14, 15	Unmodified
T _{sk} Vair	°C	Mean weighted skin temperature	Mitchell equation	27	3-Site direct measurement Direct measurement
R _D	W	Direct beam solar load	Arens et al., Breckenridge, and	2, 4, 13,	Direct or weather station values
$R_{\rm dif}$	W	Diffuse irradiance	Fanger equations		
R _{ref}	W	Reflected irradiance			
A _D	m ²	Body surface area (BSA) from DuBois equation	$A_{\rm D} = 0.202 \cdot W^{0.425} \cdot H^{0.725}$	1, 15	Observed values

tency based on a respiratory exchange ratio during submaximal intensity exercise (50% $\dot{V}_{02 peak}$) ranging from 0.8 to 0.98 (7, 13).

Although not reported, heart rate and core temperature were measured for medical monitoring purposes. Heart rate was recorded using a Polar heart rate monitor. Core temperature data were recorded using the telemetric pill technique (HQ and Mini Mitter). During the rest periods, three-site skin temperatures were measured by an YSI-409 (YSI, Yellow Springs, OH) surface thermal probe. Mean weighted skin temperature (\overline{T}_{sk}) was calculated using a three-site (chest, thigh, and arm) surface area weighting coefficient formula (27). In the present data set, clothed \overline{T}_{sk} was linearly correlated with T_a by the equation: $\overline{T}_{sk} = 0.53 \cdot T_a + 20.28 (R^2 = 0.83; SEE = \pm 0.54)$ over the range of T_a from 16 to 26°C. Skin saturation vapor pressure (kPa) was determined for each individual skin temperature value using Antoine's equation (15, 24) and the necessary evaporative heat transfer coefficients (h_e) utilized to determine E_{max} for each time interval in the respective trials.

Total sweat losses were determined from changes in body mass, corrected for nonsweat losses, and assume that sweat volume and mass are equivalent (1 ml = 1 g). Sweating rate expressed as liters/h or $g \cdot m^{-2} \cdot h^{-1}$ was determined by time and surface area weightings, as appropriate. Detailed calculations included (7):

$$m_{sw} = \Delta nude body mass$$

$$-(UV + EW + NEFL) + DV]/time$$
 (1)

where Δ nude mass is the difference in nude body mass (g) pre- to postexercise; UV is urine volume; EW is excrement weight, if any; NEFL is noneccrine fluid losses, which include respiratory water losses and CO₂-O₂ exchange (7, 36, 37); and DV is consumed drink volume. Body mass was measured while the subject was minimally clothed and fully clothed before and after each march for estimation of trapped sweat.

Environmental parameters. The environmental parameters ambient air temperature (T_a , °C), relative humidity (RH, %) (transformed to ambient water vapor pressure, kPa), and wind velocity (*V*, m/s) were collected every 30 min using a Kestrel 3000 (Caliber Sales Engineering) and recorded manually for later spreadsheet entry. Composite global solar radiation (gSL, W/m²) was recorded at two field stations in close proximity to the marches. The effective solar load was determined by calculation of R_{sol} and effective radiant field (ERF) and mean radiant temperature (MRT) (15, 16, 24, 25). The procedure employed to determine these coefficients for transient solar load will be described later. Shapiro et al. (42) originally estimated solar radiation effects via several correction factors annexed to their sweat loss prediction equation from data collected during steady-state exposure to a variety of solar load intensities. These factors were used to estimate required evaporative heat loss ($E_{req,SL}$) by assessing separate thermal radiative flux factors analyzed from the heat balance equation as:

$$E_{\text{req.SL}}(\text{watts}) = M - W_{\text{ext}} + [H_{\text{c}} + H_{\text{r}} + H_{\text{L}}].$$
(2)

In the above equation (42), M is metabolic heat production (15, 32, 35); W_{ext} is external work rate (32); H_c is convective heat transfer, calculated as $6.45 \cdot A_D(T_a - \overline{T}_{sk})/I_T$; A_D is the Dubois body surface area (m²) (15); and I_T (4) is the fixed value of total clothing insulation [originally evaluated by a static manikin that include the air (I_a) and intrinsic clothing layers (I_{cl})]. The radiative heat flux factors comprise H_r (W), which was estimated from radiative heat transfer = $[1.5 \cdot A_D \cdot (SLg^{0.6})/I_T]$, where SLg incorporates the shortwave radiative load; and long-wave emission (H_L , W) from the total body to the environment, which was estimated as:

$$\mathbf{H}_{\mathrm{L}} = \left(0.047 \cdot A_{\mathrm{D}} \cdot \mathbf{M}_{\mathrm{e,th}}\right) / \mathbf{I}_{\mathrm{T}} \tag{3}$$

where the factor $(M_{e,th})$ is the radiant heat flux that includes the combined theoretical perfect black-body long wave emission from all body surfaces. $M_{e,th}$ is equal to σ , the Stefan-Boltzman radiation constant (5.67 × 10⁻⁸ W · m⁻² · °K⁻⁴) multiplied by T⁴, calculated as the outer surface layer temperature $(\overline{T}_{cl})^4$ and transformed into °K (273.15 + °C) (4, 15, 25). Effect of heat storage (S) was not accounted for in the above analysis, and steady-state was assumed for all the heat exchange variables.

Several thermal radiation algorithms were derived in the present study quantifying a more inclusive radiative heat transfer analysis possible for the transient state (1, 2, 4, 16, 25). These analyses were applied for evaluating transient solar load on the individual {i.e., when the global solar radiation [gSL \approx (H_r + H_L)] is not constant}. Solar radiation is generally measured as the sum of the total (direct plus diffuse) radiation falling on a horizontal surface (gSL). In meteorologic terms this is expressed as I_{TH}, which varies with solar elevation (1, 2, 16). In addition, the area of the human body exposed to solar radiation, and therefore the solar energy received by the body, also varies with solar elevation. Generally, gSL [or its sequel, I_{TH}, (2, 4)] can be plotted for a specific solar elevation. A key property is the projected area (A_p) solved as a function of the solar altitude and normally is about 20–25° at the highest solar altitude and drops to around 80–90° (1, 2, 13).

The equivalence between I_{TH} , ERF, and MRT (all inclusive radiative heat transfer algorithms) involves the following assumptions. Radiation (R) and convection (C) in the heat exchange are assumed to be equal in plotting MRT. This heat exchange proportionality occurs because the (MRT – T_a) is directly proportional to ERF (14). In the present study, long-wave radiation characterized by MRT and ERF is treated as uniformly distributed (4π) on the individual during each walking phase (15, 16). There exist no provisions for the directional characteristics of the body's exposed surfaces interacting with nonuniformities in the long-wave radiant field (4). The total body surface area of the assumed person impacted by the solar load is initially estimated by A_D (15). The projected area (A_P) of an individual exposed to direct beam solar load while walking is calculated for our purposes as A_p/A_D = 0.23 (1, 2, 4, 13–16).

The effective radiant field (ERF) (1, 14, 15) is one convenient and precise measurement of the net radiant heat flux to or from the human body. ERF incorporates the summed long-wave radiation energy received by the body in a clothed state when surrounding surface temperatures are different from the air temperature. Additionally, the surrounding surface temperature may be expressed by MRT over a 4π radiating area of the body surface (14, 15) particularly with sustained marching or when surface temperatures are higher than extremities or other microclimate spaces surrounding the individual. The ERF on the human body is related to MRT by:

$$ERF = f_{eff} \cdot h_r (MRT - T_a)$$
(4a)

in which MRT is easily transformed by

$$MRT = T_a + ERF / (f_{eff} \cdot h_r)$$
(4b)

where f_{eff} , calculated as (A_r/A_D) , is the fraction of the body surface exposed to radiation from the environment; h_r includes the radiative heat transfer coefficient; and T_a is the air temperature. Typically, any transient solar load by ERF regardless whether it is direct, diffuse, or from the ground up to the individual (W/m^2) divided by the radiative coefficients $(m^2 \cdot K/W)$ increases the effective temperature (ET*15) above the prevailing ambient temperature (°C) and intensifies the heat stress as MRT rises (15, 16, 25). Gagge and Hardy (14) demonstrated that every interval of this radiative heat flux influences ERF and is linearly correlated with thermoregulatory sweating rate assessed by evaporative heat loss from body weight loss changes.

For both *trials* 6 and 7, the body surface areas of the 33 walking volunteers, as sunlight first appeared, were generally considered as being exposed to mixed diffuse, reflected, and long-wave radiation in which the $f_{eff} = 0.72$ determined using Fanger's projection factors (13). The area exposed was estimated as $0.72 \cdot A_D = 1.37 \text{ m}^2$ over a body surface of 1.9 m² for the subjects' averages. A solar elevation (β) of 45° was considered for the walks in this study (1, 2, 13, 16). Diffuse-sky and ground-reflected solar radiation (25) were assumed to be uniformly spread on one-half the exposed portion of each of the volunteer's BSA when clothed as $f_{eff} \cdot 0.95 = 0.684 \text{ m}^2$ over half of the body surface.

Because ERF incorporates the f_{eff} of the receiving individual, for this study the ERF integrates absorbed energy from long-wave (H_L) and shortwave (H_s) sources originally found in the Shapiro (42) formulation estimated as:

$$\operatorname{ERF} \cdot \alpha_{\mathrm{LW}} = \begin{bmatrix} 0.72 \cdot (0.95/1.9) \cdot (\mathbf{R}_{\mathrm{dif}} + \mathbf{R}_{\mathrm{ref}}) + \\ (0.41/1.9) \cdot \mathbf{R}_{\mathrm{D}} \end{bmatrix} \cdot \alpha_{\mathrm{SW}}$$
(5*a*)

where, for the walking individual, α_{LW} is long-wave absorptivity, $\cong 0.95$; α_{SW} is short-wave absorptivity, $\cong 0.67$ for (white) skin and military clothing (for this study $I_T = 1.26$ clo); R_D is direct beam solar radiation measured perpendicular to the beam (W/m²); R_{dif} is diffuse irradiance (W/m²) of an upward-facing horizontal surface; and R_{ref} is reflected irradiance (W/m²) of a downward-facing horizontal surface.

Since $R_D \cong$ gSL OR ($I_{TH} - R_{dif}$)/sin β , assuming I_{TH} is total solar irradiance of a horizontal surface, *Eq. 5a* can be rewritten:

$$\text{ERF} \cdot 0.95 = \left[(0.72/2) \cdot (\mathbf{R}_{\rm D} + \mathbf{R}_{\rm ref}) + (0.41/1.9 \cdot \sin\beta) (\mathbf{I}_{\rm TH} - \mathbf{R}_{\rm dif}) \mathbf{I} \cdot 0.67 \right]$$
(5b)

For the present study, from Fanger's estimates (13), $R_{\rm ref}$ was assumed to be $0.23 \cdot I_{\rm TH}$, which is the mean value of the terrain areas during the walks as solar gain (from a specific station gSL value) accumulates on the individual during the time periods.

In general, the average solar radiation load (as gSL or I_{TH}) from the various stations is not always the best approximation to quantify $E_{req,SL}$ because the lumped quantity assumes steady-state direct radiant load and each subject is generally gaining a different net gSL per time during the walk. In this study, we are interested in whole body sweat response affected by the gSL per each work/rest period.

Solar parameter estimation for transient exposures. Matthew et al. (25) extended the above solar radiation calculation approach by developing an equation that is applicable to the transient solar data of the present study data analysis. The equation can be straightforwardly migrated into various heat strain models (24, 31, 46) that input variables of MRT, ERF, and T_a or a combination of these (15, 16, 24). Extending Matthew's calculations, we developed a continuous function that integrates both H_r and H_L [from the Shapiro (42) outdoor study] and the $I_{TH} (\cong gSL)$ concept discussed above to evaluate transient solar heat load that each subject is gaining per time during a march. Our improved solution allowed us to resolve the average "constant" solar radiation variations. R_{sol} (W per person in this case) theoretically represents the best-case alternative correcting variable clothing factors and transient radiant loads by MRT and ERF (4, 15, 16). Additionally, Matthew and colleagues (25) reported that R_{sol} and ERF solutions are tightly correlated ($R^2 = 0.93$) over wide solar domains. Their separate influences can therefore be interchanged. As such, MRT that is proportional to ERF becomes a convenient index as an input into various thermal models can be easily solved from both R_{sol}, ERF, and rationally estimated from mean gSL, assuming the given weather station uses standard meteorological measuring instruments.

In the heat flow form expressed by Matthew et al. (25),

$$R_{sol} (watts) = -0.0003 \cdot (gSL)^2 + 0.681 \cdot (gSL) + 3.136$$
(6)

In the polynomial fit ($R^2 = 0.93$) of Eq. 6, MRT (°C) was derived from measurements using a pyranometer (to measure short-wave radiation fluxes) and pyrgeometer (to measure long-wave radiation fluxes). Normally, the value of the solar load differences (MRT – T_a) is the effective heat stress input parameter employed in various thermal models (1, 3, 24). This parameter may be solved in the equation to estimate solar load on the skin surface (H_{s,sk}) that is currently implemented in the USARIEM Heat Strain Decision Aid (HSDA) in which H_{s,sk} is computed as a function of various clothing factors (γ -clo and $\gamma_i = i_m$ /clo) and V_{eff} corrected for walking ["pumping" factors (4) and load carriage variables (3, 17, 24, 31, 32, 46)]. In *trials* 6 and 7, MRT was calculated by solving for the average R_{sol} and its sequel (ERF) at each marching period and time of day from the gSL collected at the various field stations. The variable I_{TH} will not be considered further.

Either R_{sol} or ERF can be utilized in the heat balance equation (as a rational variable in the heat balance equation) by combining the parameters Shapiro (42) employed to evaluate radiative short-wave (gSL, W) and long-wave (H_{Lg}, W) heat stress less radiative long-wave heat loss (H_L, W). Applying partitional calorimetric analysis (15, 16, 24), the heat balance equation (W/m²) becomes:

$$\pm S = (M - W_{ext}) - E_{sk} - (R + C) + R_{sol}$$
(7)

where S is the rate of heat storage less metabolic heat production (M) minus external work rate (W_{ext}), minus radiative (R) and convective heat loss (C), and $E_{sk} = (E - E_{res} - C_{res} - E_{dif} - m_{res})$. The variable (E) incorporates total sweat loss minus respiratory (E_{res}) and convective heat loss (C_{res}) minus skin diffusion (E_{dif}) less any metabolic heat

loss (m_{res}). The R_{sol} in *Eq.* 7 is calculated as a radiant flux (per m²). All avenues of heat exchange and respective heat transfer coefficients can be calculated as in previous studies (15, 16, 24).

The transient equation describing heat exchange between the skin surface and the radiant environment varying with time $(E_{req,sol})$ (Table 3) is therefore estimated by:

$$E_{req,sol} (W/m^2) = net heat flux - DRY +$$
(8*a*)
effective solar gain ± heat storage

$$E_{\text{req,sol}} \left(W/m^2 \right) = M_{\text{sk}} - h_{\text{r+c}} \cdot F_{\text{cl,e}} \left(\overline{T}_{\text{sk}} - T_a \right) + \left[R_{\text{sol}} \cdot F_{\text{cl,e}} \right] \pm S$$
(8b)

where M_{sk} in *Eq. 8b* now includes the net heat flux from the interior body to the skin ($M - W_{ext} - E_{res} - C_{res} - m_{res}$). The variable [$F_{cl,e}$] is the effective clothing factor determined from an articulated, movable manikin in separate analysis (4, 13, 16, 24).

In Eq. 8b, equivalent mathematical substitutions can be used assuming $R_{sol} \cong ERF = h_r \cdot (A_r/A_D) \cdot (MRT - T_a)$. The variable, $E_{req,sol}$, therefore, represents the solution of all avenues of the heat balance during transient solar loads over a given time interval. The value is substituted into the PW equation and iterated into the fuzzy piecewise analysis (44). An independent computer-generated sensitivity analysis showed that ERF (W/m²) is thermally equivalent to 0.23 · gSL for each time period of the walks where the gSL is the solar load (W/m²) as generally reported in the weather field stations. Therefore, the net solar load on the individual is optimally expressed by either R_{sol} or ERF (W/m²), and both functions can be quantified during transients in algebraically different, but equivalent heat transfer methods, as described below.

During field operations, R_{sol} (W/m²) can be calculated from 0.835 · ERF. If R_{sol} (in W/m²) is known by direct pyranometer measurements, MRT (°C) can be estimated from 0.0965 · ($R_{sol} \cdot A_D$) + T_a or vice versa if the MRT is recorded from a black or khaki-colored 6-in. (15.2 cm) globe or 4π radiometer (15, 16, 25). When roughestimated weather station gSL (W/m²) values are the only available sources, ERF can be predicted from 0.23 · gSL, and MRT can be determined from the calculated ERF as:

$$MRT(^{\circ}C) = T_a + ERF/(f_{eff} \cdot h_r)$$
(9)

Equation 9 therefore sums the effect of mixed solar radiation from direct, diffused, and ground radiant loads during a given transient solar radiation. The equation can also be used to integrate radiant exchange with the body surface when MRT differs with T_a and estimate the effect of heat storage (S) as the individual exercises over a given period of time throughout variable solar radiation intensities (15).

Heat transfer analyses. In the present study, clothing heat and evaporative potential parameters were determined using a regionally heated, articulated manikin at various wind speeds. Each element of the comprehensive heat balance equation was analyzed from the raw data, specific clothing factors by applying separate γ -coefficients for thermal and vapor resistances in an articulated, walking manikin (16, 17, 24).

The raw data were put together in a unified spreadsheet (Microsoft Excel) for later analysis. The techniques to estimate the heat transfer equations above and all other analytical equations formulated in a previous report were also applied to this study (7, 17).

Statistical analyses. Data were analyzed using a variety of statistical modules (Statistica, version 10, Tulsa, OK and STATA, College Station, TX), the latter for testing and programming specific computerized bootstrap analyses and Monte Carlo approaches (12, 33, 34, 40, 44, 45). Simple or multiple stepwise regressions analyzed the dependence between variables. Since some subjects in night *trials 1–5* were used in repeated studies, the differences between means were also analyzed using paired *t*-tests to check intraindividual sweat loss observations. For more than two tests, we used a one-way ANOVA

for repeated measures (26). Otherwise, the values were tested by unpaired *t*-tests over the various trials. The assumptions of normality and homogeneity of variance for parametric procedures were checked using Kolmogorov-Smirnov test. When the assumptions of normality or homogeneity of variance were not met, we used equivalent nonparametric tests (Kruskal-Wallis tests) for comparison of means of two independent samples (26). Following ANOVA, the data were tested using Tukey's post hoc for honestly significant differences for unpaired data or by applying a Bonferroni post hoc analysis (26).

A composite analysis was performed using pooled sweat rate data from 77 subjects completing the night marches and 550 laboratory observations from a previous study (17). The data were parsed and aggregated into a separate bootstrapping analysis to determine residual variations distinct in the original data (45). In the bootstrap analysis, the hypothesis is that a given sample $S = \{X_1, X_2, \ldots, X_n\}$ (i.e., 77 subjects from night runs) is a unique cohort of the given population $P = \{x_1, x_2, \ldots, x_N\}$, where the population includes all m_{sw} data from the original PW equation analysis (12, 17). Efron (12) developed the critical statistic, $T^*_{bs} = t(S)$ that is useful in analyses of small sample bootstrapping. This statistic supesedes the classic Student's *t* to test small departures from normality. T^*_{bs} was determined as an estimate of the corresponding population parameter $\theta =$ t(P). In this analysis, θ is assumed as a vector (bold highlight) of all parameters and T^*_{bs} the corresponding vector of estimates (12, 45).

The bootstrap analogy using Efron's criterion (12) in our prediction model analysis is to derive T^*_{bs} as high as possible; if too low (<10 or so), the S (individual m_{sw} output value) is assumed to be not very well predicted by the purported equation or contributes too large an outlier of the P (or too far out of the domain of confidence limits). The bootstrap estimate of the standard error (SE) of T^*_{bs} is subsequently determined as the square root of the bootstrap variance of T^*_{bs} as specified by Efron's criteria (12).

A bootstrapped correlation matrix was next created using output predictions generated from Monte Carlo analysis applying the principles suggested by Picard (33, 34). The Monte Carlo analysis was followed by a measure of goodness of fit of the bootstrap to explain the uncertainty for the range of values of the pooled data. The goodness of fit test that was used in our study, post Monte Carlo analysis was the Schwarz-Bayesian criteria (SBC) (40), which is a function of the natural log $[\ln(n_x)]$ of the number of observations *n*, the sum of squared errors (SSE), and the number of independent variables $k \le p + 1$ where *k* includes the intercept as shown in *Eq. 10*:

$$(SBC) = n \cdot \ln (SSE/n) + k \ln n \tag{10}$$

Equation 10 thus comprises the summed square of residuals SSE = $Sum_{(i=1 \text{ to } n)}[w_i(y_i - f_i)^2]$, where y_i is the observed m_{sw} data value and f_i is the predicted (PW) value from the fit; and w_i is the weighting applied to each data point, typically $w_i = 1$.

The bootstrapping analysis enabled determination of an estimated standard error (SE) of correlation of the modified PW equation (12), as noted above, using measured sweat rates in the new night field cohort data, assuming such data sets came from an anomalous multivariate population (12, 34) (i.e., uncertainty due to dissimilar field data tested vs. conventional indoor chamber data). Individual sweat rate values from the operational marches (*trials 1–7*) were analyzed using the data splitting technique (33). The total data set comprised all observed sweat rate values from individuals completing each trial, but *trials 1–5* (Table 1, night marches) were analyzed independently from *trials 6* and 7 (Table 2, transient solar marches). All data are expressed as means \pm SD or as means \pm 95% prediction intervals.

RESULTS

Night trials 1–5. Table 4 provides subject anthropometric characteristics, march distance, load, and selected physiologic responses for the seven trials. During *trials 4* and 5, the calculated oxygen uptake, mean weighted skin temperature,

Table 4. Kev descriptive, environmental, and physiological data from held experiments used in curr	eriments used in current validation
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Trial	Ta, °C	Pw, kPa	V, m/s	Distance, km	Load, kg; L/mass, %	BSA, m ²	Body Mass, kg	$\bar{T}_{sk},^{\circ}C$	Vo2, 1/min	SR, 1/h
1	25.1	2.28	0.6	24.0	$30.9 \pm 6.7; 40.4 \pm 8.6\%$	1.94 ± 0.09	76.7 ± 5.5	33.81 ± 0.26	2.42 ± 0.21	1.02 ± 0.21
2	20.8	1.95	0.5	29.0	$30.4 \pm 7.2; 40.2 \pm 10.7\%$	1.94 ± 0.13	77.5 ± 9.7	31.29 ± 0.41	2.43 ± 0.18	0.97 ± 0.22
3	17.4	1.30	1.3	37.0	$35.2 \pm 5.9; 45.8 \pm 8.1\%$	1.94 ± 0.13	77.4 ± 9.5	29.17 ± 0.67	2.72 ± 0.30	0.72 ± 0.23
4	17.4	1.17	0.9	14.0	$15.1 \pm 4.5; 21.5 \pm 5.1\%$	1.85 ± 0.10	69.9 ± 6.2	29.76 ± 0.93	1.84 ± 0.21	0.57 ± 0.16
5	20.0	1.65	1.1	14.0	$17.0 \pm 3.3; 24.4 \pm 3.5\%$	1.85 ± 0.10	69.7 ± 6.3	30.91 ± 0.58	2.16 ± 0.21	0.68 ± 0.18
6	25.9	1.81	1.3	16.4	$15.3 \pm 4.3; 21.1 \pm 6.3\%$	1.89 ± 0.18	73.7 ± 10.8	33.11 ± 0.33	1.69 ± 0.23	0.99 ± 0.17
7	16.2	0.94	1.4	18.3	$21.0 \pm 8.2; 30.8 \pm 11.3\%$	1.83 ± 0.10	67.9 ± 6.4	29.30 ± 0.96	1.68 ± 0.22	0.61 ± 0.14

All data are means \pm SD. Air temperature (T_a), ambient air movement (V), ambient water vapor pressure (Pw), distance traversed (km), load carried (L, kg), body surface area (BSA), body mass (kg), mean skin temperature (\overline{T}_{sk}), and observed sweating rate (SR) are end values.

and absolute sweat loss values were lower (P < 0.01) compared with mean values in *trials 1* and 2 (Table 4). The loads carried during *trials 1, 2,* and 3 were larger (P < 0.01) than the other trials. The load (L)/body mass (L/kg × 100) percentage carried in *trials 1, 2,* and 3 (ranges 40–46%, P < 0.05) was higher than %L/body mass apparent in the other two night trials.

Table 5 provides measured sweat rates for the night *trials 1*–5, the respective PW output (17), and the Shapiro (41) predicted m_{sw} values. The average deviation of each prediction output compared with measured sweat rate is provided (Δ of model – measured). For all night trials, the deviation from PW output values was not different from the measured sweat rates (mean \pm SD = 28 \pm 9.6 g·m⁻²·h⁻¹ for *trials 1*–5). For all night trials, the Shapiro (41) values deviation was greater (P < 0.01 to P < 0.001) than the measured sweat rates.

Figure 1 presents the bootstrap analysis of the PW output values (as dependent variable) plotted against measured sweat rates for *trials* 1-5 (77 experiments) and the previously collected laboratory data (17). The analysis employed analytic procedures using the bootstrap analysis on matched residual variances as described in METHODS (33, 45). This analysis incorporates E_{req} and E_{max} parameters implemented from PW prediction of m_{sw} . Thus the present study data served for both prediction and cross-validation of the original fitted PW equation (17, 33).

The bootstrap parameter regression of this analysis is shown in Fig. 1. The sweat rates calculated from the heat exchange variables (E_{req} and E_{max}) of *trials* 1–5 aggregated (closed triangles) with the PW equation vs. the sweat rates from the ARIEM lab data (open circles) had outliers that predicted lower than the 95% prediction line in 9 cases ($\approx 1.5\%$ of over 550 data points). Conversely, there were 12 cases of outliers predicting m_{sw} higher than 95% confidence limit ($\approx 2\%$ of the total data points). The higher predicted sweat rates are within the domain of variability of the bootstrapping variances inherent in the PW algorithm (12, 45) and the whole regression equation displayed a SEE = $\pm 69.2 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$. After 1,000 iterations, the bootstrap correlation (rbs) parameter estimate defaulted to 0.81 with a standard error of the β -correlation coefficient of ± 0.014 [Efron's (12) T^*_{bs} -value = 31.3, P < 0.0001] for the pooled data. The data now include field night run data that were combined with the original laboratory experiments. The sweat rate data exhibited essentially no heteroscedasticity (unequal variances among the groups) (26, 33, 34, 45). Following the bootstrapping analysis, a Monte Carlo parsing (34) was next executed on the combined data set to determine the optimal model selection based on an uncertainty goodness of fit of the PW equation using SBC. For the final Monte Carlo iterations, a SBC of 0.725 was derived (1 = perfect fit to the data) that suggests that the PW model using all combined data values (night + laboratory studies) still exhibits small residual random error components (0.275). As previously mentioned, a greater proportion of variance causing over- or underprediction errors is still accounted for in the lumped proportional control (β -coefficients) parameters present in the original fuzzy piecewise (PW) model (17). The data fit also conformed with the less robust Ordinary Least Squares (OLS) (r = 0.71, P < 0.001) and confirms that sweat loss prediction using the PW model was not adversely limited by any outliers changing the gain algorithm (β -coefficients) in the model prediction structure due to too high or too low sweat rates among the subjects during the various trials 1-5 (26, 33, 46). We next analyzed sweat rates in the marches where solar load was apparent.

Transient solar radiation trials 6–7. Table 4 displays the subject anthropometric characteristics, load, and selected physiologic responses for *trials* 6 and 7. In *trial* 6, 20 subjects began marching at 0330, with explicit solar gain appearing at 0500 and terminating with a maximum global solar load (gSL) of 341 W/m². During this march, T_a was 25.9°C but the effective heat stress gain owing to the increased MRT was 35.9°C. As shown in Table 2, *trial* 6 was a scenario that comprised two marching tasks up a mountainous gravel road (median terrain

Table 5. Measured sweat rate compared with predicted output during night marches of trials 1–5

	Trial 1	Trial 2	Trial 3	Trial 4	Trial 5
No. of subjects	13	12	12	20	20
SR, $g \cdot m^{-2} \cdot h^{-1}$	524 ± 96	502 ± 121	366 ± 104	307 ± 84	367 ± 96
PW prediction (Ref. 17)	493 ± 75	489 ± 55	405 ± 41	338 ± 28	393 ± 60
Shapiro prediction (Ref. 41)	854 ± 113	847 ± 106	752 ± 42	636 ± 30	727 ± 101
$\Delta(PW - SR)$	31	13	39	31	26
Δ (Shapiro – SR)	330*	345*	386†	329*	360†

Values are means \pm SD. Comparison of average deviation Δ of model output to actual sweat rate (SR): *P < 0.01; $\dagger P < 0.001$; Δ (PW - SR) in all other trials, not significant.



Fig. 1. PW prediction plotted as a function of sweat rate during night *trials* 1–5 (closed triangles) aggregated with previous laboratory results (open circles) (17). Data include bootstrapping correlation, $r_{\rm BS}$ (12, 34, 45); solid line is the identity line, PW = sweat rate. The bootstrap estimate of standard error (SE) for the pooled data was ± 0.014 with a $\mathbf{T}^*_{\rm b} = 31$ (12). The standard error estimate of the regression (SEE) was $\pm 69.2 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$. Typically, once the original fuzzy piecewise PW equation is applied (17, 44), this output value can be substituted in the above OLS equation (125 + 0.67 · PW) to calculate the m_{sw} required; for example, 600 g · m⁻² · h⁻¹ determined from the equation yields 522 g · m⁻² · h⁻¹ m_{sw}, within the 95% prediction interval of the boot strap. These data now include field night runs combined with the original lab experiments.

coefficient, $\eta = 1.3$) with work/rest cycles of 65 min work and 18 min rest followed by another march of 48 min work/15 min, and concluding with a resting period of 62 min. Total exposure time to the transient solar load was 208 min.

In *trial* 7, 13 subjects marched on a mixed paved and gravel road ($\eta = 1.25$). These marches began at 1420 at which time maximum global solar load (gSL) was 612 W/m². During this march, T_a was 16.2°C and the resulting MRT was 26.2°C. The work/rest marches in *trial* 7 continued until 1800 at which time solar load reached a nadir with minimal or no solar load. *Trial* 7 comprised 220 min of exposure to a transient solar load which had two separate marches with work/rest cycles that included 58 min work/15 min rest and another session that was 71 min work/14 min rest, followed by a final resting phase of 62 min.

Figure 2 shows the mean (\pm SD) solar radiation (W/m²) as a function of time of day during the marches using R_{sol} derived from gSL for *trials* 6 and 7. The MRT calculated from R_{sol} and ERF increased from a value of 25.7°C to as high a 50°C during *trial* 6, and decreased from 58°C to as low as 16.1°C during *trial* 7. R_{sol} and ERF as explained in METHODS incorporated each timed output to determine E_{req} and E_{max} for later input in the modified PW prediction equation in *trials* 6 and 7.

Based on E_{req} and E_{max} adjustments using R_{sol} , MRT, and V_{eff} calculated for the transient solar-night trials, a revised PW ($\dot{P}w$,sol) ordinary least squares (OLS) equation for transient solar radiation conditions was developed [$m_{sw} = 0.72 \cdot (\dot{P}w$,sol) + 135], where $\dot{P}w$,sol reflects the original PW equation (17) with E_{req} now modified to include R_{sol} ($E_{req,sol}$). The value of $E_{req,sol}$ must be first determined by pertinent solar coefficients. Table 6 provides the results of a multiple regression analysis conducted using sweat rate (dependent variable) from each of subjects completing *trial* 6 and 7. The output of

three prediction equations were compared: 1) Pw,sol as developed in the current analysis; 2) Shapiro (42), which has been discussed; and 3) HSDA, which is often used by the military to predict sweat rate for outdoor activities (3, 31). The magnitude of the β -coefficients for each prediction equation describes the relative contribution of each independent variable in the prediction of sweat rate. Table 6 indicates that Pw,sol had the highest β -coefficients and was the only equation that accounted for significant (P < 0.0001) variance contributions from each predictor variable in the orthogonal correlation structure of the multiple regression analysis (26). The Pw, sol output was also significantly correlated with measured sweat rates from the pooled transient solar experiments. Figure 3 also presents output showing the OLS analysis of the predictability of *Pw*,sol output values (here plotted as the independent variable) and measured m_{sw} for trials 6 and 7. A significant correlation (r = 0.96; P < 0.001) and SEE $(\pm 33.8 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1})$ were detected. Once the equation is solved for the various independent variables in the heat exchange, the model output appears as a simple, practical tool in prediction of m_{sw} for a given transient solar load.

Additional data exploration. Further investigation of the combined data allowed modification of the laboratory-derived



Fig. 2. R_{sol} output values (25) plotted vs. time of day during the transient solar experiments of *trial* 6 (top panel) and *trial* 7 (bottom panel). Saw-toothed dips in R_{sol} of *trial* 6 are due to mixed cloud formation impacting the solar flux in some trials.

Model Equation	β*	SE of β^*	β	SE of β	<i>t</i> (23)	<i>P</i> <
HSDA	-0.020	0.062	-0.113	0.350	-0.32	0.748
Pw,sol	0.929	0.066	0.66	0.047	14.05	0.0001
Shap_out (Ref. 42)	0.066	0.075	0.21	0.240	0.87	0.391

Table 6. Multiple regression of sweat rate $(g \cdot m^{-2} \cdot h^{-1})$ vs. output from Shapiro equation (Ref. 42) (Shap_out), Heat Strain Decision Aid (Refs. 3, 31) (HSDA), and PW, sol equation for pooled data from the transient solar trials 6 and 7

 β * is standardized regression coefficient; β is raw regression coefficient; magnitude of β coefficients compares relative contribution of each independent variable in prediction of the sweat rate for each subject. HSDA out (Refs. 3, 31) and Shap_out (Ref. 42) equations were not good predictors of sweat rate (P > 0.05, NS) for the transient solar experiments. N = 33 subjects.

PW equation with a focus on cool environments during resting or low metabolic activities. Cool (<16–18°C) ambient temperatures result in low skin wettedness, ($\omega \le 0.15$) with water loss primarily from skin diffusion (5, 15, 19, 22). This effect takes place often when E_{max} is $\ge 400 \text{ g} \cdot \text{m}^{-2} \cdot \text{h}^{-1}$ (approximately >270 W/m²) and/or E_{req} becomes <50 g $\cdot \text{m}^{-2} \cdot \text{h}^{-1}$ (13, 20, 22, 41). In such environments, the equation to predict sweat rates (within 131 g $\cdot \text{m}^{-2} \cdot \text{h}^{-1}$ of actual values) can now be determined from the following:

The above equation does not alter the β -coefficients (algorithm gain) from the original PW equation but increases the intercept by 203 g·m⁻²·h⁻¹ when E_{req} is low, but E_{max} is high. Therefore, for the E_{req} and E_{max} mentioned, *Eq. 10* predicts m_{sw} = \sim 2.5 g/min occurring with elevated wind speeds during laboratory and night (limited outdoor field) experiments.

DISCUSSION

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This study validated a previously developed sweat rate prediction equation and derived pertinent biophysical-physiological corrections to modify that equation for the valid prediction of sweat rate (water needs) during transient solar radiation and cool conditions. The new \dot{P} w,sol and PW,cool equations have important implications for military and disaster relief planning and a variety of other occupational problems related to the logistical planning for water needs. We also



Fig. 3. Sweat rate from *trials* 6 and 7 plotted as a function of \dot{P} w,sol equation derived from heat exchange parameters following analytical solution of $E_{req, sol}$ as explained in text.

demonstrated that several other often used sweat prediction equations, for outside activities with a solar radiation, were far less accurate compared with the modified \dot{P} w,sol equation.

During the transient solar experiments, we observed high sweat rates, despite the low ambient temperatures, due to the impact of the solar gain quantified by elevated MRT. Even though load carriage and metabolic level would be considered nominal, the ambient temperatures ($T_a = 25.9^{\circ}C$ in *trial* 6 and 16.2°C in trial 7) were influenced by the added rise in MRT that exacerbated the sweat rates found in *trial* 6 compared with the values in trial 7. During the transient solar gain, average sweat rates calculated from the 20 individuals in trial 6 were 523.4 g·m⁻²·h⁻¹ (\pm 73.6 SD), compared with 332.5 $g \cdot m^{-2} \cdot h^{-1}$ (±69.4 SD) in the 13 individuals of *trial* 7 (58%) increase, P < 0.001, nonpaired t = 7.45). These values amount to some 16.6 g/min higher sweat rates observed in trial 6 vs. 10.5 g/min in trial 7. The necessary water requirements to sustain such sweat rates to maintain thermoregulation are greatly increased by the solar impact (ERF and MRT) during the walks despite the mild ambient conditions. Interestingly a constant cool ambient temperature (as in trial 7; Table 4), reducing solar radiation from a maximum (612 W/m^2) in the late afternoon to zero at night, markedly reduced sweat rates (and water needs, respectively) compared with early morning marches in which solar load gradually accumulates with a moderate air temperature. These findings are consistent with Gagge and Hardy (14) who first observed that thermoregulatory sweating (evaporative heat loss) changes were highly correlated with ERF altered by short bursts of infrared heating (heat flux from IR quartz lamps) at $T_a = 23-24$ °C. They also proved that as ERF increased monotonically at each higher constant ambient temperature (from 9°C to 30°C), the evaporative heat loss by sweating increased proportionately. Nielsen et al. (30) also showed similar high sweat rates during outdoor cycle exercise in the sun.

The present study confirmed our initial hypothesis that sweat rate predictive equations developed from laboratory studies (17) are suitable for matching sweat requirements (or at least were not statistically overpredictive; i.e., SEE < \pm 70 g·m⁻²·h⁻¹) to actual sweat loss for disparate military activities during the night time. This was an anticipated finding since the experiments involved similar conditions (T_a, RH, clothing thermal resistance values, and work rates) as in previous environmental chamber studies (7, 17). Additionally, the major finding from the present study was improvement of a sweat loss prediction equation for transient solar loads quantified by R_{sol}, ERF, and MRT. To our knowledge, this has not been possible before and may require additional investigation particularly at higher ambient (hot dry and tropical) environments.

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Most experiments that involve solar load challenges in humans are done during constant thermal radiation exposures and brief time periods (14, 30). In that respect, the avenues of heat exchange (E_{req} and E_{max}) are assumed as being under steady-state conditions. Our data analysis shows that R_{sol} as a variable input into the heat balance equations can be used for estimating sweating during transient solar environments.

The prediction equations for estimating sweat rates using R_{sol} garnered from the present experiments are an important new finding because they include persistent effects of heat storage (S) as core and skin temperatures increase (37) and thereby integrate complex solar environments more rigorously than previous investigations (4, 42). We also derived by exploration of present and past (17, 41) data sets, an adjusted PW equation (PW,cool) that is applicable for cooler weather conditions when PW might predict negative sweating values because E_{req} is too low or E_{max} is too high. The adjustment requires only a change to the legacy PW equation intercept term. We recommend that these new equations should be included in current thermal models (3, 24, 46) especially for field use when solar load is present. Fundamentally, once the various discrete parameters (V_{eff}, R_{sol}, i_m/clo, etc.) influencing dynamic clothing heat transfer and walking factors are quantified into the heat balance determining E_{req} and E_{max} , the *P*w,sol equation is valid in predicting m_{sw} (within an SEE \pm 34 $g \cdot m^{-2} \cdot h^{-1}$ or 1.1 g/min of actual sweat rate values or predicting fluid needs $\approx \pm 0.1$ liter/h) (Fig. 3). The approximation is a best case prediction scenario possible in field studies that is limited by the domain of thermal environments, metabolic intensities, and clothing ensembles studied here considering the sweat rate variability of a general population (18).

Water needs are currently estimated for the US military using HSDA or similar approaches (3, 21, 23, 28). Our past (7, 17) and this study clearly demonstrate that the PW equations provide for more accurate predictions of sweat rates during various exercise intensities and environments. A caveat of the HSDA guideline is that the input value for skin temperature executed in the calculation of dry heat loss (R + C) is determined by a fixed value of 36.5°C [skin saturation vapor pressure of 45 Torr (5.99 kPa)] rather than actual values as used in this study. Furthermore, the H_{s,sk} values employed that determine MRT in that guideline are highly sensitive to fluctuations (γ -values) occurring in a variety of thermal and vapor resistances (20, 22, 24) as determined using thermal manikins. For example, Table 6 showed that calculation of the H_{s.sk} factor in the HSDA model (3) did not predict sweat rates reliably during the transient solar trials in this study. One reason may be because H_{s,sk} is a collective equation in the HSDA empirical model that incorporates MRT, but is coupled to arbitrary clothing and air movement coefficients (3). Therefore, any derived sweat loss prediction can therefore be too high or too low based on the inaccuracies of the $H_{s,sk}$ factor. A new rational multimodel also demonstrated large residuals even when applied to group data (46). The variety of equations: PW, Pw,sol, and PW,cool could be implemented in various model input interfaces (for example by using a Boolean logic "doloop" contingency) when T_a is less than 20°C, solar load is present, wind movement is high, or cloudy outdoor activity is planned (provided all Ereq/Emax caveats and domain of validity are upheld).

In summary, we performed a series of outdoor military field studies in which sweat rate was quantified in 110 soldiers exercising during night trials and during transient solar radiation conditions. We validated our recently published sweat rate prediction equation (17) for outdoor military activities and modified it so it predicts m_{sw} accurately for transient solar radiation and cooler ambient conditions. We compared our PW sweat prediction equations to other existing predictions equations and established that PW was an improved calculation readily applicable during field training exercises with (Pw,sol), without (original PW) transient solar loads, and finally when environmental conditions embrace low Ereq and high Emax capacities (PW,cool) during moderate exercise intensities. The family of PW sweat prediction equations allows easy implementation tools in civilian, sports, and military medicine communities needed to estimate water needs during a variety of heat stress/exercise conditions.

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AUTHOR CONTRIBUTIONS

Author contributions: R.R.G., S.N.C., D.S.M., A.H., and M.N.S. conception and design of research; R.R.G., B.R.E., D.S.M., A.H., T.L.E., and M.N.S. analyzed data; R.R.G., S.N.C., B.R.E., D.S.M., A.H., T.L.E., and M.N.S. interpreted results of experiments; R.R.G. prepared figures; R.R.G., S.N.C., and M.N.S. drafted manuscript; R.R.G., S.N.C., B.R.E., D.S.M., A.H., T.L.E., and M.N.S. edited and revised manuscript; R.R.G., S.N.C., B.R.E., D.S.M., A.H., T.L.E., and M.N.S. approved final version of manuscript; S.N.C., B.R.E., D.S.M., A.H., and T.L.E. performed experiments.

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