



# NAVAL MEDICAL RESEARCH UNIT SAN ANTONIO

# A TWO-STEP PHAGE DISPLAY PANNING METHOD FOR SELECTING PEPTIDES TO DETECT HMGB1 AND ITS POTENTIAL FOR DEVELOPING PEPTIDE-BASED BIOSENSORS

DAVID J. LEMON, AMANDA M. BACHE, HOLLY C. MAY, STEVEN X. MOFFETT, EUN Y. HUH, APRIL A. FORD, AND YOON Y. HWANG PHD

MAXILLOFACIAL INJURY AND DISEASE DEPARTMENT CRANIOFACIAL HEALTH AND RESTORATIVE MEDICINE

# NAMRU-SA REPORT # 2020-604

Approved for public release; distribution is unlimited

## **DECLARATION OF INTEREST**

The views expressed in this article are those of the authors and do not necessarily reflect the official policy or position of the Department of the Navy, Department of Defense, nor the U.S. Government. This work was funded by the Naval Medical Research Center's Advanced Medical Development Program using work unit number G1722. Authors are employees of the U.S. Government. This work was prepared as part of their official duties. Title 17 USC §105 provides that 'copyright protection under this title is not available for any work of the US Government.' Title 17 USC §101 defines a US Government work as a work prepared by a military service member or employee of the US Government as part of that person's official duties.

This project was supported in part by an appointment to the Naval Research Enterprise Internship Program, administered by the Office of Naval Research.

#### REVIEWED AND APPROVED BY:

CARDIN.SYLVAIN.1289083940 Date: 2020.12.31 10:46:32 -06'00'

Sylvain Cardin, PhD Chair, Scientific Review Board Chief Science Director Naval Medical Research Unit San Antonio 3650 Chambers Pass, BLDG 3610 Fort Sam Houston, TX 78234-6315

## VAUGHN.ANDR Digitally signed by VAUGHN.ANDREW.F.117 EW.F.11717310 42 Date: 2021.01.14 11:06:36 -06'00'

CAPT Andrew F. Vaughn, MC, USN Commanding Officer Naval Medical Research Unit San Antonio 3650 Chambers Pass, BLDG 3610 Fort Sam Houston, TX 78234-6315 Date

Date

# TABLE OF CONTENTS

ABBREVIATIONS	
EXECUTIVE SUMMARY	6
INTRODUCTION	7
MATERIALS AND METHODS	
Results	
DISCUSSION	
MILITARY SIGNIFICANCE	
References	
Figures	

# **ABBREVIATIONS**

μl	Microliter
°C	Degrees Celsius
1°	Primary
2°	Secondary
DMSO	Dimethyl sulfoxide
DNA	Deoxyribonucleic acid
E. coli	Escherichia coli
EDTA	Ethylenediaminetetraacetic acid
ELISA	Enzyme-linked immunosorbent assay
HMGB1	High Mobility Group Box 1
HRP	Horseradish peroxidase
IPTG	Isopropyl β-d-1-thiogalactopyranoside
М	Molar
mM	Millimolar
NNK	Nucleic acid code for two of any base pair (NN) and one guanine or thymine (K)
OD450	Optical density for light with wavelength 450 nanometers
OD <sub>600</sub>	Optical density for light with wavelength 600 nanometers
PBS	Phosphate buffered saline
PFU	Plaque-forming units
pН	Negative of the base 10 logarithm of the activity of the hydrogen (H) ion
RCF	Relative centrifugal field
RPM	Rotations per minute
S+	With affinity for saliva

S-	With no affinity for saliva
S+H+	With affinity for both saliva and HMGB1
S+H-	With affinity for saliva and not for HMGB1
S-H+	Without affinity for saliva and with affinity for HMGB1
S-H-	Without affinity for saliva or HMGB1
SAW	Surface acoustic wave
TBST	Tris-buffered saline with polysorbate 20 (Tween)
X-gal	5-bromo-4-chloro-3indoyl-β-D-galactopyranoside

#### **EXECUTIVE SUMMARY**

**Background:** Expeditionary and deployed personnel are exposed to the widest variety of biological, chemical, environmental, and biomedical threats. Biosensors, devices that combine a biological element with a technological sensor platform to detect an analyte, have great promise and are urgently needed to detect and identify threats in real-time. Unfortunately, biosensors are hampered by a historical reliance upon animal-generated antibodies as their biological recognition elements. Antibody production and characterization are slow, difficult, and sequential processes that rely upon inducing an immune response in a laboratory animal. **Objective:** We characterized an alternative method for producing biological recognition elements: phage display leverages small viruses (bacteriophages) which display short, random peptides. We intended to develop a phage panning protocol that excludes phages with peptides that bind a background solution and collects only those which bind a desired analyte.

**Methods:** Phage panning was conducted by a two-step method where phages which bound to the background solution (human saliva) were excluded before the remaining phage pool was panned again to collect only those which bound the analyte (recombinant human high mobility group box 1 protein). Phages collected by this scheme were then amplified, tested for affinity to the analyte, and sequenced to determine the identity of their displayed peptide.

**Results:** The phage panning scheme collects phages that do not bind the background solution, but do have a high affinity for the selected analyte. These phages bound the analyte with even greater affinity when presented with the analyte in the background solution. The peptides displayed on these phages are all unique and have no conserved motifs, secondary structures, or hydrophobic regions.

**Conclusions:** This two-step panning scheme can be tuned to include almost any analyte or background solution. It produces many unique peptides with desirable characteristics for use as biological detection elements in biosensors. The entire pipeline can be completed in approximately ten weeks and the peptides it yields have many advantages as recognition elements in biosensors when compared to more traditional, antibody-based elements.

#### INTRODUCTION

Deployed or expeditionary forces are necessarily at risk, but some risks are easier to identify than others. In situations where military personnel may contact natural or weaponized bacterial pathogens, lethal viruses, or toxic and debilitating chemicals, there is an urgent need to detect and identify these hazards immediately. This is especially true with viral and bacterial pathogens (Centers for Disease Control and Prevention, 2018), that are invisible to the naked eye and can cause harm with only a small number of particles (Lonsdale, Taba et al. 2013). Biosensors, devices that use a biological element (*e.g.* cells, enzymes, antibodies, peptides, or DNA aptamers) to detect the presence of an analyte, are a common tool for identifying these types of hazards (Walper, Lasarte Aragones et al. 2018).

Biosensors combine a peptide, antibody, enzyme, etc. biorecognition element with a sensing platform that can detect and quantify the biorecognition element's signal. An ideal biosensor is one that is: (1) label-free, meaning that it recognizes the analyte directly and without some added fluorophore, dye, or other marker, (2) real-time, meaning that it measures the analyte and reports its findings immediately, (3) rugged or fieldable, (4) accurate and precise, and (5) simple to operate, read, and produces an actionable output (Drake and Levine 2005, Coimbatore, Presley et al. 2008, Shabani, Zourob et al. 2008, Ahmed, Rushworth et al. 2014).

Unfortunately, antibodies, the typical biorecognition element for many biosensors, have several problems that make these sensors less than ideal (Coimbatore, Presley et al. 2008, Tolba, Ahmed et al. 2012). First, antibodies are generated in animals, which means they will not be useful against any highly toxic or contagious analytes, since these may kill or harm the animal before the antibodies could be produced (Wesolowski, Alzogaray et al. 2009, Walper, Anderson et al. 2012, Rahim, Wang et al. 2019). Antibodies are often used with other labels, secondary antibodies, and after sample processing steps (Soelberg, Stevens et al. 2009, Billingsley, Riley et al. 2017, Selvam, Wangzhou et al. 2017), making them not label-free. Also, antibodies are relatively massive when compared to aptamers or peptides, which can lead to off-target binding (Mukundan, Kumar et al. 2012) and signal-to-noise problems in some detector types. Finally, antibodies often degrade and lose their affinity for the analyte in temperatures outside a narrow range (Walper, Lee et al. 2013, Raina, Sharma et al. 2015), so they may not be rugged enough for field use. Our approach to address the problems of antibodies as biorecognition elements

(Walper, Lasarte Aragones et al. 2018) is to use phage display-derived peptides (Goldman, Pazirandeh et al. 2000) to bind and recognize a specific hazard.

Phage display is the technique of inserting the sequence for a short protein, also called a peptide, into one of the genes coding for an exterior protein of a bacteriophage virus (Tikunova and Morozova 2009). These bacteriophages (phages) display the inserted peptide on their viral coat. A phage display library is created by inserting randomized peptides into a large collection of phages (Ledsgaard, Kilstrup et al. 2018). These libraries can then be screened, or "panned," against any desired analyte to isolate only phages with peptides that have affinity for the analyte selected (positive panning) (Fralick, Chadha-Mohanty et al. 2008). Panning can also be done to exclude any phages with peptides that have affinity for a sample (negative panning), for example whole blood (Arap, Kolonin et al. 2002) or saliva.

We developed a two-step approach for phage display panning. First, we panned the phage library against whole human saliva to exclude any phages with peptides that have affinity for saliva. Next, we panned the non-saliva binding fraction of the phage library against human High Mobility Group Box 1 (HMGB1), a potential biomarker for traumatic brain and cranial nerve injuries (VanPatten and Al-Abed 2017, Aucott, Lundberg et al. 2018, Paudel, Shaikh et al. 2018), and collected the fraction that bound HMGB1. This gave us a pool of phages with peptides that have affinity for HMGB1, but no affinity for human saliva to use as a proof-ofconcept for our two-step panning approach. These phages bind the selected analyte (HMGB1) in vitro even in the presence of the background solution (saliva). We tested several phages and found many displayed increased affinity for their analyte when the background solution is present. These phages were all distinct from one another, suggesting our approach is a rapid and simple way to isolate large pools of phages with unique peptides that bind only the analyte selected and not a pre-screened background solution. This approach is much faster and less expensive than antibody production, and its peptide products are easier to modify than antibodies. It also has the benefit of not requiring an animal or successful immune response to generate large numbers of useful peptides for biorecognition elements in much-needed biosensors.

#### **MATERIALS AND METHODS**

### Materials

*Tubing*. Microcap capillary micropipettes (32 mm, Drummond Scientific Company, Broomall, PA) and 0.8 mm bore  $\times$  1.6 mm wall, size #13 Marprene tubing (Watson-Marlow, Wilmington, MA) were used during phage panning.

*Equipment*. A Pumpdrive 5201 peristaltic pump (Heidolph, Schwabach, Germany) was used for phage panning. A 50TS microplate washer (BioTek, Winooski, VT) and a Synergy H1 hybrid plate reader (BioTek) were used during the enzyme-linked immunosorbent assays. Two centrifuges were used; a benchtop 5430R microcentrifuge (Eppendorf, Hamburg, Germany) for slower spins at 4,300 ×relative centrifugal field (RCF) and a Avanti JXN-30 high-speed centrifuge (Beckman Coulter, Brea, CA) for faster spins at 20,800 ×RCF.

*Bacteria and phage propagation.* A Ph.D.-12 commercial phage display library kit (New England BioLabs, Ipswich, MA) provided all phages and the *Escherichia coli* ER2738 K12 host bacterial strain. All bacterial cultures were grown in Luria-Bertani liquid medium (1% tryptone, 1% sodium chloride, 0.5% yeast extract by weight).

### **Procedures**

*Phage display panning – crosslinking panning target to microcapillary tube interior*: Panning procedures were conducted as previously reported by Titus et al. (Titus, Kay et al. 2017) with some modifications. Acetone was wicked into a 10 μl microcapillary tube (32 mm Microcap capillary micropipette, Drummond Scientific Company, Broomall, PA) to clean it, then wicked away with a paper tissue. After the tube air dried for 30 minutes, freshly prepared 2% aminosilane in acetone was wicked into the tube and incubated at room temperature. After 30 seconds, the aminosilane solution was wicked out of the tube and the tube was allowed to air dry for at least 30 minutes. Next, freshly prepared 10 mM sulfo-LC-SPDP (sulfosuccinimidyl 6-(3'- (2-pyridyldithio)propionamido)hexanoate, ThermoFisher Scientific, Waltham, MA) in 1×phosphate buffered saline (PBS) + 10 mM ethylenediaminetetraacetic acid (EDTA) was wicked into the capillary tube and incubated at room temperature for one hour. The tube was rinsed twice by wicking with 1×PBS + 10 mM EDTA before the panning target solution, HMGB1 (recombinant human HMGB1 protein CF, R&D Systems, Minneapolis, MN) or whole human saliva (saliva, normal, pooled human donors, Lee Biosolutions, Maryland Heights, MO) diluted in PBS, was wicked into the tube and incubated overnight in a humidified container at 4 °C. The following day, the panning target solution was wicked out and the tube was again rinsed twice with  $1 \times PBS + 10$  mM EDTA before proceeding to phage library recirculation.

*Phage display panning – phage library recirculation*: One end of the microcapillary tube with the panning target crosslinked to its interior surface was mated with tubing (Marprene Tubing, 0.8 mm bore  $\times$  1.6 mm wall, size #13, Watson-Marlow, Wilmington, MA) and the entire assembly was rinsed with 250 µl 70% ethanol from one end by peristaltic pump (Pumpdrive 5201, Heidolph, Schwabach, Germany) at 20 rotations per minute (RPM). The assembly was air dried for 30 minutes at 5 RPM then rinsed with 1×PBS + 10 mM EDTA and filled with blocking buffer (SuperBlock, ThermoFisher Scientific, Waltham, MA). The blocking buffer was incubated for one hour at 4 °C then drained at 5 RPM, and 1.5 ml tris-buffered saline with 0.1% polysorbate 20 detergent (TBST) was washed through the tubing and microcapillary assembly at 5 RPM. The phage display library (Ph.D.-12 Phage Display Peptide Library, New England BioLabs, Ipswich, MA) was diluted 1:100 in TBST and approximately 250 µl was used to completely fill the assembly. The other end of the microcapillary tube was mated with the tubing and the phage library was recirculated at room temperature for one hour at 5 RPM.

After recirculation, the binding fraction (the portion with phages with high affinity for the crosslinked analyte) was adsorbed on the interior surface of the microcapillary tube while the non-binding fraction (the portion with phages with low or no affinity for the crosslinked analyte) remained in circulation. The non-binding fraction was collected, then the assembly was rinsed with 2.5 ml TBST. The binding fraction was collected by filling the assembly with 0.2 M glycine hydrogen chloride (pH 2.2) elution buffer and recirculating it at room temperature for ten minutes at 5 RPM. The binding fraction was collected in a clean tube and neutralized with 17 µl tris-buffered saline pH 9.2. This binding fraction was stored at 4 °C for up to two weeks or at -20 °C for longer if needed.

We used a two-step panning scheme (Figure 1). First, the phage library was recirculated through a microcapillary tube with a biological background solution (whole human saliva) crosslinked to its interior surface. After panning, two fractions were collected. The non-binding fraction contained phages with low or no affinity for the saliva, the biological background solution (S- phages). The binding fraction contained phages with high affinity for saliva, the biological background solution (S+ phages). Each fraction was panned again, through a

microcapillary tube with the desired analyte (HMGB1) crosslinked to its interior surface. This yielded four fractions: the S+ phages without affinity for the analyte (S+H-), the S+ phages with affinity for the analyte (S+H+), the S- phages without affinity for the analyte (S-H-), and the S-phages with affinity for the analyte (S-H+). The S+H+ fraction was retained for use as a positive control. The S-H- fraction was retained for use as a negative control. The S-H+ fraction was retained for future use as biorecognition elements for detecting the analyte (HMGB1) in a biological background solution (saliva). All three fractions were separated into individual phage clones, amplified, titered, and characterized.

*Isolating individual phage clones*: Non-binding and binding fractions from phage display panning contain many, many individual phages. To amplify and characterize an individual phage, it must first be isolated from the others. We used the double agar overlay technique to separate phages from each other and identify individual phage clones. First, an overnight culture of ER2738 K12 E. coli started the day prior was subcultured by adding fresh media in a 1:1 ratio and further incubating at 37 °C with shaking. After 30 minutes to one hour, the culture's OD<sub>600</sub> was measured, the bacterial cells were spun down at 4,300 ×RCF for 5 to 10 minutes at room temperature and resuspended in sterile media to OD<sub>600</sub> 0.4 to 0.6. The phage display fraction was serially diluted in sterile media from  $10^{-1}$  × to  $10^{-12}$  × its original concentration. Next, 3 µl of 5% isopropyl β-d-1-thiogalactopyranoside (IPTG) and 4% 5-bromo-4-chloro-3indoyl-β-Dgalactopyranoside (X-gal) in dimethyl sulfoxide (DMSO) (ChromoMax IPTG/X-Gal solution, Fisher Scientific, Waltham, MA) and 250 µl resuspended bacterial culture were added to 100 µl of the diluted phage fraction. This entire mixture was then added to 3.5 ml of molten agar media in a pre-warmed glass tube, and the tube mixed by rolling vigorously between palms. The tube's mixed contents were then poured onto a pre-warmed solid agar media plate, which was swirled to distribute the molten agar uniformly. The plate was incubated in a biosafety cabinet with the lid ajar until the molten agar gelled, then the new overlay plate was incubated at 37 °C overnight. This process was repeated in duplicate or triplicate for each phage display fraction dilution. The following day, individual phage clones from the phage display fraction were visible as small clearings with blue-green halos or hazy blue-green circles (phage plaques) within the bacterial overgrowth. These plates were sealed and stored at 4 °C for up to two weeks.

*Phage amplification*: Once separated from other phages in the phage display fraction, unique phage clones on a double agar overlay plate can be picked and amplified. First, an overnight culture of ER2738 K12 E. coli started on the day prior was diluted to OD<sub>600</sub> 0.09 and incubated at 37 °C with shaking. After 15 minutes incubating in a baffled flask with vented (or loose) cap, 100 ml of the liquid E. coli culture was inoculated with a single phage plaque picked from a double agar overlay plate with a sterile transfer pipette (if amplifying from an already amplified stock, cultures were inoculated at a multiplicity of infection < 1.0) and incubated at 37 °C with vigorous shaking. After 4.75 to 5 hours, the infected E. coli culture was aliquoted into 50 ml conical tubes with approximately 35 ml of infected culture per tube. These tubes were centrifuged at 4,800 ×RCF for 10 minutes at 4 °C to pellet bacterial cells. The supernatant was removed (the pellet was discarded) to another sterile 50 ml conical tube, one-sixth volume 20% polyethylene glycol in 2.5 M sodium chloride was added, and the tubes were incubated overnight at 4 °C. After at least 8 to 12 hours, the tubes were centrifuged again at 4,800 ×RCF for 55 minutes at 4 °C to pellet the phages. The pellets were retained (the supernatants were poured off and discarded) and 1 ml 1×PBS + 10 mM EDTA was added. This was incubated at least one hour at room temperature to soften the pellet. Vortexing periodically during and after incubation helped to resuspend the pellet. Repeated gentle pipetting also sped resuspension. Newly resuspended pellets were transferred to sterile microcentrifuge tubes and centrifuged at 20,800 ×RCF for 10 minutes at 4 °C. The supernatant was removed and discarded and the pellets were finally resuspended in 50  $\mu$ l 1×PBS + 10 mM EDTA.

Determining amplified phage stock concentrations: Stocks of amplified phage clones must be titered to reveal their concentrations. The protocol for titering phage stocks was identical to the protocol for isolating individual phage clones described above, except more replicates were performed across a smaller range of stock concentrations. Since amplified phage stocks typically had between 10<sup>8</sup> and 10<sup>14</sup> plaque-forming units (PFU)/ml, performing triple replicates of 10<sup>-7</sup>, 10<sup>-8</sup>, and 10<sup>-9</sup> dilutions was usually sufficient. Counting the phage plaques on each plate and multiplying to correct the dilution factor revealed the concentration of the amplified stock per 100 µl. Further multiplying by 10 to correct the amount added revealed the number of PFU/ml.

Enzyme-linked immunosorbent assay and analysis: High titer phage stocks were characterized for affinity to the desired analyte by enzyme-linked immunosorbent assay (ELISA). First, 96-well plates were coated with the desired analyte. The desired analyte (recombinant human HMGB1) was diluted to 10 µg/ml in 0.1 M sodium bicarbonate (pH 8.6), and 100 µl was added to each well. Plates were then incubated overnight at 4 °C in a humidified air-tight container. The following day, the analyte solution was removed and each well rinsed six times with TBST before being incubated with 200 µl of blocking buffer per well at 4 °C for two hours. After incubating the blocking buffer, it was removed, each well was rinsed six times with TBST, and 100 µl of phage (in place of 1° antibody in a traditional indirect ELISA) diluted in PBS was added to each well. After incubating the phage dilution at room temperature for two hours (with agitation at ~240 RPM), the phage solution was removed, each well was rinsed six times with TBST, and 100 µl of horseradish peroxidase (HRP)-conjugated 2° antibody (Anti-M13 g8p Monoclonal Antibody (HRP), Antibody Design Laboratories, San Diego, CA) in PBS was added to each well. The secondary antibody was incubated at room temperature for one hour (with gentle agitation at ~240 RPM). Before developing the color reaction to indicate phage 1° binding to the target analyte, the 2° antibody was removed, each well was rinsed six times with TBST, and 100 µl of HRP substrate (o-phenylenediamine dihydrochloride, SIGMAFAST OPD tablet set, Sigma-Aldrich, St. Louis, MO) diluted 1:20 in TBST was added. The color reaction was incubated in the dark at 25 °C and each well's OD<sub>450</sub> was measured every five minutes for 75 to 90 minutes.

 $OD_{450}$  values for each combination of phage concentration and analyte concentration were pooled and the means compared (plus or minus standard error of the mean) with other combinations and controls as appropriate. Each 96-well plate was set up such that every batch of experimental ELISA data was accompanied by a blocked negative control (blocked with blocking buffer but no 1° phage or 2° antibody) and unblocked negative control (never blocked with blocking buffer, incubated with 1° phage, or incubated with 2° antibody) to reveal baseline values for the color reaction. Greater  $OD_{450}$  indicated a relatively greater amount of 2° antibody bound to 1° phage, which we interpreted as higher affinity for the target analyte by that 1° phage's displayed peptide. Monitoring changes in  $OD_{450}$  over time, as a function of target analyte concentration, revealed which phages had relatively higher affinity for the target analyte or bound the analyte at relatively lower analyte concentrations.

Sanger sequencing and sequence analysis: Once a phage was found to have a relatively high affinity for the analyte or to bind the analyte at a relatively low analyte concentration, the phages were reserved for Sanger sequencing to reveal the identity of their displayed peptide (Figure 2). We used the -96 sequencing primer reverse strand (5'-CCC TCA TAG TTA GCG TAA CG-3' or 3'-GCA ATG CGA TTG ATA CTC CC-5') from the Ph.D.-12 phage display library kit. Since the sequencing primer was on the reverse strand, all results had to be converted to the reverse complement such that the first base read became the last base in the final sequence and the complementary base pair was used instead. This made reading and analyzing the sequencing results simpler. In the reverse complement of the sequencing results we looked for signature sequences directly upstream and downstream of the inserted phage display peptide. The upstream signature sequence was 5'-TCT CAC TCT-3' and the downstream signature sequence was 5'-GGT GGA GGT-3'. Finding both signature sequences in the reverse complement of the sequencing results revealed the 36 base pairs coding for the 12 amino acids in the inserted peptide (Figure 3). These 36 base pairs were parsed into 3 base pair codons and translated into amino acids (Wernersson 2006). By design of the phage display library, each codon should be made up of base pairs NNK (any base pair, any base pair, guanine or thymine).

*Peptide analysis*: Once peptide identities were extracted from Sanger sequencing data, they were compared using the PRALINE multiple sequence alignment tool (ibi.vu.nl/programs/pralinewww) (Heringa 1999, Heringa 2002, Pirovano, Feenstra et al. 2008). Peptide sequences were aligned to check for any conserved sequences or motifs, conserved patterns of similar amino acid type, conserved patterns of similar hydrophobicity, and conserved secondary structures.

#### RESULTS

Selection of high specific peptide probes: Our panning scheme (Figure 1) eliminated many phages without peptides that have affinity for the chosen analyte. After two successive rounds of negative panning, where phages that do not bind the substance immobilized inside the glass microcapillary tube were collected (*e.g.* S-H- phages), we collected on the order of  $10^9$ PFU/ml (data not shown). When a double panning strategy to collect phages that bound only one of the two substances immobilized inside the glass capillary tube were collected (*e.g.* S-H+ or S+H- phages), we collected on the order of  $10^5$  PFU/ml (data not shown). When the panning strategy collected only phages that bound to both substances immobilized inside the glass capillary tubes (*e.g.* S+H+ phages), we collected on the order of  $10^3$  PFU/ml (data not shown).

*Confirmation of probe specificity by ELISA:* Both positive (selecting for phages with peptides that do bind a given substance) and negative (selecting for phages with peptides that do not bind a given substance) panning protocols succeeded. When phages with peptides that do not bind to either the biological background solution or the chosen analyte (S-H- phages) were tested by ELISA for the ability to bind the analyte, we found the mean OD<sub>450</sub> values changed very little over time as the ELISA color reaction was developed (Figure 4A). Conversely, when phages with peptides that do not bind the biological background solution but do bind the chosen analyte (S-H+ phages) were tested by ELISA using the analyte as a target, we found that mean OD<sub>450</sub> values rose markedly over time (Figure 4B). This effect seems to be dose-dependent with the amount of analyte used as the target, as 10  $\mu$ g HMGB1/ml wells reached the highest OD<sub>450</sub>, followed by 5  $\mu$ g HMGB1/ml (Figure 4B). Mean OD<sub>450</sub> values for 0.1 and 0.0  $\mu$ g HMGB1/ml were approximately equivalent (Figure 4B).

Advantage of panning to eliminate phages with background affinity: The strategy (see Figure 1) of one negative then one positive round of phage panning yielded multiple phages with peptides that bind the chosen analyte even better when these phages, the target analyte, and the background solution were all incubated together during the phage-as-primary-antibody step of an ELISA (Figure 5). The increase in phage binding was less evident at higher concentrations of the target analyte but became clear when increasingly smaller amounts of the analyte incubated in a 10% dilution of the background solution were used as the ELISA target.

Unlike the S-H+ phages, which bind their analyte well even when incubated with the biological background solution (Figure 6A-B), phages with affinity for both the analyte and the background solution (S+H+ phages) do not bind the analyte well when it is incubated with the background solution (Figure 6C-D.

*Analysis of amino acid sequences of selected probes:* After collecting multiple phages with measured affinity for the chosen analyte even when incubated with a biological background solution, we used Sanger sequencing (see Figures 2-3) to reveal the identity of each displayed peptide. When the sequences for nine S-H+ phages were checked for conserved residues (Figure

7), residue types (Figure 8), hydrophobicity (Figure 9), or secondary structure (Figure 10), we did not detect any common patterns or conserved motifs.

#### DISCUSSION

*The potential of phage display for peptide probe selection:* The development of peptide probe-based biosensors is an emerging field (Kim, Cho et al. 2019, Wasilewski, Szulczyński et al. 2019). Phage display is an excellent and underutilized tool for screening probe peptides that can be used as biorecognition elements in biosensors. Phages with peptides that bind the analyte (Figure 4B), but not a biological background solution (Figure 6B), can be preferentially selected very rapidly. Though we report on only a small number of phages here, at the end of our panning process (Figure 1) we collected 50  $\mu$ l of S-H+ phages at 10<sup>5</sup> PFU/ml concentration. This gives us a large pool to draw upon for further phage and peptide characterization should one or more of our (randomly) selected peptides fail as biorecognition elements. The ten S-H+ phages we characterized are all unique with no conserved motifs (Figure 7), residue types (Figure 8), hydrophobicity or hydrophilicity regions (Figure 9), or secondary structures (Figure 10). This gives us confidence that within the remaining pool of roughly 2500 S-H+ phages (25  $\mu$ l of 10<sup>5</sup> PFU/ml S-H+ phages) there are a high number of other unique peptides with potential for use in biosensors.

*The advantage of phage display:* These large numbers of phages and their peptides, along with the speed of panning and amplification procedures, give phage display-derived peptides tremendous advantages over antibodies. Many phages (on the order of 10<sup>9</sup>) are screened at once during one hour of phage display *in vitro* recirculation, making this technique highly parallel in contrast to the lengthy in series and *in vivo* techniques required to isolate a new monoclonal antibody (Wesolowski, Alzogaray et al. 2009, Walper, Anderson et al. 2012, Rahim, Wang et al. 2019).

*The advantages of phage display over antibody selection:* Phage display has other advantages over antibody production beyond those of speed and number. At 7-12 amino acids in length, phage display-derived peptides are much easier and less expensive to produce (Newton, Kelly et al. 2006). The peptide approach is also animal-independent and does not depend upon the immune response, making it possible to use phage display even against analytes which would otherwise be lethal or dangerous to a production animal (Leenaars and Hendriksen 2005, Rahim, Wang et al. 2019). Because peptides are much shorter and smaller than antibodies, it is easier to optimize and test each amino acid on a peptide (Otvos and Wade 2014). Their short lengths also make them easier to produce synthetically en masse than antibodies (Wylie, Wylie et al. 2018), more thermostable (Raina, Sharma et al. 2015), and much easier to customize during production (Goldman, Pazirandeh et al. 2000). With only 12-20 amino acids, peptides have less bulk to be responsible for off-target binding and produce correspondingly less background (Tawil, Sacher et al. 2012). Finally, in sensing platforms that rely on an increase in mass to detect the analyte (*e.g.* surface acoustic wave (SAW)- or quartz crystal microbalance-based platforms), the small size of a peptide being used as biorecognition element means a much greater signal-to-noise ratio than if a small analyte was bound by a relatively massive antibody (Tawil, Sacher et al. 2012).

*Combining phage display-derived peptide probes and SAW sensors:* The ease of collection, characterization, and customization, and the advantage in signal-to-noise ratio suggests phage display-derived peptides are best suited for use in SAW-based biosensors. Since SAWs produce a signal based on a change in mass density on their piezoelectric surface (Tawil, Sacher et al. 2012), they are primed to exploit the greater signal-to-noise ratio inherent in a relatively small and stiff peptide (Mukundan, Kumar et al. 2012). Since peptides like the ones described here can be selected with low affinity to the background solution, they are ready for use in a continuously sampling, label-free sensor like a SAW (Mujahid and Dickert 2017). The real-time capabilities of a SAW sensor would be wasted on a biorecognition element that requires sample preparation or labeling steps. Instead, a biological fluid can flow over the SAW's sensitive surface, an analyte can bind to the phage display-derived peptide tethered on the surface, and the SAW will detect this binding event within microseconds. Such a sensor might even be implanted into the body (Murphy, Bahmanyar et al. 2013) or other sensitive location and interrogated wirelessly (Fachberger and Erlacher 2009, Shevchenko, Kukaev et al. 2018, Tao, Hasan et al. 2018).

## MILITARY SIGNIFICANCE

Applying peptide probes to developing a biosensor for traumatic brain and cranial nerve *injuries:* Beyond serving as a proof-of-concept for our phage display pipeline, the peptides we characterized and identified also have functionality for detecting traumatic brain and cranial nerve injuries. U.S. military personnel suffered more than 383,000 traumatic brain injuries from

2000 to 2018 (Defense and Veterans Brain Injury Center 2020), and modern warfare is increasingly expeditionary (O'Brien 2020). Future naval conflict with near-peer adversaries will produce large numbers of blast casualties and the requirement for prolonged field care. Reverberating shockwaves in confined areas, such as shipboard compartments, light armored vehicles, and amphibious assault vehicles, will amplify a blast's effects (Leibovici, Gofrit et al. 1996). An increase in blast-related injuries will necessitate new ways for corpsmen to identify, diagnose, triage, and treat a corresponding increase in traumatic brain and cranial nerve injuries. Quantitative testing will eliminate the need for Sailors and Marines to identify and self-disclose their own symptoms, which they may loathe to do for fear of disrupting their own mission. In the near-term these peptides will enable rapid, objective, and quantitative testing for traumatic brain and cranial nerve injuries. In the long-term these peptides will help to address multiple Naval operational gaps including: (1) the lack of ability to use imaging or biomarkers in diagnosis, (2) the inability to objectively and definitively identify traumatic brain and cranial nerve injuries, (3) the lack of understanding of these injuries and the insufficient understanding of their short- and long-term effects, (4) the lack of screening criteria for milder injuries, and (5) the need for Commanders to have real-time insight into the mental health, physical health, and medical readiness of their Sailors and Marines.

While the SAW sensing platform we propose is a relatively mature technology (Coimbatore, Presley et al. 2008, Fachberger and Erlacher 2009, Rocha-Gaso, March-Iborra et al. 2009, Mukundan, Kumar et al. 2012, Mujahid and Dickert 2017, Chen, Wu et al. 2018, Tao, Hasan et al. 2018), it is hindered by a reliance on antibodies as primary detectors. Our approach, which leverages phage display-derived peptides, has many advantages over antibody-based methods (Goldman, Pazirandeh et al. 2000, Kehoe, Velappan et al. 2006, Tolba, Ahmed et al. 2012, Raina, Sharma et al. 2015). The entire pipeline from securing a sample of the desired analyte to peptide sequences ready-for-synthesis takes less than one month of laboratory time. In this case, our methods were developed and refined by one undergraduate student and one contract research scientist over the course of a Naval Research Enterprise Internship Program 10week internship. Conversely, antibodies can take months to produce and isolate, much less characterize and produce in high quantities (Committee on Methods of Producing Monoclonal Antibodies 1999, Leenaars and Hendriksen 2005). The shorter timelines enabled by our phage display pipeline will accelerate sensor development to meet the needs for monitoring

18

environmental samples for contamination (Suk, Zmorzynska et al. 2011, Luka, Samiei et al. 2019), disease surveillance and diagnosis (Gallego, Sintchenko et al. 2009), for biomarker quantification (Sage, Besant et al. 2015), and biological threat warning systems (Coimbatore, Presley et al. 2008).

There are many threats U.S. military personnel must be prepared for, and the list is growing longer. Breaking the historical reliance on antibodies as biorecognition elements for sensors will let us produce tests and sensors much more rapidly and without production animals. We should eliminate the antibody bottleneck by incorporating phage display into the biosensor development pipeline. Phage display-derived peptides, especially when paired with SAW-based sensor platforms, are poised to replace traditional antibodies and should be embraced. These sensors with phage display-derived peptides will be useful in operational environments, for environmental monitoring, and for biomedical purposes in the military health system.

#### REFERENCES

- Ahmed, A., J. V. Rushworth, N. A. Hirst and P. A. Millner (2014). "Biosensors for whole-cell bacterial detection." <u>Clin Microbiol Rev</u> 27(3): 631-646.
- Arap, W., M. G. Kolonin, M. Trepel, J. Lahdenranta, M. Cardo-Vila, R. J. Giordano, P. J. Mintz, P. U. Ardelt, V. J. Yao, C. I. Vidal, L. Chen, A. Flamm, H. Valtanen, L. M. Weavind, M. E. Hicks, R. E. Pollock, G. H. Botz, C. D. Bucana, E. Koivunen, D. Cahill, P. Troncoso, K. A. Baggerly, R. D. Pentz, K.-A. Do, C. J. Logothetis and R. Pasqualini (2002). "Steps toward mapping the human vasculature by phage display." <u>Nature Medicine</u> 8: 121-127.
- Aucott, H., J. Lundberg, H. Salo, L. Klevenvall, P. Damberg, L. Ottosson, U. Andersson, S. Holmin and H. E. Harris (2018). "Neuroinflammation in response to intracerebral injections of different HMGB1 redox isoforms." J Innate Immun 10(3): 215-227.
- Billingsley, M. M., R. S. Riley and E. S. Day (2017). "Antibody-nanoparticle conjugates to enhance the sensitivity of ELISA-based detection methods." <u>PLoS One</u> **12**(5): e0177592.
- Centers for Disease Control and Prevention. (4 April 2018). "Bioterrorism emergency preparedness and response." <u>Specific Hazards</u> Retrieved 27 August 2020, from https://emergency.cdc.gov/agent/agentlist.asp.
- Chen, L., D. Wu and J. Yoon (2018). "Recent advances in the development of chromophore-based chemosensors for nerve agents and phosgene." <u>ACS Sens</u> **3**(1): 27-43.
- Coimbatore, G., S. M. Presley, J. Boyd, E. J. Marsland and G. P. Cobb (2008). Sensing biological and chemical threat agents. <u>Advances in biological and chemical terrorism</u>

<u>countermeasures</u>. R. J. Kendal, S. M. Presley, G. P. Austin and P. N. Smith. Boca Raton, FL, CRC Press, Taylor & Francis Group: 159-178.

- Committee on Methods of Producing Monoclonal Antibodies (1999). Monoclonal antibody production. Committee on Methods of Producing Monoclonal Antibodies Institute for Laboratory Animal Research. Washington D.C., National Academy Press.
- Defense and Veterans Brain Injury Center. (2020, 18 June 2020). "DoD worldwide numbers for TBI." <u>TBI & the military</u> Retrieved 23 June 2020, 2020, from https://dvbic.dcoe.mil/dod-worldwide-numbers-tbi.
- Drake, C. and R. A. Levine (2005). "Sensitivity, specificity, and other diagnostic measures with multiple sites per unit." <u>Contemp Clin Trials</u> **26**(2): 252-259.
- Fachberger, R. and A. Erlacher (2009). "Monitoring of the temperature inside a lining of a metallurgical vessel using a SAW temperature sensor." <u>Procedia Chemistry</u> 1(1): 1239-1242.
- Fralick, J. A., P. Chadha-Mohanty and G. Li (2008). Phage display and its application for the detection and therapeutical intervention of biological threat agents. <u>Advances in biological and chemical terrorism countermasures</u>. R. J. Kendal, S. M. Presley, G. P. Austin and P. N. Smith. Boca Raton, FL, CRC Press, Taylor & Francis Group: 179-201.
- Gallego, B., V. Sintchenko, Q. Wang, L. Hiley, G. L. Gilbert and E. Coiera (2009). "Biosurveillance of emerging biothreats using scalable genotype clustering." J Biomed <u>Inform</u> 42(1): 66-73.
- Goldman, E. R., M. P. Pazirandeh, J. M. Mauro, K. D. King, J. C. Frey and G. P. Anderson (2000). "Phage-displayed peptides as biosensor reagents." <u>J Mol Recognit</u> 13: 382-387.
- Heringa, J. (1999). "Two strategies for sequence comparison: profile-preprocessed and secondary structure-induced multiple alignment." <u>Comput Chem</u> **23**(3-4): 341-364.
- Heringa, J. (2002). "Local weighting schemes for protein multiple sequence alignment." <u>Comput</u> <u>Chem</u> **26**(5): 459-477.
- Kehoe, J. W., N. Velappan, M. Walbolt, J. Rasmussen, D. King, J. Lou, K. Knopp, P. Pavlik, J. D. Marks, C. R. Bertozzi and A. R. Bradbury (2006). "Using phage display to select antibodies recognizing post-translational modifications independently of sequence context." <u>Mol Cell</u> <u>Proteomics</u> 5(12): 2350-2363.
- Kim, J. H., C. H. Cho, M. Y. Ryu, J.-G. Kim, S.-J. Lee, T. J. Park and J. P. Park (2019). "Development of peptide biosensor for the detection of dengue fever marker, nonstructural 1." <u>PLoS One</u> 14(9).

- Ledsgaard, L., M. Kilstrup, A. Karatt-Vellatt, J. McCafferty and A. H. Laustsen (2018). "Basics of antibody phage display technology." <u>Toxins</u> **10**(6).
- Leenaars, M. and C. F. M. Hendriksen (2005). "Critical steps in the production of polyclonal and monoclonal antibodies: evaluation and recommendations." <u>ILAR J</u> **46**(3): 269-279.
- Leibovici, D., O. N. Gofrit, M. Stein, S. C. Shapira, Y. Noga, R. J. Heruti and J. Shemer (1996).
  "Blast injuries: bus versus open-air bombings--a comparative study of injuries in survivors of open-air versuse confined-space explosions." J Trauma 41(6): 1030-1035.
- Lonsdale, C. L., B. Taba, N. Queralto, R. A. Lukaszewski, R. A. Martino, P. A. Rhodes and S. H. Lim (2013). "The use of colorimetric sensor arrays to discriminate between pathogenic bacteria." <u>PLoS One</u> 8(5): e62726.
- Luka, G., E. Samiei, S. Dehghani, T. Johnson, H. Najjaran and M. Hoorfar (2019). "Label-free capacitive biosensor for detection of Cryptosporidium." <u>Sensors (Basel)</u> 19(2).
- Mujahid, A. and F. L. Dickert (2017). "Surface acoustic wave (SAW) for chemical sensing applications of recognition layers." <u>Sensors (Basel)</u> 17(2716).
- Mukundan, H., S. Kumar, D. N. Price, S. M. Ray, Y. J. Lee, S. Min, S. Eum, J. Kubicek-Sutherland, J. M. Resnick, W. K. Grace, A. S. Anderson, S. H. Hwang, S. N. Cho, L. E. Via, C. Barry, 3rd, R. Sakamuri and B. I. Swanson (2012). "Rapid detection of *Mycobacterium tuberculosis* biomarkers in a sandwich immunoassay format using a waveguide-based optical biosensor." <u>Tuberculosis (Edinb)</u> 92(5): 407-416.
- Murphy, O. H., M. R. Bahmanyar, A. Borghi, C. N. McLeod, M. Navaratnarajah, M. H. Yacoub and C. Toumazou (2013). "Continuous *in vivo* blood pressure measurements using a fully implantable wireless SAW sensor." <u>Biomed Microdevices</u> 15: 737-749.
- Newton, J. R., K. A. Kelly, U. Mahmood, R. Weissleder and S. L. Deutscher (2006). "In vivo selection of phage for the optical imaging of PC-3 human prostate carcinoma in mice." <u>Neoplasia</u> 8(9): 772-780.
- O'Brien, R. C. (2020). Why the U.S. is moving troops out of Germany. <u>Wall Street Journal</u>. New York, NY, Dow Jones & Company, Inc.
- Otvos, L. J. and J. D. Wade (2014). "Current challenges in peptide-based drug discovery." <u>Front</u> <u>Chem</u> **2**(62).
- Paudel, Y. N., M. F. Shaikh, A. Charkraborti, Y. Kumari, A. Aledo-Serrano, K. Aleksovska, M. K. M. Alvim and I. Othman (2018). "HMGB1: a common biomarker and potential target for TBI, neuroinflammation, epilepsy, and cognitive dysfunction." <u>Front Neurosci</u> 12(628).
- Pirovano, W., K. A. Feenstra and J. Heringa (2008). "PRALINE: a strategy for improved multiple alignment of transmembrane protein." <u>Bioinformatics</u> **24**(4): 492-497.

- Rahim, M., M. Wang, T. Wang, S. He, B. Griffin, D. Kobasa, R. Yang, Z. Du and X. Qiu (2019). "Generation and characterization of anti-filovirus nucleoprotein monoclonal antibodies." <u>Viruses</u> 11(3): 259.
- Raina, M., R. Sharma, S. E. Deacon, C. Tiede, D. Tomlinson, A. G. Davies, M. J. McPherson and C. Walti (2015). "Antibody mimetic receptor proteins for label-free biosensors." <u>Analyst</u> 140(3): 803-810.
- Rocha-Gaso, M. I., C. March-Iborra, A. Montoya-Baides and A. Arnau-Vives (2009). "Surface generated acoustic wave biosensors for the detection of pathogens: a review." <u>Sensors</u> (Basel) 9(7): 5740-5769.
- Sage, A. T., J. D. Besant, L. Mahmoudian, M. Poudineh, X. Bai, R. Zamel, M. Hsin, E. H. Sargent, M. Cypel, M. Liu, S. Keshavjee and S. O. Kelley (2015). "Fractal circuit sensors enable rapid quantification of biomarkers for donor lung assessment for transplantation." <u>Sci Adv</u> 1.
- Selvam, A. P., A. Wangzhou, M. Jacobs, T. Wu, C. Mohan and S. Prasad (2017). "Development and validation of an impedance biosensor for point-of-care detection of vascular cell adhesion molecule-1 toward lupus diagnostics." <u>Future Sci OA</u> 3(3).
- Shabani, A., M. Zourob, B. Allain, C. A. Marquette, M. C. Lawrence and R. Mandeville (2008). "Bacteriophage-modified microarrays for the direct impedimetric detection of bacteria." <u>Anal Chem</u> 80: 9475-9482.
- Shevchenko, S., A. Kukaev, M. Khivrich and D. Lukyanov (2018). "Surface-acoustic-wave sensor design for acceleration measurement." <u>Sensors (Basel)</u> 18(7).
- Soelberg, S. D., R. C. Stevens, A. P. Limaye and C. E. Furlong (2009). "Surface plasmon resonance (SPR) detection using antibody-linked magnetic nanoparticles for analyte capture, purification, concentration, and signal amplification." <u>Anal Chem</u> 81(6): 2357-2363.
- Suk, J. E., A. Zmorzynska, I. Hunger, W. Biederbick, J. Sasse, H. Maidhof and J. C. Semenza (2011). "Dual-use research and technological diffusion: reconsidering the bioterrorism threat spectrum." <u>PLoS Pathog</u> 7(1): e1001253.
- Tao, R., S. A. Hasan, H. Z. Wang, J. Zhou, J. T. Luo, G. McHale, D. Gibson, P. Canyelles-Pericas, M. D. Cooke, D. Wood, Y. Liu, Q. Wu, W. P. Ng, T. Franke and Y. Q. Fu (2018). "Bimorph material/structure designs for high sensitivity flexible surface acoustic wave temperature sensors." <u>Sci Rep</u> 8(1): 9052.
- Tawil, N., E. Sacher, R. Mandeville and M. Meunier (2012). "Surface plasmon resonance detection of *E. coli* and methicillin-resistant *S. aureus* using bacteriophages." <u>Biosensors and</u> <u>Bioelectronics</u> 37(1): 24-29.

- Tikunova, N. V. and V. V. Morozova (2009). "Phage display on the base of filamentous bacteriophages: application for recombinant antibodies selection." <u>Acta Naturae</u> 1(3): 20-28.
- Titus, J., M. Kay, J. Glaser and Y. Y. Hwang (2017). "Application of phage display for the development of a novel inhibitor of PLA<sub>2</sub> activity in Western Cottonmouth venom." J <u>Venom Res</u> 8: 19-24.
- Tolba, M., M. U. Ahmed, C. Tlili, F. Eichenseher, M. J. Loessner and M. Zourob (2012). "A bacteriophage endolysin-based electrochemical impedance biosensor for the rapid detection of Listeria cells." <u>Analyst</u> **137**(24): 5749-5756.
- VanPatten, S. and Y. Al-Abed (2017). "High mobility group box-1 (HMGb1): current wisdom and advancement as a potential drug target." J Med Chem **61**(12): 5093-5107.
- Walper, S., P. Lee, G. Anderson and E. Goldman (2013). "Selection and Characterization of Single Domain Antibodies Specific for Bacillus anthracis Spore Proteins." <u>Antibodies</u> 2(4): 152-167.
- Walper, S. A., G. P. Anderson, P. A. Brozozog Lee, R. H. Glaven, J. L. Liu, R. D. Bernstein, D. Zabetakis, L. Johnson, J. M. Czarnecki and E. R. Goldman (2012). "Rugged single domain antibody detection elements for *Bacillus anthracis* spores and vegetative cells." <u>PLoS One</u> 7(3): e32801.
- Walper, S. A., G. Lasarte Aragones, K. E. Sapsford, C. W. Brown, 3rd, C. E. Rowland, J. C. Breger and I. L. Medintz (2018). "Detecting biothreat agents: From current diagnostics to developing sensor technologies." <u>ACS Sens</u> 3(10): 1894-2024.
- Wasilewski, T., B. Szulczyński, M. Wojciechowski, W. Kamysz and J. Gębicki (2019). "A highly selective biosensor based on peptide directly derived from the HarmOBP7 aldehyde binding site." <u>Sensors</u> **19**(19).
- Wernersson, R. (2006). "Virtual ribosome a comprehensive DNA translation tool with support for integration of sequence feature annotation." <u>Nucleic Acids Res</u> **34**: W385-W388.
- Wesolowski, J., V. Alzogaray, J. Reyelt, M. Unger, K. Juarez, M. Urrutia, A. Cauerhff, W. Danquah, B. Rissiek, F. Scheuplein, N. Schwarz, S. Adriouch, O. Boyer, M. Seman, A. Licea, D. V. Serreze, F. A. Goldbaum, F. Haag and F. Koch-Nolte (2009). "Single domain antibodies: promising experimental and therapeutic tools in infection and immunity." <u>Med Microbiol Immunol</u> 198(3): 157-174.
- Wylie, K. M., T. N. Wylie, R. Buller, B. Herter, M. T. Cannella and G. A. Storch (2018).
   "Detection of viruses in clinical samples by use of metagenomic sequencing and targeted sequence capture." J Clin Microbiol 56.

### FIGURES



Figure 1. Example panning scheme for collecting phages that do not bind a biological sample matrix (saliva) but do bind an analyte (HMGB1). Panning the phage display library against the biological sample matrix (saliva) first and collecting the nonbinding phages eliminates any phages with strong affinity for the matrix solution. These phages are then panned against the desired analyte (HMGB1) and the phages that bind the analyte are collected. This process can also be adapted to collect phages for use as positive (binding both the matrix and the analyte) and negative (binding neither the matrix nor the analyte) controls.



#### Confirm peptide as unique

Figure 2. Pipeline from HMGB1-binding phage to unique peptide sequence. After phage affinity for HMGB1 is confirmed by ELISA, the inserted phage display peptide's identity is revealed by Sanger sequencing. Peptides are compared with one another to confirm each is unique.

### Example (from S-H+9):

←

## 5′ – TTTGGAGATTTTCAACGTGAAAAAATTATTATTCGCAATTCCTTTAGTGGTACCTTTC 3′ – AAACCTCTAAAAGTTGCACTTTTTTAATAATAAGCGTTAAGGAAATCACCATGGAAAG

Upstream signature	12 codons for inserted peptide	Downstream signature
TAT <b>TCTCACTCTCA</b>	ATGTTTTTGGTATGAATTTTAAGATGGAGATGG	<b>TGGGTGGAGGT</b> TCGG
ATAAGAGTGAGAGT	TACAAAAACCATACTTAAAATTCTACCTCTACC	CACCCACCTCCAAGCC

# CCGAAACTGTTGAAAGTTGTTTAGCAAAATCCCATAC...CGTTACGCTAACTATGAGGG-3' GGCTTTGACAACTTT<u>CAACAAATCGTTTTAGGGTATG</u>...<u>GCAATGCGATTGATACTCCC</u>-5'

-28 Sequencing primer  $\leftarrow$  -96 Sequencing primer

**Figure 3. Example sequencing result using the -96 sequencing primer.** After Sanger sequencing with the recommended -96 sequencing primer (3'-GCAATGCGATTGATACTCCC-5'), the 12 codons of the inserted phage display peptide are revealed by searching for the upstream (red) and downstream (blue) signature sequences which flank them. The 12 codons for the inserted peptide can also be found by identifying the -28 sequencing primer (3'-CAACAATCGTTTTAGGGTATG-5') downstream and counting 28 base pairs upstream. In actual sequencing results, the -96 sequencing primer and many base pairs upstream of it will not be present, though the -28 sequencing primer may be and the downstream signature should be.

←



Figure 4. Panning separates phages by their affinity for the analyte (HMGB1). Phages displaying peptides with no (or low) affinity for a chosen analyte (HMGB1) are not retained inside the glass microcapillary tube during panning, and are easily separated from those which do bind the chosen analyte. A representative nonbinding phage (S-H- #1, shown in A) does not bind to HMGB1 with high affinity and produces low optical density (OD<sub>450</sub>) during ELISA tests. A representative HMGB1-binding phage (S-H+ #1, shown in B) does bind to HMGB1 and produces a correspondingly higher OD<sub>450</sub>.



**Figure 5.** Phages bind their analyte (HMGB1) even in the presence of a biological fluid (saliva). Phages selected for their inability to bind a biological fluid (saliva) and ability to bind an analyte (HMGB1) bind the analyte even when incubated with the biological fluid. Two representative phages, S-H+ #2 (A-B) and S-H+ #4 (C-D) are shown. Both phages bind their analyte with greater affinity at lower analyte concentrations when incubated with the biological fluid.



**Figure 6.** Negative panning to remove phages with affinity for the biological solution results in higher affinity for the analyte when incubated in the biological solution. The panning scheme eliminated phages with affinity for the biological solution (saliva) before collecting phages with affinity for the chosen analyte (HMGB1). These S-H+ phages (representative phage S-H+ #5 shown) bind the analyte well in buffer (A) and in buffer plus saliva (B). S+H+ phages with affinity for both the biological solution and the analyte bind the analyte well in buffer (C) but do not bind as well when incubated in buffer plus saliva (D).



**Figure 7. Alignment and residue conservation.** S-H+ peptides aligned and marked for the conservation of each residue relative to the other residues at the same position in other peptides. Relatively conserved residues are marked with redder colors, while less conserved residues are marked with bluer colors.



**Figure 8. Alignment and residue type.** S-H+ peptides aligned and marked for their residue type and frequency (ClustalX color scheme).



**Figure 9. Alignment and residue hydrophobicity.** S-H+ peptides aligned and marked for the hydrophobicity (bluer colors) or hydrophilicity (redder colors) of each residue.



Figure 10. Alignment and secondary structure propensity. S-H+ peptides aligned and marked for their propensity to form helix-shaped ( $\alpha$ -helices, red) or strand-shaped ( $\beta$ -folds, blue) secondary structures.

# **REPORT DOCUMENTATION PAGE**

The public reporting burden for this collect sources, gathering and maintaining the d aspect of this collection of information, im 1215 Jefferson Davis Highway, Suite 120 to any penalty for failing to comply with a <b>THE ABOVE ADDRESS.</b>	ction of information is estimated to average ata needed, and completing and reviewin cluding suggestions for reducing the bur 14, Arlington, VA 22202-4302, Responde collection of information if it does not dis	ge 1 hour per respor ng the collection of ir den, to Washington I nts should be aware play a currently valid	ase, including the time for reviewing instructions, searching existing data formation. Send comments regarding this burden estimate or any other Headquarters Services, Directorate for Information Operations and Reports, that notwithstanding any other provision of law, no person shall be subject OMB Control number. <b>PLEASE DO NOT RETURN YOUR FORM TO</b>	
1. REPORT DATE (DD MM YY) 28 10 20	2. REPORT TYPE Technical Report		3. DATES COVERED (from – to) June 2019 – Sept 2020	
<ul> <li>4. TITLE <ul> <li>A two-step phage display panning method for selecting peptides to detect</li> <li>HMGB1 and its potential for developing peptide-based biosensors</li> </ul> </li> <li>6. AUTHORS <ul> <li>Lemon, Bache, May, Moffett, Huh, Ford, and Hwang</li> </ul> </li> <li>7. PERFORMING ORGANIZATION NAME(S) AND ADDRESS(ES) <ul> <li>Naval Medical Research Unit San Antonio</li> <li>3650 Chambers Pass BLDG 3610</li> </ul> </li> </ul>			5a. Contract Number:         5b. Grant Number:         5c. Program Element Number:         5d. Project Number:         5e. Task Number:         5f. Work Unit Number: G1722	
JBSA Fort Sam Houston, TX 78234-6315			8. PERFORMING ORGANIZATION REPORT	
9. SPONSORING/MONITORING AGENCY NAMES(S) AND ADDRESS(ES) Advanced Medical Development Program			Report No. 20-604	
503 Robert Grant Ave BLDG 500		10. SPONSOR/MONITOR'S ACRONYM(S)		
Silver Spring, MD 20910		11. SPONSOR/MONITOR'S REPORT NUMBER(s)		
12. DISTRIBUTION/AVAILABILITY Approved for public release	<b>STATEMENT</b> se; distribution is unlimited.			
13. SUPPLEMENTARY NOTES N.A.				
14. ABSTRACT Expeditionary and deployed p biomedical threats. Biosenso analyte, have great promise are hampered by a historical production and characterizat a laboratory animal. We chan Phage display leverages sma phage panning protocol that bind a desired analyte. This t produces many unique peptie entire pipeline can be comple recognition elements in biose	personnel are exposed to the ors, devices that combine a b and are urgently needed to or reliance upon animal-gener ion are slow, difficult, and se racterized an alternative met all viruses (bacteriophages) excludes phages with peptic two-step panning scheme ca des with desirable character eted in approximately ten we ensors when compared to m	e widest variet biological elem detect and ider ated antibodie equential proce hod for produc which display les that bind a in be tuned to istics for use a reks and the po ore traditional,	by of biological, chemical, environmental, and ent with a technological sensor platform to detect an ntify threats in real-time. Unfortunately, biosensors s as their biological recognition elements. Antibody esses that rely upon inducing an immune response in cing biological recognition elements: phage display. short, random peptides. We intended to develop a background solution and collects only those which include almost any analyte or background solution. It is biological detection elements in biosensors. The eptides it yields have many advantages as , antibody-based elements.	
Biosensors, biorecognition, phage display				
16. SECURITY CLASSIFICATION a. REPORT b. ABSTRACT c.	OF: 17. LIMITATION THIS PAGE OF ABSTRACT	18. NUMBER OF PAGES	19a. NAME OF RESPONSIBLE PERSON Commanding Officer	
UNCL UNCL	UNCL UNCL UNCL UNCL	34	19b. TELEPHONE NUMBER (INCLUDING AREA CODE) COMM/DSN: 210-539-5334 (DSN: 389)	
	•		Standard Form 298 (Rev. 8-98)	